Shape Projectors for Landmark-Based Spline Curves

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Abstract—We present a generic method to construct orthogonal projectors for 2D landmark-based parametric spline curves. We construct vector spaces that define a geometric transformation (*e.g.*, affine, similarity, scaling) that is applied to a reference curve. These vector spaces contain all parametric curves up to the chosen transformation. We define the vector spaces implicitly through an orthogonal projection operator and present a theorem that characterizes the projector for landmark-based spline curves which are popular for the user-interactive analysis of biomedical images. Finally, we show how shape priors are constructed with the spline projector and provide an example of application for the segmentation of microscopy images in biology.

Index Terms-projector, landmarks, splines, shape prior

I. INTRODUCTION

W E consider the problem of aligning a *query* curve r defined in the continuous domain as $r(t) = (r_x(t), r_y(t))$ with $t \in \mathbb{R}$, onto a reference shape r^{ref} . Thereby, we allow r^{ref} to deform as $r^{\text{ref}} \mapsto \mathcal{T}_{\theta}\{r^{\text{ref}}\}$ according to a subclass of geometric transformations \mathcal{T}_{θ} that belong to the affine family (see Table I) parameterized by θ . To that end, we consider the generic parametric alignment problem

$$\min_{\boldsymbol{\theta}} \| \mathcal{T}_{\boldsymbol{\theta}} \{ \boldsymbol{r}^{\text{ref}}(t) \} - \boldsymbol{r}(t) \|_{L_2}^2.$$
 (1)

Problem (1) arises in image segmentation settings [1], [2], [3], [4] when prior knowledge is integrated [5], [6], [7] such that the solution should be close to a given shape [8], [9]. For specific transformations where a particular structure is enforced on \mathcal{T}_{θ} several algorithms have been proposed [10], [11], [12], [13]. In [14], we have presented a solution for the specific case $r \mapsto \Theta r + \rho$ with $\Theta \in \mathbb{R}^{2 \times 2}$ and $\rho \in \mathbb{R}^2$, which is not generalizable for the arbitrary case. Here, we derive a closed-form solution of (1) that is applicable to any particular type of transformation of the affine family. Our solution includes the classical case described in procrustean analysis [15], [16] but we are able to retrieve the sought-after similarity transformation in one step. Moreover, we propose an exact spline-based implementation of our continuous-domain framework. We provide a generic solution by defining a finitedimensional vector space that contains all possible shapes obtained by a given transformation of r^{ref} defined by \mathcal{T}_{θ} . We characterize a vector space as a subspace that contains all shapes that are related to a reference shape by a specific transformation. The subspace itself is implicitly characterized by its orthogonal projector. This allows us to compute the "best

Copyright (c) 2017 IEEE. Personal use of this material is permitted. However, permission to use this material for any other purposes must be obtained from the IEEE by sending a request to pubs-permissions@ieee.org. match" among curves defined by a subspace w.r.t. an arbitrary shape. Intuitively speaking, projecting a query shape onto the subspace defined by the reference amounts to "choosing" the reference up to a specific transformation that is closest to the input shape. We propose solutions for continuously defined parametric spline curves. They are popular for interactive applications, where a user manually enforces landmark correspondance to increase robustness. Other applications, where invariance to parameterization is required have been studied in [17], [18], [19].

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II. VECTOR SPACES DEFINING AFFINE SHAPE SPACES

A. Hilbert Space H Containing All Parametric Curves

We denote by $\mathcal{H} : L_2([0,1], \mathbb{R}^2)$ the Hilbert space that contains all parametric curves and is associated with the standard L_2 inner product $\langle \boldsymbol{r}_i, \boldsymbol{r}_j \rangle_{L_2} := \int_0^1 \boldsymbol{r}_i^{\mathrm{T}}(t) \boldsymbol{r}_j(t) dt$. The corresponding norm is defined as $\|\boldsymbol{r}\|_{L_2} := \sqrt{\langle \boldsymbol{r}, \boldsymbol{r} \rangle_{L_2}}$. Without loss of generality, we restrict the parameter domain to $t \in [0, 1]$.

