

Modeling capillary forces for large displacements

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Originally applied to the accurate, passive positioning of submillimetric devices, recent works proved capillary self-alignment as effective also for larger components and relatively large initial offsets. In this paper we describe an analytic quasi-static model of 1D capillary restoring forces that generalizes existing geometrical models and extends the validity to large displacements from equilibrium. The piece-wise nature of the model accounts for contact line unpinning singularities ensuing from large perturbations of the liquid meniscus and dewetting of the bounding surfaces. The superior accuracy of the generalized model across the extended displacement range, and particularly beyond the elastic regime as compared to purely elastic models, is supported by finite element simulations and recent experimental evidence. Limits of the model are discussed in relation to the aspect ratio of the meniscus, contact angle hysteresis, tilting and self-alignment dynamics.

I. INTRODUCTION

Liquid bridges connecting adjacent surfaces^{1,2} find extensive use in assembly³ and precision engineering⁴. A common example is represented by a liquid droplet bridging a flat (*e.g.* surface-mount⁵⁻⁷) component onto a stationary bottom surface. The position of the droplet—and hence that of the floating component—can be constrained by patterning a receptor site onto the substrate⁸. A single state of globally minimal energy exists for this capillary system⁹, provided that the surface of the component matches in shape and size that of the bottom site and that the volume of the droplet is sufficiently small to avoid tilting^{10,11}. In this equilibrium state the component stands parallel to the substrate and its edges are aligned to those of the site⁹. Upon formation of the vertical liquid bridge, capillary forces^{9,12} and torques^{9,13,14} act on the component. Capillary self-alignment refers to the motion of the component towards the absorbing state across an initial lateral offset. The same capillary forces tend to restore the system into the equilibrium state against perturbations and displacements⁸. Self-recovery of rest position and intrinsic mechanical compliance sparked interest in droplet-based capillary systems for relevant technological applications, such as conformal joints¹⁵⁻¹⁷, compliant handling⁴, precise registration of components^{18,19} and self-assembly⁸. Thereby the focus has mainly been on sub-millimetric components actuated by droplets of similar size, and correspondingly on displacements from equilibrium of relatively small magnitude. Elastic models accurately capture the response of the capillary system to such small lateral displacements^{9,12,20-22}. In this type of models the restoring capillary forces arise exclusively from the shear deformation of liquid interfaces pinned to bounding solid surfaces. Recently however capillary self-alignment was successfully

demonstrated also for centimeter-sized components^{7,23} across relatively large lateral offsets^{24,25}. Accounting for such evidence prompts an expansion of the reach of purely elastic models through wetting arguments.

In this paper we present a generalized quasi-static model of lateral capillary restoring forces valid for a significantly extended range of relative component displacements as compared to elastic models. By accounting for both liquid meniscus' partial wetting of solid surfaces (earlier attempted^{26,27}) and limited angle hysteresis over edges, the model portrays more accurately the behavior of finitely-deformable solid/liquid interfaces. For displacements larger than the elastic limit, we show that this behavior is distinctively characterized by the unpinning of triple contact lines. These wetting discontinuities are integral to the presented model, and supported by recent experimental evidence^{24,25}. We claim for the first time that the discontinuities divide the capillary response of the meniscus into three sequential regimes and pose the physical justification of the piece-wise nature of the model. The proposed model coincides with the purely elastic one for small displacements, and it describes the system with significantly better accuracy otherwise. It thus bridges the gap with abstract geometrical models²⁶ which tend to hold in the domain of large displacements.

An intuitive formulation of the model and its finite element simulation are presented respectively in Sect. II A and II B. Comparative results are illustrated in Sect. III, followed by a discussion of experimental support and limitations of the model (Sect. IV), and by conclusions (Sect. V). Full derivation of the model is described in the Appendix.

II. MODEL FORMULATION

A. Analytical model

We consider the system geometry sketched in figure 1. We refer to the solid bounding objects as *pads*, and to

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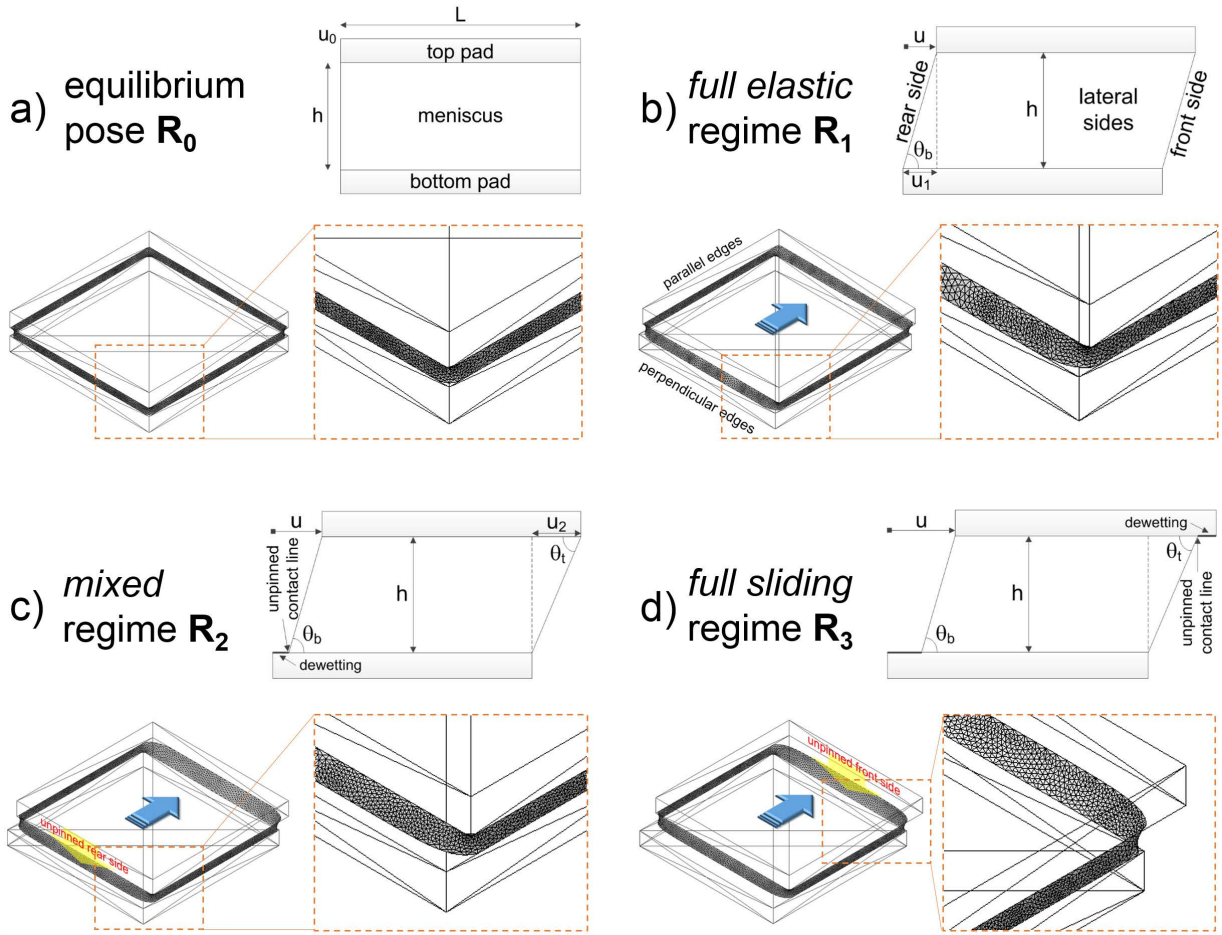


