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1 **Neural compensation mechanisms of siblings of schizophrenia patients as revealed by**
2 **high-density EEG**

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19

20 **Abstract**

21 Visual backward masking (VBM) deficits are candidate endophenotypes of schizophrenia
22 indexing genetic liability of the disorder. In VBM, a target is followed by a mask that deteriorates
23 target perception. Schizophrenia patients and, to a lesser extent, their unaffected relatives show
24 strong and reproducible VBM deficits. In patients, VBM deficits are associated with strongly
25 decreased amplitudes in the evoked-related potentials (ERPs). Here, to unveil the neural
26 mechanisms of VBM in schizophrenia, circumventing illness-specific confounds, we investigated
27 the EEG correlates of VBM in unaffected siblings of schizophrenia patients. We tested 110
28 schizophrenia patients, 60 siblings, and 83 healthy controls. As in previous studies, patients
29 showed strong behavioral deficits and decreased ERP amplitudes compared to controls.
30 Surprisingly, the ERP amplitudes of siblings were even higher than the ones of controls, while
31 their performance were similar. ERP amplitudes in siblings were found to correlate with
32 performance. These results suggest that VBM is deteriorated in patients and siblings. However,
33 siblings, unlike patients, can partially compensate for the deficits by over-activating a network of
34 brain regions.

35 **Keywords:** siblings, schizophrenia, compensation, GFP, EEG, backward masking

36 **1. Introduction**

37 Endophenotypes are trait rather than state markers of a disease supervening on the genetic
38 makeup¹. Several candidate endophenotypes have been proposed for schizophrenia.
39 Endophenotypes based on visual processing are of great interest because of their good
40 reproducibility, language independence, and contributions to higher cognitive impairments²⁻⁶.

41 Visual backward masking (VBM) is one of such endophenotypes of schizophrenia⁷⁻¹¹, specially
42 the shine-through paradigm, which has a much higher sensitivity and specificity for schizophrenia
43 than most other cognitive and perceptual paradigms^{4,12}. In VBM, a briefly presented target is
44 followed by a mask, which decreases performance in discriminating the target¹³. In the shine-
45 through paradigm, the target is comprised of a vernier stimulus and the mask is comprised of 25
46 straight verniers making up a grating (sub-section 2.2). If the stimulus-onset asynchrony (SOA) is
47 short enough, the vernier *shines-through* the grating appearing wider and brighter than it really is.
48 The decrement of performance due to the mask is much stronger in schizophrenia patients than in
49 healthy controls¹⁴. Strong impairments are also found in healthy adolescents with psychosis¹⁵⁻¹⁷,
50 dismissing the argument that VBM deficits are primarily due to long term medication and social
51 situation. Unaffected first-order relatives (offsprings, siblings, and parents) of schizophrenia
52 patients also show strong VBM deficits, as requested for an endophenotype^{4,18,19}. Importantly,
53 relatives are not medicated and thus these deficits add further evidence that masking deficits are
54 trait rather than state markers. Here, in experiment 1, we replicated these results. Moreover, we
55 identified abnormalities in a single nucleotide polymorphism (SNP) related to the cholinergic
56 nicotinic receptor ($\alpha 7$), which correlated well with performance in the shine-through paradigm²⁰.

57 The large behavioral deficits in schizophrenia patients are reflected in equally large deficits in
58 electrophysiology correlates as measured by the electroencephalogram (EEG)²¹. Patients have

59 decreased N1 amplitudes at ~200ms after stimulus presentation, as measured by the Global Field
60 Power (GFP). Similar results were found with a cohort of patients with first episode of psychosis²²
61 and students scoring high in schizotypal traits²³.

62 Schizophrenia has a high heritability (70-85%)²⁴ and siblings of schizophrenia patients have an
63 empirical risk of approximately 10-fold higher to develop schizophrenia than the general
64 population^{25,26}. Hence, siblings share a large genetic risk with their affected brothers and sisters.
65 Here, we investigated the neural mechanisms of the shine-through masking paradigm in siblings
66 of schizophrenia patients. As mentioned above, siblings show deteriorated performance in the
67 shine-through paradigm. For this reason, we expected their EEG amplitudes to be in between
68 patients and controls.

69 **2. Methods**

70 **2.1. Participants**

71 122 schizophrenia patients, 62 unaffected siblings of schizophrenia patients, and 85 healthy
72 controls joined the experiments. We excluded 6 patients and 1 sibling because their vernier
73 durations were too long as well as 3 other patients because their SOAs were too long (subsection
74 2.3). 3 patients, 1 sibling, and 2 controls were excluded due to excessive EEG artifacts (subsection
75 2.4.1). Data from 110 patients, 60 siblings, and 83 controls were kept for further analyses. 97 out
76 of 110 patients were receiving neuroleptic medication. Chlorpromazine equivalents are indicated
77 in **Table 1**. Siblings of patients had no history of psychoses. Controls were recruited from the
78 general population, aiming to match patients and siblings as closely as possible. Refer to
79 [Supplementary Material 1.1](#) for additional information on inclusion/exclusion criteria and clinical
80 assessments.

81 Group characteristics are presented in **Table 1**. Since patients and controls differ in terms of
82 gender, education and visual acuity, gender was used as a factor while education and visual acuity
83 were used as covariates in subsequent analyses.