B. Vector Spaces as Subspaces of H

We define a subspace that contains all *specific* affine transformations of the *reference* curve r^{ref} . It can be defined as the finite-dimensional vector space S^{ref} of dimension I, whose basis consists of elements $\{e_i^{\text{ref}}\}_{i=1,...,I}$, which themselves are curves that depend on r^{ref} . Every element (*i.e.*, curve) living in S^{ref} can be expressed as a linear combination of the basis elements. Thus, $S^{\text{ref}} = \left\{\sum_{i=1}^{I} u_i e_i^{\text{ref}}(\cdot) : u_i \in \mathbb{R}\right\}$ is a subspace of the Hilbert space \mathcal{H} .

1) Example: A linear mapping of a 2D curve can be expressed as Θr , where $\Theta = \begin{pmatrix} \theta_1 & \theta_2 \\ \theta_3 & \theta_4 \end{pmatrix}$ is a (2×2) matrix with elements $\theta_i \in \mathbb{R}$. By explicitly evaluating the matrix-vector product, we obtain

$$\boldsymbol{\Theta}\boldsymbol{r}(t) = \theta_1 \begin{pmatrix} r_x(t) \\ 0 \end{pmatrix} + \theta_2 \begin{pmatrix} r_y(t) \\ 0 \end{pmatrix} + \theta_3 \begin{pmatrix} 0 \\ r_x(t) \end{pmatrix} + \theta_4 \begin{pmatrix} 0 \\ r_y(t) \end{pmatrix} + \theta_4 \begin{pmatrix} 0 \\ r_y($$

Therefore, the subspace associated to the 2D reference curve r^{ref} is a four-dimensional vector space (*i.e.*, I = 4) whose basis is given by

$$\{\boldsymbol{e}_i^{\text{ref}}\}_{i\in[1,\ldots,4]} = \left\{ \begin{pmatrix} r_x^{\text{ref}}\\ 0 \end{pmatrix}, \begin{pmatrix} r_y^{\text{ref}}\\ 0 \end{pmatrix}, \begin{pmatrix} 0\\ r_x^{\text{ref}} \end{pmatrix}, \begin{pmatrix} 0\\ r_y^{\text{ref}} \end{pmatrix} \right\},\$$

where we have omitted the continuous parameter t to simplify the notation. Note that the choice of the basis is not unique. However, different bases w.r.t. to a given transformation describe the same space.

C. Construction of Vector Spaces

In Table I we present examples of bases $\{e_i\}_{i=1,...,I}$ that can be used to construct a subspace S^{ref} for specific 2D transformations. Taking a reference curve $r^{\text{ref}} = (r_x^{\text{ref}}, r_y^{\text{ref}})$ and choosing a transformation given in Table I, the corresponding vector space is given by the indicated basis.

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Transformation Degrees of Freedom w.r.t. r^{ref} Basis $\{e^{ref}\}$ uniform scaling 1 non-uniform scaling $\mathbf{2}$ 2 translation 2 uniform scaling + rotation similarity (uniform scaling + rotation + translation) 4 linear mapping 4 affine 6 shear + unifrom scaling $\mathbf{2}$ shear + uniform scaling + translation 4 shear + uniform scaling 2 shear + uniform scaling + translation 4 reflection + uniform scaling + rotation 2 reflection + similarity 4

TABLE I Example Bases for 2D vector spaces.

III. LANDMARK-BASED PARAMETRIC SPLINE CURVES

We consider curves of the form

$$\boldsymbol{r}(t) = \begin{pmatrix} r_x(t) \\ r_y(t) \end{pmatrix} = \sum_{n=0}^{N-1} \boldsymbol{c}[n] \varphi_n(t), \qquad (2)$$

where φ is a compactly supported spline-based generator function and $N \in \mathbb{N}_+$ represents the number of *control points* of the curve. The spline coefficients are given by $\{c[k] = (c_x[k], c_y[k])\}_{k=0,...,N-1}$. The following algorithm can be easily generalized for the case where the summation limits are different than in (2). The sum in (2) is finite which implies that the number of non-zero coefficients c[k]is finite too. From (2), we see that the curve is constructed through integer shifts (represented by n) of the generator φ . Furthermore, for the model (2) to be *affine invariant*, the generator φ needs to be capable of reproducing constants as specified by Proposition 1.