FIG. 1. Geometrical sketches (upper rows, not to scale) and SE snapshots with inset views (lower rows, $L = 1$ mm, $h = 50$ μ m) of sequential regimes R_j with $0 < \theta_t < \theta_b < \pi/2$. a) Global equilibrium, b) *full elastic* regime, c) *mixed* regime, d) *full sliding* regime. During capillary self-alignment the regimes are traversed in the reverse order with respect to model derivation.

the liquid bridge interchangeably as *meniscus*. Top (t) and bottom (b) pads have the same square shape of side-length L . The meniscus has constant volume V , density ρ , surface tension γ and height or *gap* h . Starting from the equilibrium position $u_0 = 0$ (figure 1a), a quasi-static horizontal displacement $u > u_0$ of the top relative to the bottom pad is imposed along a main orthogonal direction (figure 1b). Null relative tilt of the top pad is assumed for all u values considered. *Lateral*, *front* and *rear* sides of the meniscus, and *parallel* and *perpendicular* edges of the pads, are defined by their respectively parallel or perpendicular orientation with the direction of deformation (refer to figure 1b). The shearing perturbation u induce an asymmetrical deformation of the meniscus. The model describes the capillary response of the system to increasing deformations.

The following simplifying model assumptions are used:

1. *quasi-static equilibrium*, i.e. the system is originally in global equilibrium and arbitrarily close to local equilibrium in every perturbed configuration. Inertial and viscous effects are therefore neglected by

assuming $We \ll 1$ and $Ca \ll 1$, respectively;

2. *constant gap* $h(u) = h_0 = h$, and smaller than the capillary length $L_c = \sqrt{\gamma/\rho g}$ (i.e. $Bo \ll 1$) to neglect gravitational effects;
3. *ideally straight surfaces* of meniscus sides, including negligible weight of the top pad;
4. *ideal smoothness and chemical homogeneity of solid surfaces*, i.e. null contact angle hysteresis except along edges, and smooth unpinning of triple contact lines upon dewetting;
5. *no liquid overflow* beyond pad edges.

Given the previous hypotheses, which define the quasi-static model framework, contact angles θ_* can be defined everywhere on each solid surface (except over discontinuities such as edges) by the corresponding Young-Dupr  equation²⁸:

$$\gamma_{sv}^* - \gamma_{sl}^* = \gamma \cos \theta_* \quad (1)$$

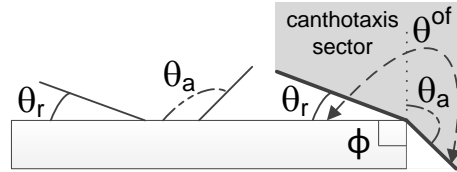
where the pedexes s, l, v refer to solid, liquid and vapor phases, respectively, and $*$ stands for t and b . Top and bottom pads are *partially* wetting. They have differing interfacial energies γ_{sl}^* and γ_{sv}^* for generality, and all its sides have the same surface energies. Given the contact angles $\theta_b \neq \theta_t$ (with $0 < \theta_* < \pi/2$), we define $\theta_{\min} = \min(\theta_t, \theta_b)$ and $\theta_{\max} = \max(\theta_t, \theta_b)$.

Upon relative displacement $u > 0$ of the pads the meniscus deforms to accomodate the shear stress. The capillary reaction against the perturbation is mainly exerted through the front and rear sides of the meniscus. For increasing values of u , the reaction assumes one of two sequential types depending on the degree of meniscus deformation. For each of the perpendicular sides of the meniscus, the transition between the two types of reaction is signaled by the unpinning of one contact line. At pad level, the contact line that undergoes unpinning is specifically the one on the perpendicular edge subtending the smallest edge angle. The opposite edge bears no unpinning since overflow is geometrically avoided according to hypothesis 5 (and as detailed below). The *elastic* reaction takes place before this discontinuity. In the elastic response the sides stretch their surfaces and incline forward due to edge angle hysteresis. Over the edges of the pads the contact lines work like hinges maintaining their position fixed. Unpinning is prompted by reaching the *receding* value of the contact angle, here coinciding by assumption with θ_* . Beyond this point, the shear deformation of the meniscus is accomodated by its unpinned side(s) by sliding the unpinned contact line across the surface of the pad. In this *sliding* response the surface area and inclination of the unpinned side(s) remain constant.