84 45 out of the 60 siblings were siblings of a single patient in the current study (hereinafter
85 referred to as siblings_45 and patients_45). The remaining 15 siblings were siblings of patients
86 that performed a battery of tests but did not participate in the current EEG experiment. Group
87 characteristics of patients_45 and siblings_45 are presented in **Table 1**. In subsequent analyses,
88 for each variable of interest, the score of siblings_45 was subtracted from their patients_45 pair,
89 resulting in a difference score (Δ), which was submitted for statistical analysis.

90 All procedures complied with the Declaration of Helsinki and were approved by the local ethics
91 committee.

Table 1 - Group average statistics (\pm SD) of schizophrenia patients, their siblings, controls, patients_45, and siblings_45.

	Patients	Siblings	Controls	Patients_45	Siblings_45	Statistics		
						Patients vs. Controls	Siblings vs. Controls	Patients_45 vs. Siblings_45
Gender (F/M)	17/93	32/28	39/44	10/35	25/20	$\chi^2(1)=22.838, p<.001$	$\chi^2(1)=.561, p=.454$	$\chi^2(1)=10.519, p=.002$
Age	35.7 \pm 8.8	32.1 \pm 9.9	34.3 \pm 7.8	33.0 \pm 8.8	32.3 \pm 9.1	$t(191)=1.147, p=.506$	$t(141)=1.482, p=.423$	$t(44)=.934, p=.506$
Education	13.3 \pm 2.6	14.1 \pm 3.0	15.2 \pm 2.8	13.4 \pm 2.6	14.6 \pm 2.9	$t(191)=4.889, p<.001$	$t(141)=2.251, p=.052$	$t(44)=2.219, p=.052$
Handedness (R/L)	105/5	57/3	78/5	43/2	43/2	$\chi^2(1)=.211, p=1.000$	$\chi^2(1)=.069, p=1.000$	$\chi^2(1)=.000, p=1.000$
Visual acuity	1.4 \pm .4	1.5 \pm .4	1.6 \pm .4	1.4 \pm .4	1.5 \pm .4	$t(191)=2.700, p=.024$	$t(141)=.914, p=0.724$	$t(44)=.896, p=.724$
Vernier duration*	30 [20, 40]	20 [20, 20]	20 [20, 20]	20 [20, 40]	20 [20, 20]	$\chi^2(1)=63.021, p<.001$	$\chi^2(1)=.000, p=1.000$	$\chi^2(1)=3.533, p=.120$
Illness duration	11.7 \pm 8.0			8.9 \pm 7.5				
SANS	10.4 \pm 5.2			10.5 \pm 5.6				
SAPS	9.8 \pm 7.4			9.2 \pm 3.2				
CPZ	560.2 \pm 393.5			560.9 \pm 398.3				

Abbreviations: SANS, Scale for the Assessment of Negative Symptoms; SAPS, Scale for the Assessment of Positive Symptoms; CPZ, Chlorpromazine equivalents.

*Median [25th percentile, 75th percentile], Mood's median test

P-values Bonferroni-Holm corrected for multiple comparisons for each pairwise group comparisons within each variable of interest.