Proposition 1. For $\Theta \in \mathbb{R}^{2 \times 2}$, $\rho \in \mathbb{R}^2$ and a curve r as defined in (2),

$$1 \in \operatorname{span}\{\varphi_n\} \Rightarrow \Theta \mathbf{r}(t) + \boldsymbol{\rho} \in \operatorname{span}\{\varphi_n\}$$

holds.

The proof follows immediately by noticing that, for any constant $\rho \in \mathbb{R}$, the relation $1 \in \operatorname{span}\{\varphi_n\} \Rightarrow \rho \in \operatorname{span}\{\varphi_n\}$ holds. Hence, any translation vector $\rho \in \mathbb{R}^2$ can be represented by (2) while the linearity of the model ensures that $\Theta r(t) \in \operatorname{span}\{\varphi_n\}$.

A. Construction of Vector Spaces Using Spline Curves

To guarantee a unique representation of a spline curve (2) by its control points as well as a stable implementation, φ needs to generate a *Riesz basis* [20] as, for instance, polynomial B-splines do. In that case, we can express the vector spaces defined in Section II-C as a function of the control points of the reference curves. For a curve $\mathbf{r}(t) = (r_x(t), r_y(t))$ we define $\mathbf{c} = (\mathbf{c}_x, \mathbf{c}_y)$, which is a vector of length 2N, where

$$\mathbf{c}_x = (c_x[0], \dots, c_x[N-1]) \tag{3}$$

contains the N coefficients that describe x(t) and the vector \mathbf{c}_y that defines y(t) is constructed in a similar way. Observe that we use regular bold font to describe the \mathbf{c} in (5) as opposed to italic bold font to describe the different object \mathbf{c} in (2).

1) Example - Affine Transformation Combined with Translation: If we include a translation $\rho \in \mathbb{R}^2$ in the transformation described in Section II-B1, then we obtain $\Theta r + \rho$, where Θ is defined as in Section II-B1 and $\rho = (\theta_5, \theta_6)$. The transformation has six degrees of freedom and it is easy to see that a basis for the vector space of the reference curve r^{ref} is given by

$$\boldsymbol{e}_{i}^{\text{ref}}\}_{i\in[1,\ldots,6]} = \left\{ \begin{pmatrix} r_{x}^{\text{ref}}\\0 \end{pmatrix}, \begin{pmatrix} r_{y}^{\text{ref}}\\0 \end{pmatrix}, \begin{pmatrix} 0\\r_{x}^{\text{ref}} \end{pmatrix}, \begin{pmatrix} 0\\r_{y}^{\text{ref}} \end{pmatrix}, \begin{pmatrix} 1\\0 \end{pmatrix}, \begin{pmatrix} 0\\1 \end{pmatrix} \right\},$$

which corresponds to

$$\{\mathbf{c}_{\mathbf{e}_{i}^{\text{ref}}}\}_{i\in[1,\ldots,6]} = \left\{ \begin{pmatrix} \mathbf{c}_{x} \\ \mathbf{0} \end{pmatrix}, \begin{pmatrix} \mathbf{c}_{y} \\ \mathbf{0} \end{pmatrix}, \begin{pmatrix} \mathbf{0} \\ \mathbf{c}_{x} \end{pmatrix}, \begin{pmatrix} \mathbf{0} \\ \mathbf{c}_{y} \end{pmatrix}, \begin{pmatrix} \mathbf{1} \\ \mathbf{0} \end{pmatrix}, \begin{pmatrix} \mathbf{0} \\ \mathbf{1} \end{pmatrix} \right\}$$

where **0** and **1** correspond to the vectors of size N (which is the size of \mathbf{c}_x or \mathbf{c}_y) and whose elements are all 0 or

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1, respectively. The spline projector is then computed by the application of Theorem 1.

IV. L2-INNER PRODUCT OF SPLINE-BASED CURVES

Next, we derive a simple and efficient expression to compute the L_2 -inner product $\langle r_1, r_2 \rangle_{L_2}$ between spline-based curves. We first compute it for the 1D case and then generalize it to higher dimensions.