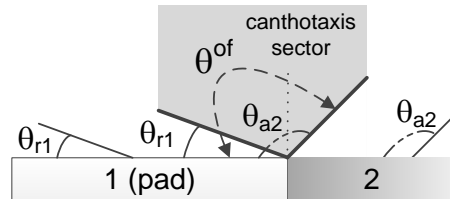
The complete response of the meniscus as function of the relative displacement u of the pads is thus divided into three sequential regimes R_j . In the first regime R_1 (*full elastic*, figure 1b), both perpendicular sides of the meniscus enact elastic response and have the same inclination; in the second regime R_2 (*mixed*, figure 1c), the perpendicular sides enact either responses; in the third and last regime R_3 (*full sliding*, figures 1d) both perpendicular sides are sliding. The separation between regimes is intrinsically set by the unpinning discontinuities. The discontinuities tend to happen for the same u instead of sequentially—*i.e.* the second regime disappears—in the limit of equal surface energies of the pads. For each of the perpendicular sides, the elastic and sliding force components have respectively the form (see Appendix) $F_{el} = \gamma L \frac{u}{\sqrt{h^2+u^2}}$ and $F_{sl} = \gamma L \cos \theta_*$. Hence the capillary restoring force $F(u)$ is described by the following piece-wise equation:

$$F(u) = \begin{cases} -2\gamma L \frac{u}{\sqrt{h^2+u^2}} & 0 < u < u_1 \\ -\gamma L (\cos \theta_{\max} + \frac{u}{\sqrt{h^2+u^2}}) & u_1 < u < u_2 \\ -\gamma L (\cos \theta_{\max} + \cos \theta_{\min}) & u_2 < u < u_{\max} \end{cases} \quad (2)$$

where u_{\max} is defined in Appendix and relates u to L



(a) Edge confinement by topographical step.



(b) Edge confinement by wetting contrast.

FIG. 2. Meniscus confinements by edge angle hysteresis for $\theta_r \neq \theta_a$. For case (a) developed in the text the quasi-static model assumes $\theta_r = \theta_a = \theta_*$ and the canthotaxis spans an angular sector of $\pi - \phi$ (see eq. 4). Case (b) is considered in the Appendix.

rather than to h . The domain boundary values:

$$u_1 = h \cot \theta_{\max} \text{ and } u_2 = h \cot \theta_{\min} \quad (3)$$

can be obtained by imposing force continuity between adjacent regimes (smooth transitions, hypothesis 4). They satisfy the geometric interpretation shown in figures 1b and 1c, respectively.

Overflow (*of*) avoidance (hypothesis 5) sets additional constraints on u and θ_* . The liquid meniscus is constrained within the edges of top and bottom pads. Along the pad edges the contact line is pinned and the angles formed by the meniscus with the surfaces of the pads (*i.e.* edge angles) can assume a multiplicity of values. Edge angle hysteresis is measured by the range of angles coexisting over the same contact line position (*i.e.* the canthotaxis sector²⁸, figure 2). While the lower limit of the edge angle coincides with the receding contact angle θ_r^* , the higher limit θ^{of} is determined by case-specific boundary conditions. Exceeding the higher limit of edge angles prompts overflow of the liquid bridge beyond the edges of the pads. This evenience represents a major failure mode for capillary self-alignment⁸—and coincides with the ultimate limit of validity of the model. Meniscus confinement can be enforced chemically or topographically. In the former case, surface chemistry is tailored to make the pads more wettable than the surrounding areas²³, and θ^{of} is

set by the advancing contact angle of the surrounding area (figure 2(b)). In latter case (figure 2(a)) the canthotaxis sector is extended by edge confinement^{29,30}, and θ^{of} is imposed by the Gibbs' criterion¹²:

$$\theta^{of} = \theta_* + \pi - \phi \quad (4)$$

ϕ being the slope angle of the pad's edge. Accordingly, overflow takes place when the edge angle reaches the value of the advancing contact angle with respect to the surface of the pad's sloped side. In the following we consider and model the case of topographical confinement with vertical pad sides (*i.e.* $\phi = \pi/2$, figure 2a). The analytical model for the chemical confinement case can be similarly derived, and is described in the Appendix.

Consistency with the Gibbs' criterion (eq. 4) to avoid meniscus overflow imposes coupled constraints on the values of θ_* with respect to eq. 3. Specifically, transitions between R_1 and R_2 and between R_2 and R_3 can take place without overflow for corresponding u_i only if:

$$\begin{cases} \theta_{\min} \geq \pi/2 - \theta_{\max} & R_1 \text{ to } R_2 \\ \theta_{\max} \geq \pi/2 - \theta_{\min} & R_2 \text{ to } R_3 \end{cases} \quad (5)$$

These model boundary conditions prescribe a mutual relation between the surface energies of the pads for physical consistency. Hence overflow avoidance implies that the full sequence of reaction regimes be conditional to the coupled choice of θ_* . The case of perfect pad wettability, normally assumed in elastic models, is trivially excluded in presence of edge confinement, and only possible for chemical confinement. Liquid overflow due to enhanced wettability of pads with topographical edge confinement was recently evidenced in self-alignment experiments²⁵.

B. Finite element model

The capillary system was simulated by a quasi-static finite element numerical model in `Surface Evolver`³¹ (SE) (figure 1). Water^{7,19,23} ($\gamma = 72$ mN/m, $\rho = 1000$ kg/m³, $L_c = 2.7$ mm) was chosen for the liquid bridge constrained within square pads of $L = 1$ mm ($Bo = \rho g L^2 / \gamma = 0.14$), thickness of 125 μm and density of 1380 kg/m³. Domain constraints were used to confine the triple contact lines of the meniscus strictly in the planes and within the perimeters of the pads. The weight of the top pad (173 μg) had negligible impact on the model. The simulations proceeded by the displacement of the top pad within the range $u_0 < u < u_{\text{lim}}$ in steps of 1 μm . $u_{\text{max}} < u_{\text{lim}} < L$ was chosen to check the limits of validity of the model within a physically realistic range of u . Values of $h|_{u_0} = 25, 50$ and 100 μm were simulated using corresponding values of liquid volume $V = 25, 50$ and 100 nL. They correspond to h/L aspect ratios (AR) of 1/40, 1/20 and 1/10, respectively, spanning the AR range used in applications. Several combinations of θ_b and θ_t values were simulated for each AR, with $\theta_* \subset \{0^\circ, 10^\circ, 35^\circ, 50^\circ, 65^\circ, 80^\circ\}$. The case of perfect