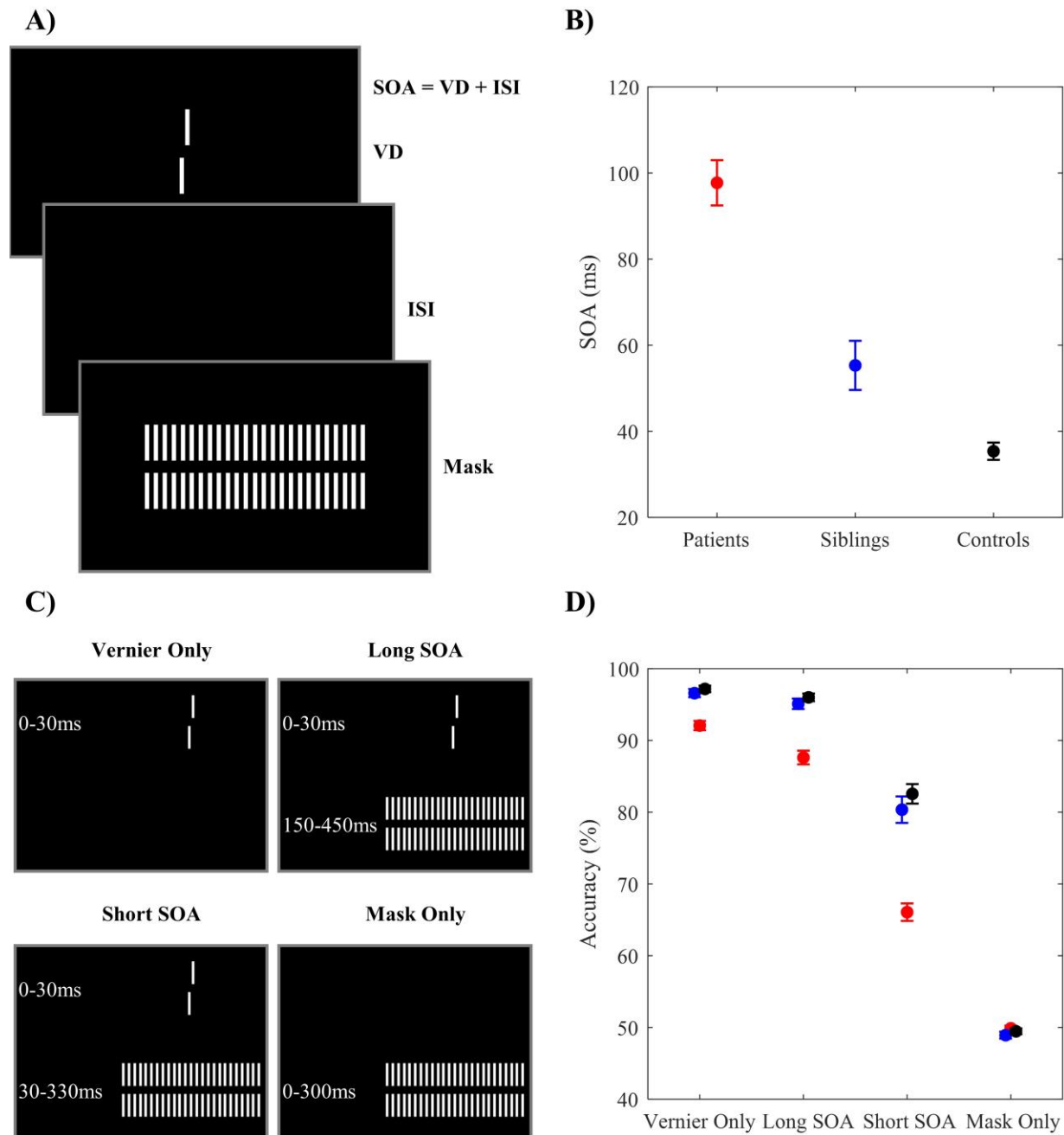
94 **2.2. Stimuli**

95 The apparatus is described in [Supplementary Material 1.2](#). The vernier stimulus consisted of 2
96 vertical line segments of 10' (arc minutes) length separated by a gap of 1' (**Figure 1A**). The lower
97 line was slightly offset randomly either to left or to the right compared to the upper one, with a
98 fixed offset of about 1.2'. The mask consisted of 25 aligned verniers without horizontal offset,
99 separated by 3.33'. Participants reported the perceived horizontal offset direction by pushing one
100 of two buttons and guessed when they were uncertain. Accuracy was emphasized over speed.

101 **2.3. Experiment 1 – Adaptive Procedure**

102 The paradigm is described in detail in previous work¹⁴. Briefly, for each participant, we
103 determined the vernier duration (VD) necessary to reach 75% correct responses for a vernier offset
104 of 0.6'. Participants had to reach a VD shorter than 100ms. 6 patients and 1 sibling were excluded
105 at this stage. Next, we presented the vernier with the individual VD for each participant and an
106 offset of 1.2', followed by an inter-stimulus interval (ISI) and the mask with a duration of 300ms
107 (**Figure 1A**). In a staircase procedure, we adaptively determined the target-mask stimulus-onset
108 asynchrony ($SOA=VD+ISI$) to yield a performance level of 75% correct responses, using
109 Parametric Estimation by Sequential Testing (PEST)²⁷. Each participant performed the test twice.
110 First and second testing results were averaged and submitted to statistical analysis. For patients vs.
111 controls, we performed a two-way ANCOVA; for siblings vs. controls, an independent samples *t*-
112 test; for patients_45 vs. siblings_45, a one-sample *t*-test.

113 Participants with mean SOAs longer than 300ms, twice the mean SOA of patients in previous
114 works^{4,14,21,22}, were excluded at this stage (3 patients).



115

116 **Figure 1 - A)** Experiment 1: stimulus display. For each participant, we determined his/hers
 117 vernier duration (VD). Then, for each observer, we used his/hers VD and presented a blank screen
 118 (ISI) and a mask. We determined the stimulus-onset asynchrony ($SOA=VD+ISI$), for which 75%
 119 correct responses were reached. B) Mean SOA for each group, in experiment 1. Performance of
 120 patients and siblings were worse than the one of controls. C) Experiment 2: stimulus conditions.
 121 In the Vernier Only condition, the vernier was presented alone for 30ms. In the Short and Long

122 SOA conditions, the vernier was followed by a mask with an SOA of either 30 or 150ms,
123 respectively. In the Mask Only condition, only the mask was presented. D) Mean accuracy for
124 each group for the 4 conditions, in experiment 2. Patients were less accurate at discriminating the
125 vernier offset compared to both siblings and controls. Siblings and controls performed at the same
126 level. Error bars indicate standard error of the mean (s.e.m.).

127 **2.4. Experiment 2 – EEG**

128 Since the ERPs peak latencies and amplitudes vary with the VD and SOAs, for the EEG
129 experiment, we fixed the VD and SOAs and used the same stimuli for all observers. To ensure that
130 patients could do the task, we set the VD to 30ms (average VD of patients in previous works^{4,14}).
131 We had 4 stimulus conditions (**Figure 1C**), as in previous works^{21,23,28}. In the Vernier Only
132 condition, only the target vernier was presented. In the Long SOA condition, the mask followed
133 the target vernier with an SOA of 150ms. In the Short SOA condition, the target vernier was
134 followed immediately by the mask (SOA=30ms). The SOAs in the Long and Short SOA conditions
135 were selected according to the mean SOA across schizophrenia patients and controls, respectively,
136 in previous works^{4,14,21,22}. We included a control, the Mask Only condition, in which only the mask
137 was presented. In this particular case, accuracy was calculated by comparing the left/right offset
138 response to a randomly chosen notional offset.