A. Inner Product

First, we consider spline-based 1D functions of the form $x(t) = \sum_{n=0}^{N-1} c_x[n]\varphi_n(t)$. The L_2 -inner product is then expressed as

$$\langle x_1, x_2 \rangle_{L_2} = \int_0^1 x_1(t) x_2(t) \mathrm{d}t = \sum_{m=0}^{N-1} \sum_{n=0}^{N-1} c_{1x}[m] c_{2x}[n] \langle \varphi_m, \varphi_n \rangle_{L_2}.$$
(4)

We collect all the coefficients of the function x in the vector of length N as specified by (3). We then define $[\Phi]_{m,n} = \langle \varphi_m, \varphi_n \rangle_{L_2}$. Now, (4) is expressed as $\langle x_1, x_2 \rangle_{L_2} = \mathbf{c}_{1x}^T \Phi \mathbf{c}_{2x}$, where Φ is the $(N \times N)$ autocorrelation matrix of φ . For an implementation (4) can be crucial. The entries of the matrix Φ can be precomputed and stored in a look-up table for fast online evaluation. The acceleration is considerable; It is due to the fact that the computation of the integral associated with the inner product (4) boils down to a matrix-vector multiplication.

Similarly, we simplify the 2D inner product. By using the notations introduced in III-A the corresponding inner product is now expressed as

$$\langle \boldsymbol{r}_1, \boldsymbol{r}_2 \rangle_{L_2} = \mathbf{c}_1^{\mathrm{T}} \boldsymbol{\Psi} \mathbf{c}_2 = \langle \mathbf{c}_1, \mathbf{c}_2 \rangle_{\boldsymbol{\Psi}},$$
 (5)

where

$$\Psi = \begin{bmatrix} \Phi & 0\\ 0 & \Phi \end{bmatrix} \tag{6}$$

and **0** is a zero matrix with the same dimensions as Φ .

V. MAIN RESULT: GENERALIZED SPLINE PROJECTORS

Using the simplified expression (5) to compute inner products of spline curves, we can now specify the projection operator. A fundamental aspect of our construction is not only that the curve r that is being projected is a spline curve, but also that the basis $\{e_i^{\text{ref}}\}$ of the subspace S^{ref} consists of spline curves of the form given by (2). Hence, each of these curves $r \in \mathcal{H}$ is uniquely determined by its corresponding vector of control points $\mathbf{c} \in \mathbb{R}^{2N}$.

In this article, we provide the expression for 2D curves, noting that the extension to 3D is straightforward. We first define the matrix $\mathbf{C}^{\text{ref}} = [\mathbf{c}_{e_1^{\text{ref}}} \cdots \mathbf{c}_{e_I^{\text{ref}}}]$. It has the dimension $(2N \times I)$ and contains the control points of the curves $\{e_i^{\text{ref}}\}_{i=1,...,I}$ that define a basis of \mathcal{S}^{ref} . To simplify the notation, we collect all basis functions in the vector $\varphi(t) := (\varphi_0(t), \ldots, \varphi_{N-1}(t))$. The corresponding (orthogonal) spline projector \mathcal{P}^{ref} : $\mathcal{H} \to \mathcal{S}^{\text{ref}}$ that minimizes the distance between the curve $\mathbf{r} \in \mathcal{H}$ and the *I*-dimensional vector space \mathcal{S}^{ref} is specified by Theorem 1.

Theorem 1. Let
$$\mathbf{r}(t) = \boldsymbol{\varphi}(t)^{\mathrm{T}} \mathbf{c}$$
. Then

$$\mathcal{P}^{ref} \boldsymbol{r}(t) = \begin{pmatrix} \boldsymbol{\varphi}(t) & \boldsymbol{0} \\ \boldsymbol{0} & \boldsymbol{\varphi}(t) \end{pmatrix}^{\mathsf{T}} \mathbf{P}^{ref} \mathbf{c},$$

where $\mathbf{P}^{\text{ref}} \in (\mathbb{R}^{2N} \times \mathbb{R}^{2N}) : \mathbb{R}^{2N} \to \mathbb{R}^{2N}$ is the $(2N \times 2N)$ projection matrix defined as

$$\mathbf{P}^{\mathrm{ref}} = \mathbf{C}^{\mathrm{ref}} (\mathbf{C}^{\mathrm{ref}^T} \mathbf{\Psi} \mathbf{C}^{\mathrm{ref}})^{-1} \mathbf{C}^{\mathrm{ref}^T} \mathbf{\Psi}.$$