wetting ($\theta_* = 0^\circ$) was considered, in spite of its inconsistency with edge confinement (eq. 5), as reference for the purely elastic scenario. u_{max} was defined for each θ_* pair and h values according to eq. 12 (see Appendix). Mesh refinement and geometry evolution made repeated use of the built-in Hessian of the energy function. Energy convergence was assumed to be attained at its fifth significant digit for all simulated configurations. The SE model complied with all assumptions stated in Sect. II A, except for the straight surface of the sides of the meniscus (see figure 1) and the constancy of $h(u)$. After every update of u , $h(u)$ was updated through a local-search routine based on Newton's method to keep the system in local equilibrium¹⁵. The non-constancy of $h(u)$ was implemented in SE for physical consistency with 1) the time scale separation due to the dominance of vertical over lateral capillary forces for this system²⁶, 2) the tendency of the liquid bridge to assume the geometry locally closest to a section of a sphere^{15,28}, and 3) conservation of the meniscus volume, which upon contact line unpinning(s) induces an increase of h to partially compensate the decrease of wet pad surface(s). After setting $h(u)$, the lateral capillary force $F(u)$ was computed by the method of virtual works³² implemented using central finite differences.

III. RESULTS

SE simulations evidenced the continuity and monotonicity of $E(u)$ and $h(u)$, and their sensitivity to the energy of the solid surfaces as lumped in the θ_* pairs (see figures 3(a) and 3(b), respectively, for $h_0 = 25$ μm). Higher surface energies (*i.e.* lower θ_*) yield higher total system energies and energy gradients (*i.e.* forces, shown below) as well as smaller variations in $h(u)$. As for the latter, values of $\theta_* > 0$ induce an increase of $h(u)$, whereas perfect wetting ($\theta_* = 0^\circ$) causes a decrease.

An instance of the capillary forces predicted by the analytical and SE models is shown in figure 4. For this case ($h = 25$ μm , $\theta_b = 65^\circ$ and $\theta_t = 50^\circ$) all regimes are encountered. The sequential unpinning discontinuities are seen to coincide with the sharp beginning of linear decrease of the wet areas A_* of the pads. The accuracy of the match between proposed and SE model across all range of u can be appreciated—particularly with respect to the purely elastic model represented by $F_1(u)$. The small deviations are attributed to the non-constancy of $h(u)$ and to the hysteresis of edge angles simulated in SE. As the gap increases with u the lateral sides of the meniscus may deform and curve, contributing elastically to the total energy and the ensuing capillary force in ways not accounted for analytically. The edge angle hysteresis in SE is larger than what considered in the analytical counterpart. Such hysteresis retards the unpinning of the contact lines. Consequently the u_i predicted by the analytical model tend to be smaller than the simulated ones—a relatively small error over θ_* may produce

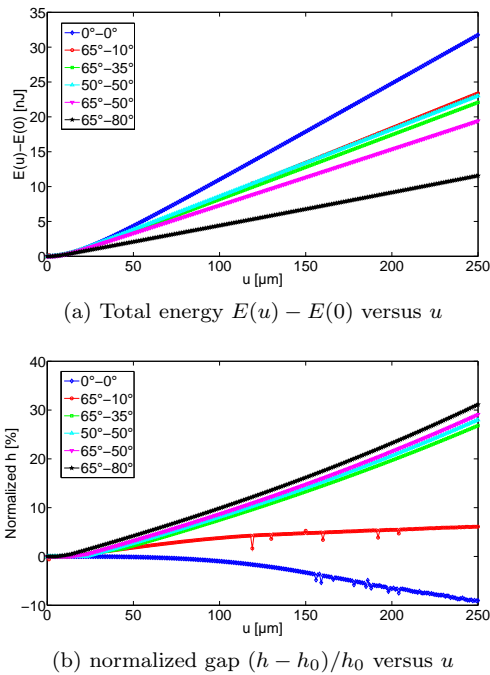


FIG. 3. SE simulations for $h_0 = 25 \mu\text{m}$ ($\text{AR} = 1/40$) parameterized by $\theta_b - \theta_t$ pairs.

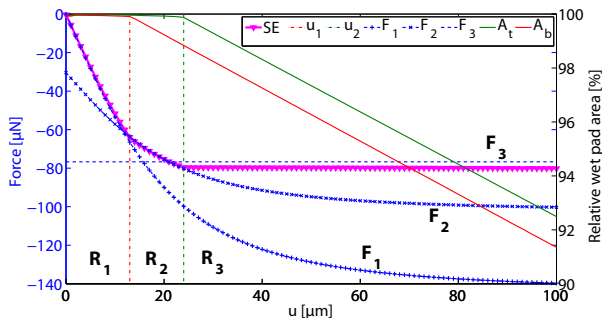


FIG. 4. SE and analytical predictions of $F(u)$ versus u for $h_0 = 25 \mu\text{m}$ ($\text{AR} = 1/40$) with $\theta_b = 65^\circ$ and $\theta_t = 50^\circ$. Vertical lines correspond to u_i and signal contact line unpinning from pad edges by the decrease in wet pad area (A_*). Analytic forces F_j , holding in respective domains R_j , are shown across the entire domain of u for comparison. Relative error for $F(u = u_{\max})$ is 4.3%.

large effects given that $\frac{\partial u_i(h, \theta)}{\partial \theta} = -\frac{h}{\sin^2(\theta)}$. The force predicted, particularly for large displacements, is hence cumulatively affected by both unaccounted effects. For instance, for the case of figure 4 the analytical values of $u_1 = 11.7$ and $u_2 = 21 \mu\text{m}$ compares with $u_1 = 13$ and $u_2 = 24 \mu\text{m}$ obtained from SE, leading to a relative error of about 4% over the value of $F_3(u_{\max})$. Figure 5 further exemplifies the verification of the model for other cases with $h = 25 \mu\text{m}$ and significant combinations of θ_* values. The error over $F_3(u)$ remains small and bounded for larger θ_* , while that of the purely elastic model increases.