139 For patients vs. controls, a three-way repeated measures (rm)-ANOVA with Greenhouse-
140 Geisser correction ($\hat{\epsilon}$) was conducted to compare the effect Group, Condition (Vernier Only, Long
141 SOA, and Short SOA), and Gender on performance; for siblings vs. controls, a two-way rm-
142 ANOVA (factors: Group and Condition); for patients_45 vs. siblings_45, a one-way rm-ANOVA
143 (factor: Condition).

144 **2.4.1. EEG Recording and Pre-Processing**

145 EEG was recorded using a BioSemi Active 2 system with 64 Ag-AgCl sintered active
146 electrodes, referenced to the common mode sense (CMS) electrode. The sampling rate was
147 2048Hz. Offline data were pre-processed using an automatic pre-processing pipeline (APP)²⁹

148 (Supplementary Material 1.4.1 for details) . Data from 3 patients and 1 control were excluded from
149 further analysis due to excessive muscular artifacts or bad electrodes.

150 **2.4.2. GFP Analysis**

151 To avoid the pitfalls of reference-dependency of ERPs and arbitrarily selecting a group of
152 electrodes for analysis, we determined the GFP for each participant and each condition. GFP is a
153 reference-independent measure of neural activity throughout the brain and it is computed as the
154 standard deviation of potentials across all electrodes at a given time point³⁰. For each group, we
155 computed a grand-average GFP for each of the 4 stimulus conditions (**Figure 2B**) and identified
156 the peak latencies for each condition. Peak amplitudes differed in each condition because the mask
157 onset latency depended on condition. We statistically compared the GFP peak amplitudes across
158 subjects. For patients vs. controls, we conducted a three-way rm-ANOVA (factors: Group,
159 Condition (Vernier Only, Long SOA, Short SOA, and Mask Only), and Gender); for siblings vs.
160 controls, a two-way rm-ANOVA (factors: Group, and Condition); for patients_45 vs. siblings_45,
161 a one-way rm-ANOVA (factor: Condition).

162 **2.4.3. Electrical Source Imaging (ESI)**

163 To identify the brain areas generating the GFP effects, we compared the estimated current
164 densities (CDs) at GFP peak latencies. Source analysis was performed using CARTOOL³¹. From
165 the individually averaged ERPs, we estimated CDs throughout the brain using a Local Auto-
166 Regressive Average (LAURA) inverse solution³². A source space of 4022 points evenly distributed
167 throughout the grey matter of the Montreal Neurological Institute's (MNI) 152 non-linear atlas
168 template brain model was defined, and a model identical to previous works³³⁻³⁵ was used.

169 For patients vs. controls and siblings vs. controls, two-way rm-ANOVAs with factors Group,
170 and Condition were computed on the CDs for each solution point. For patients_45-siblings_45,
171 their difference score (Δ) of the CDs for each solution point were submitted to a one-way rm-
172 ANOVA. Multiple comparisons across the 4022 solution points were corrected using Bonferroni-
173 Holm correction. For each cluster of statistically significant solution points, the average position
174 of its solution points, weighted according to their effect sizes, was computed for identification of
175 its center of mass (CoM). CD of the solution point closest to each CoM was used to represent the
176 corresponding brain region.

177 **3. Results**

178 **3.1. Experiment 1 – Adaptive Procedure**

179 We first made sure that siblings show VBM deficits as in previous findings⁴. Indeed, mean SOA
180 of patients and siblings were longer than the one of controls (patients vs. controls: $p_{holm}=1.624e-$
181 14, $d=1.226$; siblings vs. controls: $p_{holm}=3.103e-4$, $d=0.627$; **Figure 1B**). Patients_45 had longer
182 mean SOA than their paired siblings_45 ($\Delta=-5.78\% \pm 10.18$; $p_{holm}=6.098e-7$, $d=0.899$). Detailed
183 statistics in [Supplementary Material 2.1](#).