Proof. If \mathcal{P} is an orthogonal projector w.r.t. span $\{e_i\}_{i=1,...,I}$, then a curve r can always be decomposed as

$$\mathbf{r}(t) = \mathcal{P}\mathbf{r}(t) + \underbrace{(\mathcal{I} - \mathcal{P})\mathbf{r}(t)}_{\text{error}},$$
 (7)

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where \mathcal{I} is the identity operator and the error between the curve and the projective plane is orthogonal to the projective plane, so that error $\perp \operatorname{span}\{e_i\}$. By expressing $\mathcal{P}\mathbf{r} = \sum_i \langle \tilde{e}_i, \mathbf{r} \rangle_{L_2} \mathbf{e}_i(t) = \sum_i u_i \mathbf{e}_i(t)$ in (7) and taking the inner product on both sides w.r.t. \mathbf{e}_k , we obtain the *normal* equation

$$\langle \boldsymbol{r}, \boldsymbol{e}_k \rangle_{L_2} = \sum_i u_i \langle \boldsymbol{e}_i, \boldsymbol{e}_k \rangle_{L_2} + \underbrace{\langle \mathcal{I} - \mathcal{P} \rangle \boldsymbol{r}(t), \boldsymbol{e}_k \rangle_{L_2}}_{0}.$$
 (8)

Evaluating (8) for all elements of the basis $\{e_k\}$ and writing all the equations in matrix form, we obtain

$$\begin{pmatrix} \langle \boldsymbol{r}, \boldsymbol{e}_1 \rangle_{L_2} \\ \vdots \\ \langle \boldsymbol{r}, \boldsymbol{e}_I \rangle_{L_2} \end{pmatrix} = \mathbf{G} \mathbf{u} \Leftrightarrow \mathbf{u} = \mathbf{G}^{-1} \begin{pmatrix} \langle \boldsymbol{r}, \boldsymbol{e}_1 \rangle_{L_2} \\ \vdots \\ \langle \boldsymbol{r}, \boldsymbol{e}_I \rangle_{L_2} \end{pmatrix}.$$

Using the notation $\mathbf{E} = [e_1 \cdots e_I]$, $\mathbf{G} = \mathbf{C}^T \Psi \mathbf{C}$ being the Gram matrix with respect to the basis $\{e_i\}$ and $g = (\langle e_1, r \rangle_{L_2}, \dots, \langle e_I, r \rangle_{L_2})$, the orthogonal projection of r is expressed as

$$\mathcal{P}\boldsymbol{r}(t) = \mathbf{E}\mathbf{G}^{-1}\boldsymbol{g} = \sum_{i=1}^{I} \boldsymbol{e}_{i}(t) \underbrace{\langle \mathbf{G}_{i,1}^{-1}\boldsymbol{e}_{1} + \dots + \mathbf{G}_{i,I}^{-1}\boldsymbol{e}_{I}, \boldsymbol{r} \rangle_{L_{2}}}_{\langle \tilde{\boldsymbol{e}}_{i}, \boldsymbol{r} \rangle_{L_{2}}} \langle \boldsymbol{e}_{i}, \boldsymbol{r} \rangle_{L_{2}}}$$
(9)

where $\{\tilde{e}_i\}$ forms the dual basis of $\{e_i\}$ and is defined as $\tilde{\mathbf{E}} = \mathbf{E}(\mathbf{G}^{-1})^{\mathrm{T}} = [\tilde{e}_1 \cdots \tilde{e}_I]$. Because φ generates a Riesz basis, each coordinate function of a spline curve r given by (2) is uniquely specified by its control points $\{\mathbf{c}[k]\}_{k\in\mathbb{Z}}$. This implies that there is a one-to-one relation between the coordinate functions of the curve and its spline coefficients. Hence, the matrix \mathbf{E} in (9) that defines the basis $\{e_i\}$ for the subspace \mathcal{S} (not to be confused with the Riesz basis generated by φ) is fully specified by $\mathbf{C} = [\mathbf{c}_1 \cdots \mathbf{c}_I]$ which is the matrix that contains all the control points of the basis $\{e_i\}$. Using (5), we rewrite (9) as

$$\mathcal{P}\boldsymbol{r}(t) = \mathbf{E}\mathbf{G}^{-1}\boldsymbol{g} = \mathbf{E}\mathbf{G}^{-1}(\langle \boldsymbol{e}_1, \boldsymbol{r} \rangle_{L_2}, \dots, \langle \boldsymbol{e}_I, \boldsymbol{r} \rangle_{L_2})$$