IV. DISCUSSION

As shown by the relative errors over $F(u_{\max}(\theta_*, h))$ summarized in Table I, for larger AR values the discrepancy between analytical and SE models increases, and several effects undermine the validity of the former. As mentioned in the previous section, SE simulations show that for receding contact lines the edge angle hysteresis tend to slightly deviate from the analytical description. This may be attributed to the finite length of the pads in the direction perpendicular to u , since the ensuing curvature of the contact line is not considered in the derivation of Gibbs' criterion¹². Moreover, the hypothesis of straight meniscus sides holds fairly well in SE except expectedly at the pads' corners (figures 1b–1c). This is permitted by and consistent with the updating of $h(u)$ by time scale separation (see Sect. II B) and, importantly, the unpinning of the contact lines upon reaching the limits of the elastic responses. Contact line unpinning allows preserving the inclination of the unpinned meniscus sides independently of further increments of u —in contrast to purely elastic and perfect wetting cases. Yet the curvature and deformation of the sides of the meniscus becomes evidently less negligible as u and AR increase. As a result, contact line unpinning becomes less sharp and resembles unzipping, as it takes place not at once but rather gradually, starting from the extremities of the edges toward the center. This fuzzifies the boundaries between the regimes, since the u_i can not be univocally identified. Therefore the model tends to loose accuracy for increasing values of AR besides of u .

It can additionally be argued by the Hauksbee principle²⁸ that for relative displacements of the order of u_{\max} the condition of strictly horizontal translation of the top pad (see Section II A) may break down, as tilting of the same may intervene to accommodate the relevant perturbation of the meniscus. Together with meniscus overflow, tilting is reportedly a significant failure mode in capillary self-alignment⁸. In presence of tilting the self-aligning process is compromised because the capillary forces are opposed by friction between solid surfaces^{11,18,23}. Moreover, the tilt mode provides limited restoring torque⁹, and the system may effectively escape from the state of local energy minimum only through external agitation^{11,22}. The incidence of tilting can be lessened and even avoided by optimizing the volume^{10,23} and wetting²⁴ of the liquid meniscus—as confirmed by the experimental evidence provided below and, incidentally, by the disappearance of pad tilt during evaporation of the meniscus¹⁹.

The models, consistently with earlier instances, follow the progressive displacement of the capillary system from its state of global equilibrium opposed by restoring forces. Hereby the work of displacement is used to stretch the meniscus and eventually dewet solid surfaces. Through this approach, our extended model allows to predict the parabolic regime we earlier reported in experimental high-resolution tracking of capillary self-alignment dynamics²⁴. The parabolic regime ensues from

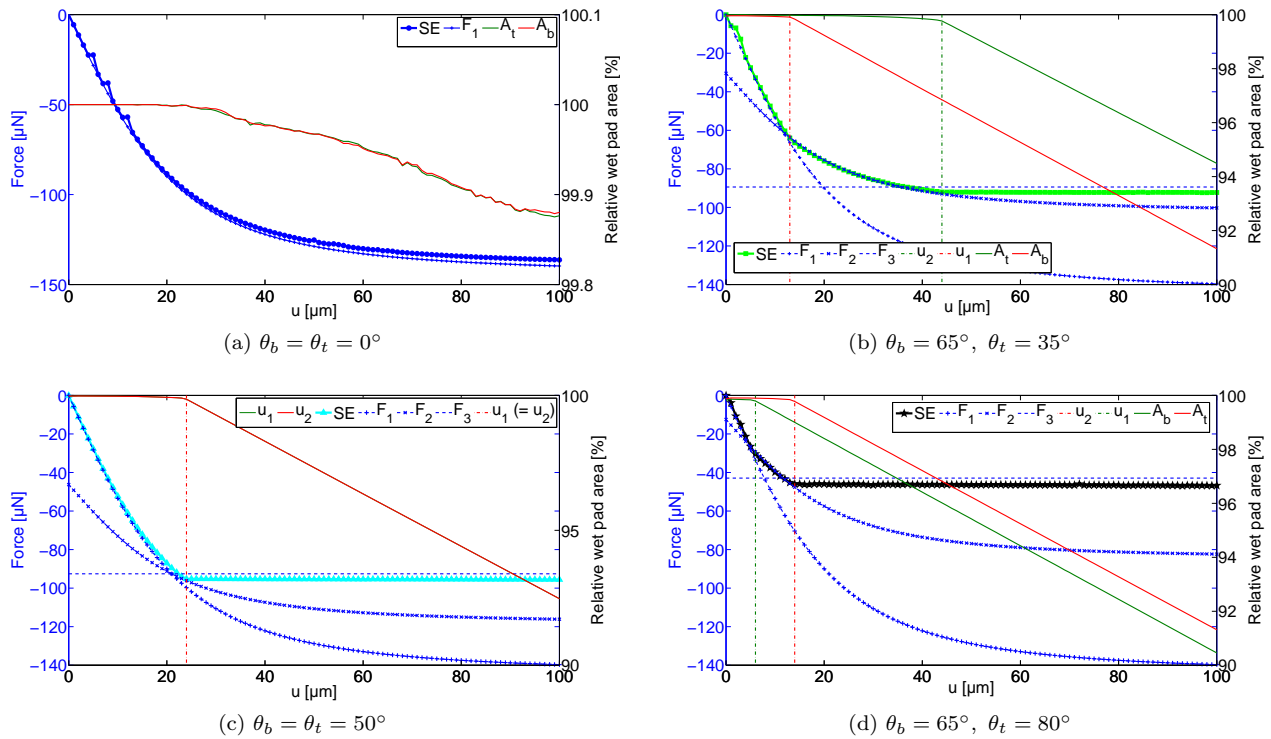


FIG. 5. Capillary forces predicted for $h = 25 \mu\text{m}$ ($AR = 1/40$) and various combinations of θ_* . (a) Perfect wetting (no contact line unpinning), (b) the three sequential regimes, first unpinning on bottom pad, (c) absence of second regime for $\theta_b = \theta_t$ ($u_1 = u_2 = u_d$, $F_1(u_d) = F_2(u_d) = F_3(u_d)$), (d) the three sequential regimes, first unpinning on top pad.