184 **3.2. Experiment 2 – EEG**

185 **3.2.1. Behavior**

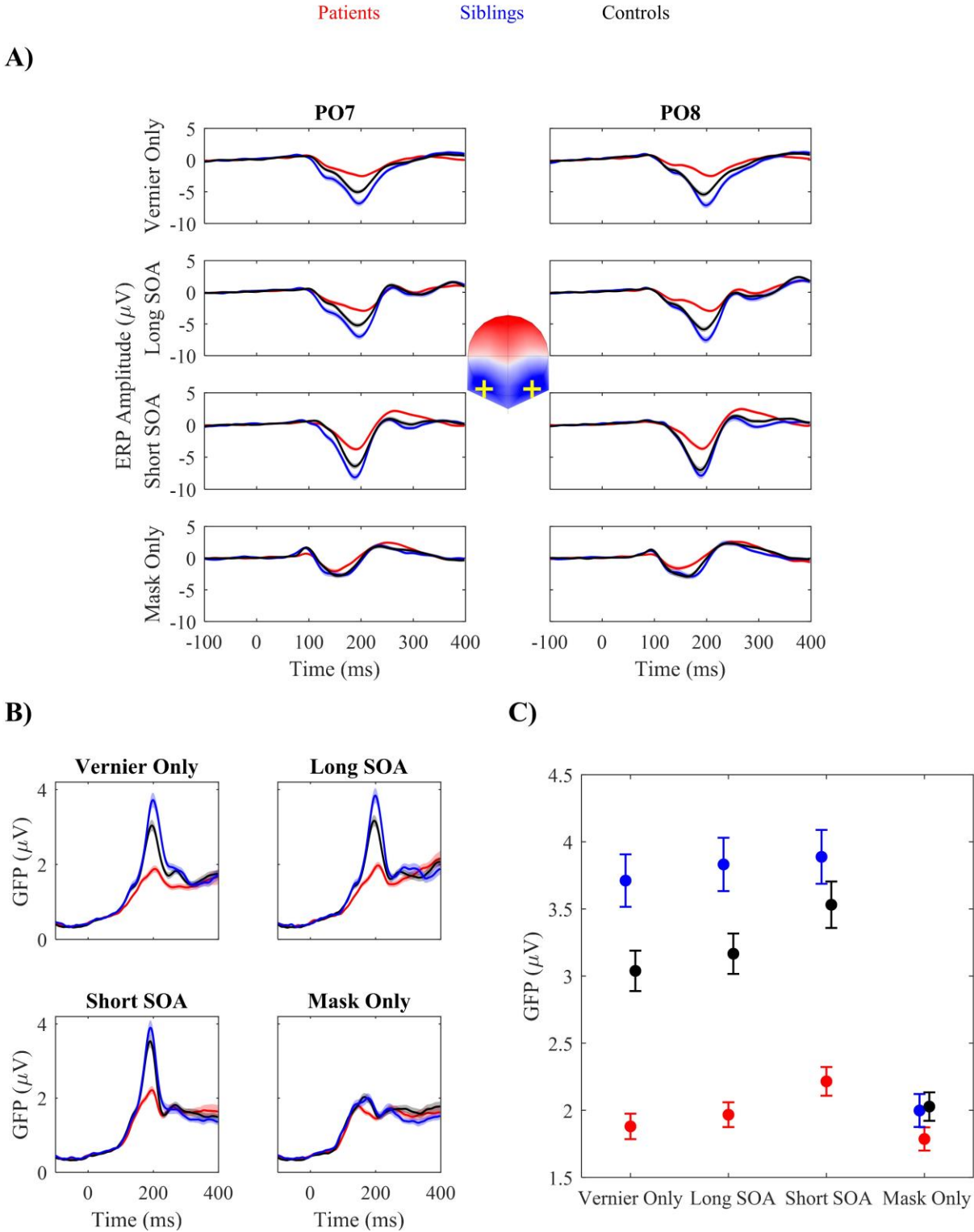
186 Performance of patients was inferior to the one of controls in the 3 conditions with the target
187 vernier (Vernier Only: $p_{holm}=8.109e-5$, $d=0.625$; Long SOA: $p_{holm}=4.577e-6$, $d=0.739$; Short SOA:
188 $p_{holm}=1.0325e-9$, $d=0.975$), while siblings and controls achieved similar performances
189 ($p_{holm}=0.297$, $d=0.180$; **Figure 1D**). Unlike in experiment 1, where we used an adaptive procedure,
190 in the EEG experiment, we used the same stimuli for all participants and fixed the VD as the mean

191 VD of patients. Likely for these reasons, the task was not challenging enough to bring out group
192 differences between siblings and controls. Regarding patients_45 vs. siblings_45, patients_45
193 achieved worse performance than their siblings_45 in all conditions: Vernier Only ($\Delta=-5.78\% \pm$
194 10.18 ; $p_{holm}=8.526e-4$, $d=0.568$), Long SOA ($\Delta=-9.04\% \pm 12.2$; $p_{holm}=4.256e-5$, $d=0.741$), and
195 Short SOA ($\Delta=-16.71\% \pm 17.28$; $p_{holm}=3.858e-7$, $d=0.967$). Detailed statistics in [Supplementary](#)
196 [Material 2.2.1](#).

197 **3.2.2. GFP**

198 Signals from occipital electrodes PO7 and PO8 were extracted to visualize the negative and
199 positive components of the ERPs (**Figure 2A**). Participants showed strong negative ERPs at
200 ~200ms after stimulus-onset. GFP time course for patients, siblings, and controls in the 4 stimulus
201 conditions are shown in **Figure 2B**. Analysis of the GFP peak amplitudes (**Figure 2C**) showed
202 that patients had decreased GFP peak amplitudes than controls in all target conditions: Vernier
203 Only ($p_{holm}=4.466e-5$, $d=0.663$), Long SOA ($p_{holm}=1.067e-5$, $d=0.721$), and Short SOA
204 ($p_{holm}=1.211e-4$, $d=0.617$). In the Mask Only condition, patients and controls GFP peak amplitudes
205 were comparable ($p_{holm}=0.856$, $d=0.110$). Patients_45 showed decreased GFP peak amplitudes
206 compared to their siblings_45 pairs in all conditions: Vernier Only ($\Delta=-1.64\mu V \pm 1.72$;
207 $p_{holm}=9.541e-07$, $d=0.954$), Long SOA ($\Delta=-1.69\mu V \pm 1.67$; $p_{holm}=2.81e-7$, $d=1.012$), Short SOA
208 ($\Delta=-1.54\mu V \pm 1.85$; $p_{holm}=1.364e-5$, $d=0.828$), and Mask Only ($\Delta=-0.43\mu V \pm 0.96$; $p_{holm}=0.030$,
209 $d=0.445$). Interestingly, GFP peak amplitudes were higher in siblings compared to controls for the
210 Vernier Only ($p_{holm}=0.030$, $d=0.469$) and Long SOA ($p_{holm}=0.030$, $d=0.461$) conditions. Siblings
211 and controls had comparable GFP peak amplitudes for Short SOA ($p_{holm}=0.543$, $d=0.228$) and
212 Mask Only ($p_{holm}=0.857$, $d=0.031$) conditions. For siblings, GFP peak amplitudes were roughly at
213 the same level in all 3 target conditions (one-way rm-ANOVA; $F(1.395,82.277)=1.593$, $P=0.208$,