which is equivalent to

$$\mathbf{C}\mathbf{G}^{-1}(\mathbf{c}_1^{\mathrm{T}}\boldsymbol{\Psi},\ldots,\mathbf{c}_I^{\mathrm{T}}\boldsymbol{\Psi})\mathbf{c}=\mathbf{C}\mathbf{G}^{-1}\mathbf{C}^{\mathrm{T}}\boldsymbol{\Psi}\mathbf{c}=\mathbf{P}\mathbf{c}.$$

Hence, $\mathbf{P} = \mathbf{C}(\mathbf{C}^{\mathrm{T}} \boldsymbol{\Psi} \mathbf{C})^{-1} \mathbf{C}^{\mathrm{T}} \boldsymbol{\Psi}$. It is easily verified that \mathbf{P} is a projector, characterized by the idempotent relation $\mathbf{P}^{2} = \mathbf{P}$.

Theorem 1 provides a direct method to compute the control points of the projected curve. Note that the projection of the vector **c** of control points is itself not orthogonal. However, it corresponds to the orthogonal projection of \boldsymbol{r} in the L_2 -sense. Therefore, we have $(\mathbf{P}^{\text{ref}})^2 = \mathbf{P}^{\text{ref}}$ and $\mathbf{P}^{\text{ref}^T} \neq \mathbf{P}^{\text{ref}}$. Hence, Theorem 1 shows that \mathbf{P}^{ref} is an *oblique* projector from \mathbb{R}^{2N} onto the *I*-dimensional invariant subspace of \mathbb{R}^{2N} defined by the basis $\{\mathbf{c}_{\boldsymbol{e}_1^{\text{ref}}}\}_{i=1,...,I}$. This means that $\mathcal{P}^{\text{ref}} : \mathcal{H} \to \mathcal{S}^{\text{ref}}$, which is the orthogonal projector in the L_2 -sense, is efficiently implemented via the oblique projector $\mathbf{P}^{\text{ref}} \in (\mathbb{R}^{2N} \times \mathbb{R}^{2N})$: $\mathbb{R}^{2N} \to \mathbb{R}^{2N}$.

A. Example

We show how the projectors that correspond to the vector spaces listed in Table I are implemented using splines, in accordance with Theorem 1. The simplest case is the scaling projector which can be expressed by solving $\min_{a} ||ar^{\text{ref}} - r||_{L_2}^2$ such that $\mathcal{P}^{\text{ref}}r(t) = ar^{\text{ref}}$, where r^{ref} is the reference curve that defines the vector space. Its well known solution is $a = \frac{\langle r^{\text{ref}}, r\rangle_{L_2}}{\langle r^{\text{ref}}, r^{\text{ref}} \rangle_{L_2}}$. Using (5), the corresponding spline projector is specified by $\mathbf{P}^{\text{ref}} = \mathbf{c}^{\text{ref}} \frac{\mathbf{c}^{\text{ref}} \Psi}{\langle \mathbf{c}^{\text{ref}}, \mathbf{c}^{\text{ref}} \rangle_{\Psi}}$, which corresponds to the solution obtained by the direct application of Theorem 1.

VI. APPLICATION: SEGMENTATION IN BIOIMAGING

In segmentation algorithms, it is advantageous if prior knowledge about shapes can be integrated [5], [6], [21], for instance in active contour models [1], [11], [22], [23], [24]. Our proposed formulation of a projector allows us to compute the distance between a shape and the vector space given by a reference shape. Hence, we can penalize the cases where a shape is distant from the given vector space defined by the reference shape r^{ref} . To illustrate this concept, we consider the example of spline-based snakes [25]. We denote by $E(\Omega)$ the standard energy term that usually needs to be minimized w.r.t. the snake-defining parameters described by Ω . The minimization of $E(\Omega)$ attracts the contour of the snake towards the boundary of the object of interest. We propose to add a prior term to E that we define as $E_{\text{prior}} = \gamma \| \boldsymbol{r} - \mathcal{P}^{\text{ref}} \boldsymbol{r} \|_{L_2}^2$, where $\gamma \in \mathbb{R}$ controls the contribution of the prior energy term. We re-express E_{prior} as