TABLE I. Relative errors for $F(u_{\max}(\theta_*, h))^a$

| $\theta_b - \theta_t$ | $h_0 = 25 \mu\text{m}$ | $h_0 = 50 \mu\text{m}$ | $h_0 = 100 \mu\text{m}$ |
|-----------------------|------------------------|------------------------|-------------------------|
| $0^\circ - 0^\circ$ | 2.7% | 4.2% | 7.4% |
| $65^\circ - 10^\circ$ | 2.8% | 5.5% | 16% |
| $65^\circ - 35^\circ$ | 3.1% | 4.3% | 7% |
| $50^\circ - 50^\circ$ | 3.2% | 5.4% | 3.7% |
| $65^\circ - 50^\circ$ | 4.3% | 7.3% | 7.4% |
| $65^\circ - 80^\circ$ | 8.6% | 14.7% | 17.1% |

^a See eq. 12 in the Appendix for the numerical values of u_{\max} .

a constant acceleration imparted by the relaxing liquid bridge to the top pad. The constant acceleration is consistent with the constant restoring capillary force predicted by eq. 2 for large relative displacements.

However, in its present form the proposed model can not frame the actual experimental dynamics of capillary self-alignment²⁴. This can be illustrated through sequential snapshots from a high-speed recording of a capillary self-alignment experiment, shown in figure 6. In this realization a transparent top pad (polyethylene naphthalate, water contact angle $\theta_t = 65^\circ$) was controllably dropped onto a thin water layer ($h = 125 \mu\text{m}$) pre-coated over the entire bottom receptor site (silicon dioxide surface, $\theta_b = 10^\circ$) except for its corners⁸ (figure 6(a)). Chemical edge confinement was used as the

bottom pad was surrounded by non-wetting areas with water contact angle $\theta_{of} = 120^\circ$ ²³. Edge confinement is exemplified elsewhere²⁵. In spite of the optimized pre-coating²³, conformal coverage of both pads by the liquid bridge is achieved along the self-alignment process only after a sequence of *dynamic* regimes. In the initial transient wetting regime²⁴ the meniscus deforms and spreads until its contact lines pin on the edges of the pads³³ (figure 6(b)). Only then can the capillary forces exerted by the meniscus be applied to the pads, causing their relative translation. Henceforth the self-aligning motion starts and proceeds along a predictable spatio-temporal trajectory across the aforementioned parabolic regime (figure 6(c)) and subsequent underdamped harmonic oscillations²⁴ (figure 6(e)). In case of partial wetting, it is only after crossing the receptor site for the first time that the surfaces of both pads are fully wet by the liquid bridge (figure 6(d)). After transient wetting, the front side of the meniscus was pinned throughout the process on both pads. Hence the mixed R_2 regime predicted by the model extended from the inception of the translational motion of the top pad through the constant acceleration regime (figure 6(c)) till first crossing of the target position. The rear side of the meniscus remained unpinned, as expected from the model. Fully elastic regime R_1 appeared during all subsequent overshoots conducting the oscillating top pad to the final equilibrium position in accurate alignment with the bottom site (figure 6(f)).

Notably, in our consistently repeatable experiments²⁵ no tilt of the top pad was recorded even for very large initial offsets²⁵ (1.5 mm in the illustrated instance, *i.e.* about 30 % of L)—*i.e.* also for offsets larger than the limiting value of u_{max} correspondingly estimated in the model. This evidence further suggests that the incidence of tilt is also significantly dependent on the contingent dynamics through which the rest position is approached.

Importantly, during the actual dynamics of self-alignment the reaction regimes R_j described by the proposed model are traversed in a different, generally reverse temporal sequence, so that R_0 represents the absorbing state of the dynamics instead of the initial state as assumed in the modeling. A comprehensive dynamic model of the process would therefore need to consider advancing rather than receding contact angles (dependent on line velocity³⁴) in the sliding regimes—together with inertia, fluid flow and viscosity²⁰ and possibly energy dissipation at the moving contact lines³⁴. The proposed model provides an extended quasi-static scenario toward the development of such as yet elusive^{20,24} description.

V. CONCLUSIONS

We introduced an analytic description of restoring capillary forces accounting for an extended range of lateral perturbations of a confined liquid bridge. The proposed model provides a simple and accurate description of the capillary system by integrating the effect of partial wetting of the bounding solid surfaces by the liquid bridge. Thanks to this, important physical and geometrical parameters of the system—such as surface energies, pad dimensions and type of edge confinement against liquid overflow—are additionally accounted for, which further distinguishes the present from earlier models. The analytic description is supported by physically consistent finite element simulations. The numerical simulations also highlight the physical limits of validity of the model, coherently with its stated assumptions and boundary conditions. Predictions concerning the effect of surface energies on meniscus overflow²⁵ and transiently constant acceleration of the top pad during capillary self-alignment²⁴ are supported by recent experimental evidence.

The model bridges the domain of small displacements of purely elastic models with that of large displacements. The latter is captured by computationally efficient models based on two-dimensional convolutions of the shapes of the bounding pads²⁶ (figure 7). The analytical formulation of the model, hereby developed for identical square shapes of the pads, can be trivially adapted to rectangular pads. A generalization for polygonal pad shapes of higher order may also be conceived²¹.

Experimental benchmarking of the analytical force model may be envisioned, for instance through the adaptation of an earlier setup for lateral capillary force measurement¹² which could notably impose a strictly horizontal displacement of the top pad.