214 $\eta^2=0.002$, $\hat{\epsilon}=1.434$). For controls and patients, GFP peak amplitudes increased with task difficulty,
215 i.e., from Vernier Only to Long SOA and to Short SOA conditions (one-way rm-ANOVA;
216 controls: $F(1.309,107.314)=16.761$, $P=1.522e-5$, $\eta^2=0.021$, $\hat{\epsilon}=1.528$; patients:
217 $F(1.395,152.074)=13.834$, $P=4.415e-5$, $\eta^2=0.019$, $\hat{\epsilon}=1.434$). GFP peak amplitudes correlated
218 positively with the performance for all target conditions, when considering all participants.
219 Considering each group separately, this was also the case for siblings for the Vernier Only
220 ($r(58)=0.393$, $p_{holm}=0.018$) and Long SOA ($r(58)=0.362$, $p_{holm}=0.040$) conditions. Detailed
221 statistics in [Supplementary Material 2.2.2](#).
222



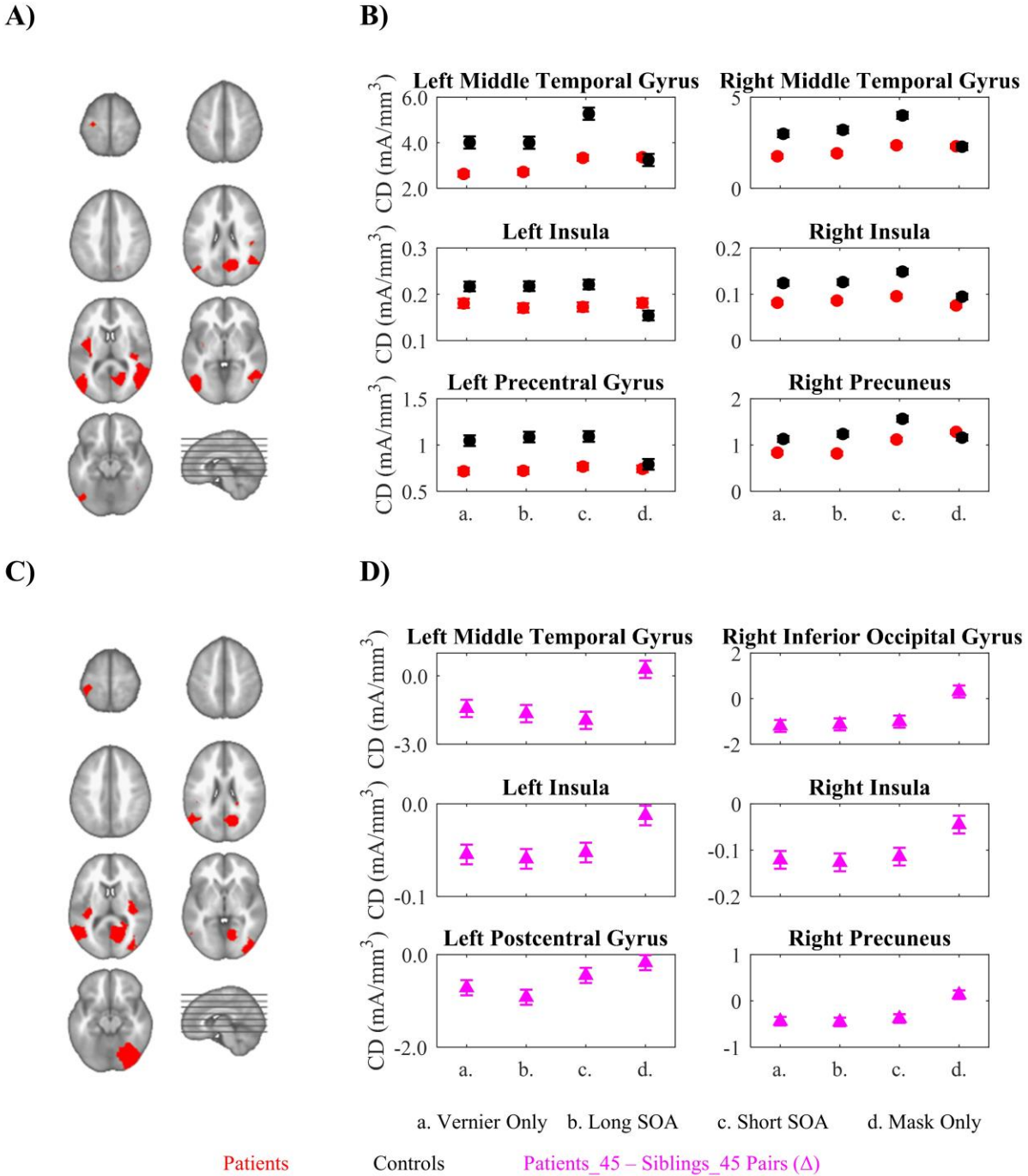
223

224 **Figure 2 - A)** Group grand average ERPs at PO7 and PO8 electrodes, in each condition.
 225 Participants showed negative deflections peaking around 200ms, resembling the N1 component.