$$\|\boldsymbol{r} - \boldsymbol{\mathcal{P}}^{\mathrm{ref}}\boldsymbol{r}\|_{L_2}^2 = \langle \boldsymbol{r}, (\boldsymbol{\mathcal{I}} - \boldsymbol{\mathcal{P}}^{\mathrm{ref}})\boldsymbol{r} \rangle_{L_2}, \quad (10)$$

where \mathcal{I} denotes the identity operator and where we have used the fact that, since \mathcal{P}^{ref} is orthogonal and hence, self-adjoint, then $(\mathcal{I} - \mathcal{P}^{\text{ref}})$ is also an orthogonal projector. We use (5) and Theorem 1 to compute the projector. Then, (10) is developed as

$$\|\boldsymbol{r} - \boldsymbol{\mathcal{P}}^{\text{ref}}\boldsymbol{r}\|_{L_{2}}^{2} = \mathbf{c}^{\mathrm{T}} \underline{\boldsymbol{\Psi}(\mathbf{I} - \mathbf{P}^{\text{ref}})\mathbf{c}} \\ = \mathbf{c}^{\mathrm{T}} \underbrace{\underline{\boldsymbol{\Psi}(\mathbf{I} - \mathbf{C}(\mathbf{C}^{\mathrm{T}}\underline{\boldsymbol{\Psi}}\mathbf{C})^{-1}\mathbf{C}^{\mathrm{T}}\underline{\boldsymbol{\Psi}})}_{\mathbf{S}} \mathbf{c} = \mathbf{c}^{\mathrm{T}}\mathbf{S}\mathbf{c}.$$
(11)

A. Similarity Transformation

Our solution is generic in the sense that it is applicable to any subclass of the affine family. The case that shows the most potential for biomedical segmentation problems is the new formulation and closed-form solution that we provide for the similarity transformation. In Figure 1 (top), we illustrate how prior knowledge improves robustness in a segmentation setting, where we compare the affine and similarity transformation. We see that similarity-based shape-priors allow for a substantial improvement over the affine transformation of [14]. We also tested the robustness of the similarity prior on simulated data where the gold standard is known (Figure 1, bottom) including an image corrupted by Gaussian white noise with SNR=0.44dB. The 19 rod-shaped cells are arranged in clumps, which makes the segmentation more challenging. The computed Jaccard indices (J) are reported in Table II. While our experiments involved quadratic B-splines, we like to point out that our framework is applicable to splines of any order.

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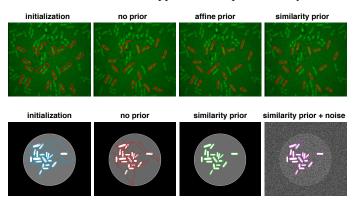


Fig. 1. Segmentation of rod-shaped yeast cells [26] (real data, top; simulated data, bottom). Several snakes are initialized (left) and an image-energy term is optimized with and without prior (affine and similarity). The shape prior corresponds to an approximate rod-shape. For the simulated data the gold standard is known and the segmentation results are measured with the Jaccard index (see Table II).

	initialization	no prior	similarity	similarity + noise
J	0.61 ± 0.17	0.69 ± 0.25	0.98 ± 0.4	0.93 ± 0.14

TABLE II MEAN JACCARD INDICES ON SIMULATED DATA

VII. CONCLUSION AND SUMMARY

We provide an explicit closed-form formulation to compute the minimal distance between an arbitrary query curve and a vector space defined by a reference. Our solution is generically characterized for landmark-based spline curves as a projection operator once the basis of the vector space is defined. This allows us to compute the continuous-domain distance as a fast matrix-vector operation. It can be used to efficiently characterize shape priors for landmark-based segmentation models. As application and additional contribution we provide a new direct formulation and implementation of the similarity transform, and we show how it robustifies segmentation algorithms by the integration of prior knowledge. The spline-based solution has the additional advantage that the proposed construction can also be applied to curves that are defined by a set of discrete points or landmarks, by simply interpolating them with a linear B-spline. Our framework can be extended to 3D tensor-product spline surfaces [27] by noting that the inner product between spline surfaces can also be expressed as a matrix-vector multiplication.

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