Pivotal to the formulation of the model is the energetic description of contact line unpinning and subsequent sliding. Under model assumptions, this has the simple form derived from the Young-Dupré equation. A similar formulation could be adopted to describe more realistic scenarios involving finite contact angle hysteresis, provided substitutive descriptions of the energy and force balance at the triple contact lines³⁴.

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APPENDIX: MODEL DERIVATION

In this section we present the full derivation of the analytical model presented in the main text.

With reference to the geometry sketched in figure 1, we subsume the partial wetting of the surfaces of the pads in considering $0 < \theta_t < \theta_b < \pi/2$, yielding $u_1 = h \cot \theta_b$ and $u_2 = h \cot \theta_t$ according to eq. 3. The alternative case of $0 < \theta_b < \theta_t < \pi/2$ differs only in the sequence of contact line unpinning over the pads, its formulation being the same upon mutual replacement of t with b . Figure 8 provides the reference geometries for the estimation of the updated values h' and h'' of $h(u)$ upon transitions between regimes under conservation of meniscus volume.

The following holds under model assumptions:

1. the surface energy $E(u)$ coincides with the total free energy of the capillary system, and it is invariant under swapping of the surface energies of pads;
2. partial wettability of the surfaces of the pads determines the existence of finite relative displacements u_i causing the sequential unpinning of the extremal contact lines (*i.e.* those whose vertical projection lies outside the opposite pads' surface).

The analytical formulation of the model proceeds from the calculation of the energy $E_j(u)$ of the system²⁶ for each regime R_j determined by sequential unpinning discontinuities. The lateral capillary force $F_j(u)$ and stiffness $k_j(u)$ of the meniscus are computed by subsequent partial derivatives over u of the energy function.

The energy of the global equilibrium state R_0 is (up to an additional arbitrary constant):

$$E_0 = E(u_0 = 0) = \underbrace{L^2(\gamma_{sl}^t + \gamma_{sl}^b)}_{\text{pads}} + \underbrace{4\frac{V}{L}\gamma}_{\text{meniscus}} \quad (6)$$

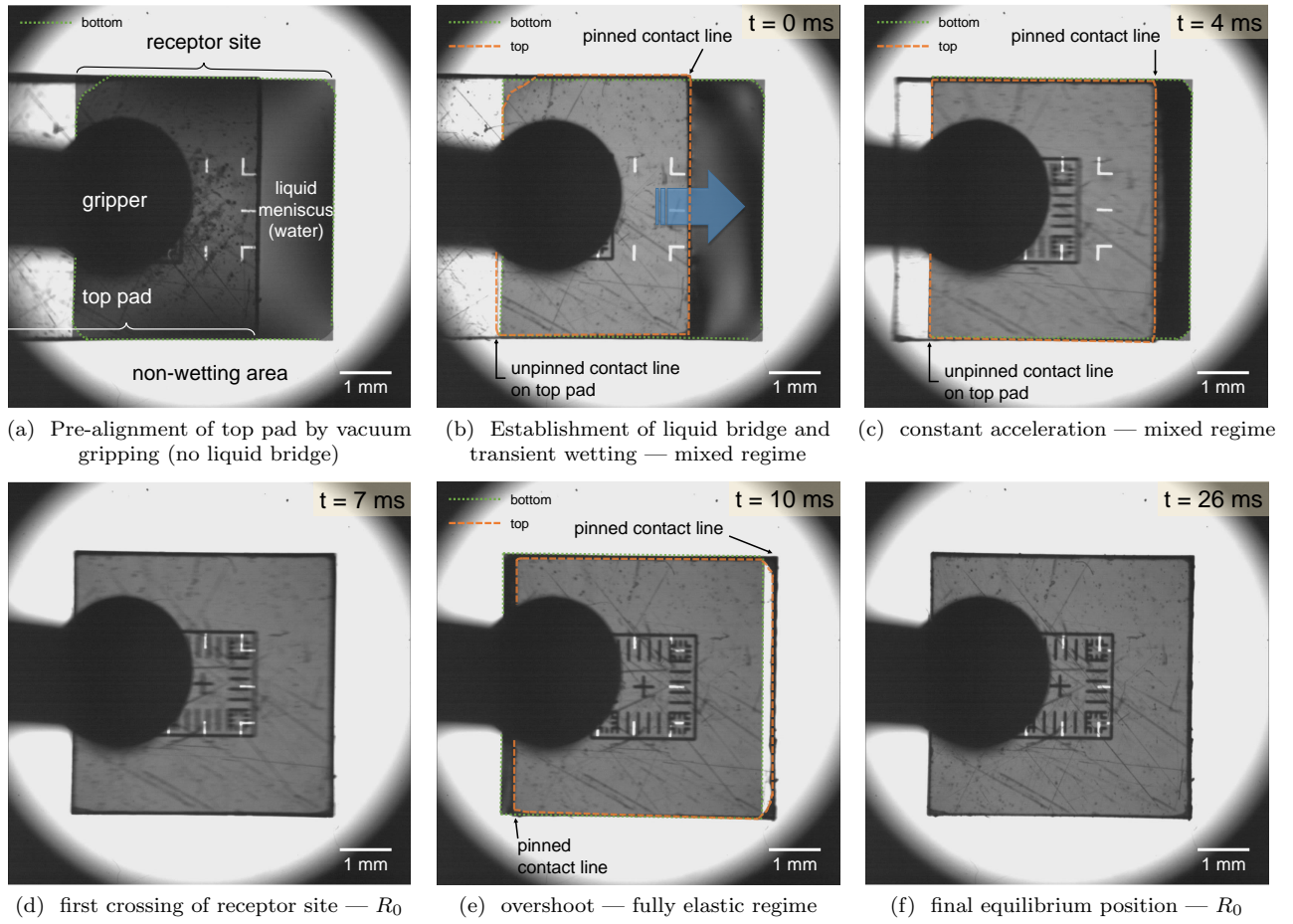


FIG. 6. Sequential snapshots from high-speed recording of a capillary self-alignment experiment. The transparent top square pad was released from a vacuum gripper onto a chemically patterned and shape-matching receptor site conformally pre-coated with water ($L = 5$ mm, $h = 125$ μ m (AR = 1/40), $\theta_t = 65^\circ$ and $\theta_b = 10^\circ$). Top and bottom contact lines are highlighted. Full video available in Supporting Information.