226 B) Group average Global Field Power (GFP) time series in each condition. C) Group average peak
227 GFP amplitudes for all conditions. Patients had decreased GFP peak amplitudes in all target
228 conditions. Siblings had higher amplitudes than controls in the Vernier Only and Long SOA
229 conditions. For patients and controls, GFP amplitudes increased with task difficulty. For siblings,
230 GFP amplitudes remained on a high level. Shaded areas and error bars indicate s.e.m.

231 3.2.3. ESI

232 **Figure 3** shows the EEG source clusters exhibiting statistically significant Group×Condition
233 interaction effects (for patients vs. controls) and Condition effects (for patients_45 vs. siblings_45)
234 after correction for multiple comparisons, as well as the corresponding average CD in each group.
235 No statistically significant interactions effects were found for siblings vs. controls. For patients vs.
236 controls, clusters were located bilaterally in the middle temporal gyrus and insula, as well as in the
237 left precentral gyrus and the right precuneus. For patients_45 vs. siblings_45, clusters were located
238 in the left middle temporal gyrus, right inferior occipital gyrus, right/left insula, left postcentral
239 gyrus and right precuneus. **Table 2** lists the Talairach coordinates of the CoM for these clusters.
240 Detailed statistics in [Supplementary Material 2.2.4](#).



241

242 **Figure 3** - Source imaging results. A) Clusters exhibiting significant Group x Condition
 243 interaction effects for patients vs. controls are indicated in red. B) Average current density (CD)
 244 at the centers of mass (CoM) for the 6 clusters, indicating the direction of the interaction effects.
 245 C) Clusters exhibiting significant Condition effects for patients_45 vs. siblings_45. D)
 246 Patients_45-siblings_45 difference score at the CoM for the 6 clusters, indicating the direction of

247 the differences. In general, group differences were larger in target conditions compared to the
 248 Mask Only condition. Error bars indicate s.e.m.

249

250 **Table 2** - Locations of the center of mass of the EEG source clusters showing condition
 251 dependent group effects.

Comparison	Label	Talairach Coordinates (x,y,z)
Patients vs. Controls	Left Middle Temporal Gyrus	-43, -68, 6
	Left Insula	-34, -6, 14
	Left Precentral Gyrus	-27, -21, 56
	Right Middle Temporal Gyrus	47, -54, 11
	Right Insula	36, -27, 21
	Right Precuneus	15, -63, 23
Patients_45 vs. Siblings_45	Left Middle Temporal Gyrus	-54, -61, 17
	Left Insula	-31, -27, 21
	Left Postcentral Gyrus	-34, -33, 58
	Right Inferior Occipital Gyrus	32, -75, -3
	Right Insula	35, -22, 15
	Right Precuneus	20, -63, 18

252

253 Results of multiple linear regressions to predict the accuracy based on the estimated CDs of the
 254 CoM of the source clusters revealed that for siblings the activity of the right insula predicted
 255 accuracy in all conditions with the target vernier: Vernier Only ($\beta=1.330$, $SE=0.553$, $t(58)=2.410$,
 256 $p=0.019$); Long SOA ($\beta=1.754$, $SE=0.701$, $t(58)=2.502$, $p=0.015$); Short SOA ($\beta=4.026$,
 257 $SE=1.798$, $t(58)=2.239$, $p=0.029$). Detailed statistics in [Supplementary Materials 2.2.4](#).

258 4. Discussion

259 VBM deficits are candidate endophenotypes for schizophrenia^{4,7-11}. Importantly, not only
 260 patients show strong VBM deficits but also their unaffected relatives^{4,18}, a result that we
 261 reproduced in experiment 1.

262 In schizophrenia patients, the large behavioral deficits are associated with strongly decreased
263 ERP amplitudes at ~200ms after stimulus presentation²¹. Similar results were also found in patients
264 with a first episode of psychosis²² and students with high schizotypal traits²³. Here, we tested 60
265 unaffected siblings of schizophrenia patients. These siblings do not have the disease but they share
266 a large genetic risk with their affected brother and sisters. We expected that, since behavioral
267 performance of relatives is in between the ones of patients and controls, their ERP amplitudes
268 would also be in between the ones of patients and controls. Surprisingly, we found that, on the
269 contrary, ERP amplitudes in siblings were even higher than in controls (we found similar results
270 using the area under the curve, [Supplementary Material 1.4.2.](#) and [2.2.3.](#)). Interestingly, in siblings,
271 these amplitudes were almost constant across target conditions. While, for patients and controls,
272 ERP amplitudes increased with task difficulty, i.e., from Vernier Only to Long and Short SOA.

273 We interpret these results as a compensation signal. To process the target vernier, whose neural
274 correlates are indexed by the ERP component at around 200ms^{36,37}, siblings might need to engage
275 all relevant neural resources in all conditions, independently of task difficulty. Since, in siblings,
276 ERP amplitudes were stable across all target conditions, it suggests that their ERP amplitudes were
277 at ceiling. All observed effects were specific to the target vernier and did not occur when only the
278 mask was presented, suggesting that mainly top-down processes are responsible for these effects.

279 The lack of behavioral differences between siblings and controls in the EEG experiment
280 suggests that, by over-enhancing neural responses to the target, siblings can partially compensate
281 for their VBM deficits, if the task is not too challenging. In siblings, ERP amplitudes correlated
282 with performance, further supporting a compensation hypothesis. Nevertheless, if the task is
283 extremely challenging, e.g., during the adaptive procedure in experiment 1, this compensation
284 mechanism is not sufficient for normal performance.

285 To identify the brain regions generating the ERP effects, we conducted an EEG source
286 localization analysis. For patients-controls comparison, we identified 6 brain regions where the
287 groups processed the stimuli differently: left/right middle temporal gyrus, left/right insula, left
288 precentral gyrus, and right precuneus. Our results are similar to the ones reported in previous
289 works²¹, which identified 7 regions where patients processed the stimuli differently from controls:
290 left middle occipital gyrus, right middle temporal gyrus, left/right insula, left postcentral gyrus,
291 and left/right precuneus. We attribute the small discrepancies between our studies to the
292 intrinsically low spatial resolution of EEG source localization. For siblings-controls comparison,
293 we did not identify any significant differences. Potentially, the effects were not large enough to
294 survive multiple comparison correction. For patients_45-siblings_45 comparison, we identified 6
295 brain regions where the groups processed the stimuli differently. The results were similar to the
296 patients-controls comparison: left middle temporal gyrus, right inferior occipital gyrus, left/right
297 insula, left postcentral gyrus and right precuneus. Again, we attribute the discrepancies to the low
298 spatial resolution of the source localization. In general, as shown in Figure 3, group differences
299 were larger in the target conditions than in the Mask Only condition, providing further evidence
300 that mainly top-down processes are responsible for the ERP effects.

301 Among the identified brain regions, the right insula is of special interest. Multiple regression
302 analysis indicated that activity of the right insula best predicted the behavioral performance,
303 especially for siblings. The insula is associated with several functions. One of special interest is
304 the high-level integration of information from different modalities and brain areas³⁸. It has been
305 proposed that the right insula regulates the interaction between selective attention and arousal to
306 keep focused on the target³⁹. Too little activity of the right insula, as in patients, may lead to an
307 impairment in collecting evidence for decision making. Too much activity of the right insula, as

308 in siblings, might indicate that participants need to engage more to achieve a good performance in
309 this challenging task. However, these interpretations should be taken with care since we lacked a
310 specific hypothesis for the source localization and the accuracy of the method is limited. Further
311 studies with better spatial resolution and targeting the right insula might provide more evidence
312 for these claims.

313 Here, we propose the following hypothesis. When a faint stimulus is presented for a short time,
314 only a weak neural response is elicited and the stimulus goes unnoticed³⁷. Only if this stimulus is
315 task-relevant, mechanisms of target enhancement are recruited to avoid overwriting by
316 subsequently presented stimuli. We believe that target enhancement is a general mechanism
317 occurring at all sorts of processing of task-relevant information, from auditory and visual mismatch
318 negativity^{40,41} to P50 auditory gating⁴² and prepulse inhibition⁴³, rather than vision specific. Target
319 enhancement is potentially a multi-factorial construct³⁶, comprised of, but not limited to, recurrent
320 processing⁴⁴, attention^{45,46}, and/or neuromodulation, for example, by the cholinergic nicotinic
321 system^{20,47,48}, which are important mechanisms to potentiate weak but important information.
322 Attention deficits are core deficits in schizophrenia⁴⁹ and the cholinergic nicotinic system might
323 be deficient in patients²⁰. In the Mask Only condition, patients and controls showed similar
324 amplitudes but patients showed significantly lower amplitudes than their siblings. This indicates
325 that patients might have some slight bottom-up deficits but deficits only become obvious when
326 there is a target. In patients, amplitudes are low in all target conditions. This suggests that patients
327 cannot translate the briefly presented target into a stable neural representation, making the target
328 more vulnerable to masking¹¹. These masking deficits are also present in their unaffected relatives,
329 as corroborated by experiment 1 and previous works^{4,18}. We speculate that, to overcome these
330 deficits, siblings are able to recruit more neural resources. Their increased ERP amplitudes

331 compared to controls support the hypothesis of a compensation mechanism, such that by increasing
332 the activity of a network of brain regions, siblings, unlike patients, can partially compensate for
333 their behavior deficits, if the task is not too challenging (experiment 2). In this network, our results
334 suggest that the right insula, with its extensive connections to many areas of the cortex, might play
335 a key role by integrating high-level sensory as well as perceptual information and subsequent
336 decision-making. Nonetheless, if the task is extremely challenging, as in experiment 1, this
337 compensation mechanism is too weak to fully compensate for the deficits.

338 Our results suggest that even if there are genetic risks for schizophrenia, the brain is somehow
339 capable of compensating for them. Better understanding of these compensation mechanisms might
340 help to explain why some siblings develop schizophrenia and while others do not, which might
341 open new avenues for characterization of schizophrenia and possible treatments of the disorder.

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