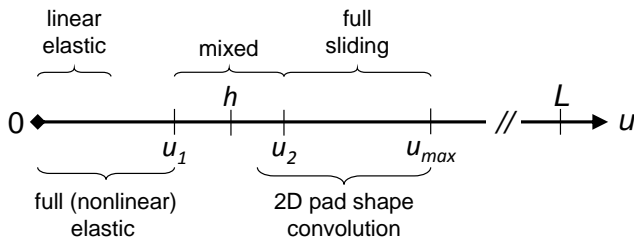


FIG. 7. Qualitative range of validity of capillary force models.

For the deformed states R_1 and R_2 :

$$\begin{aligned}
 E_1 &= E(0 \leq u \leq u_1) \\
 &= \underbrace{L^2(\gamma_{sl}^t + \gamma_{sl}^b)}_{\text{pads}} + \underbrace{2\frac{V}{L}\gamma}_{\text{lateral}} + \underbrace{2\gamma L\sqrt{h^2 + u^2}}_{\text{front \& rear}} \\
 &= E_0 - 2\frac{V}{L}\gamma + 2\gamma L\sqrt{h^2 + u^2}
 \end{aligned} \quad (7)$$

$$\begin{aligned}
 E_2 &= E(u_1 \leq u \leq u_2) \\
 &= \underbrace{L^2\gamma_{sl}^t}_{\text{top pad}} + \underbrace{L(u - u_1)\gamma_{sv}^b + L[L - (u - u_1)]\gamma_{sl}^b}_{\text{bottom pad}} \\
 &\quad + \underbrace{2\gamma\frac{V}{L}}_{\text{lateral}} + \underbrace{\gamma L\sqrt{h'^2 + u_1^2}}_{\text{rear}} + \underbrace{\gamma L\sqrt{h'^2 + u^2}}_{\text{front}} \\
 &= E_1(u_1) + \gamma L(\sqrt{h'^2 + u^2} - \sqrt{h'^2 + u_1^2}) \\
 &\quad + (\gamma_{sv}^b - \gamma_{sl}^b)L(u - u_1) \\
 &\cong \text{const} + \gamma L\sqrt{h^2 + u^2} + \gamma L(u - u_1)\cos(\theta_b)
 \end{aligned} \quad (8)$$

using eq. 1 and the following approximation for the constancy of h (see Figure 8(a)):

$$\begin{aligned}
 h' &= h\frac{L}{L - \frac{u - u_1}{2}} \\
 &= h\left(1 + \frac{u - u_1}{2L}\right) + o^2(u - u_1) \\
 &\cong h \text{ for } u \ll 2L + u_1 = 2L + h \cot \theta_b
 \end{aligned} \quad (9)$$

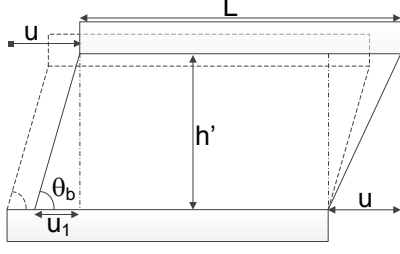
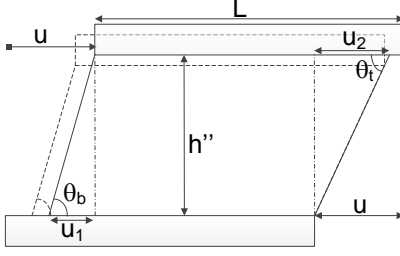
(a) Sketch for h' (b) Sketch for h''

FIG. 8. Sketches (not to scale) for geometrical estimation of h' and h'' under model assumptions upon transitions between adjacent regimes: (a) from R_1 to R_2 , (a) from R_2 to R_3 .

Similarly for R_3 :

$$\begin{aligned}
 E_3 &= E(u_2 \leq u < u_{\max}) \\
 &= \underbrace{2\frac{V}{L}\gamma}_{\text{lateral}} + \underbrace{\gamma L\sqrt{h''^2 + u_1^2}}_{\text{rear}} + \underbrace{\gamma L\sqrt{h''^2 + u_2^2}}_{\text{front}} \\
 &\quad + \underbrace{L(u - u_1)\gamma_{sv}^b + L[L - (u - u_1)]\gamma_{sl}^b}_{\text{bottom pad}} \\
 &\quad + \underbrace{L(u - u_2)\gamma_{sv}^t + L[L - (u - u_2)]\gamma_{sl}^t}_{\text{top pad}} \\
 &\cong E_2(u_2) + \gamma L(u - u_2)(\cos \theta_b + \cos \theta_t)
 \end{aligned} \tag{10}$$

using the approximation (see Figure 8(b)):

$$\begin{aligned}
 h'' &= h \frac{L}{L - (u - \frac{u_1 + u_2}{2})} \\
 &\cong h \text{ for } u \ll L + \frac{u_1 + u_2}{2} = L + \frac{h}{2}(\cot \theta_b + \cot \theta_t)
 \end{aligned} \tag{11}$$

Eq. 11, more stringent than eq. 9, sets the strict limit of validity of the model over u under the assumptions of constant V and h . This condition assumes and is consistent with choices of coupled pairs of θ_* satisfying the condition set by eq. 5 for overflow-less transition between adjacent capillary regimes. Eq. 11 defines $u_{\max}(\theta_*, h)$

and relates it to the pad size L rather than to h ($L \gg h$ in general) as in purely elastic models. Given $L = 1$ mm, h and θ_* , the relative errors in capillary force estimates between analytical and numerical models for each of the cases reported in Table I of the main text were evaluated for the corresponding value:

$$u_{\max} = \frac{1}{10} \left[L + \frac{h}{2} (\cot \theta_b + \cot \theta_t) \right] \tag{12}$$

From eqs. 7, 8 and 10 it follows respectively:

$$R_1 \begin{cases} F_1(u) &= -\frac{\partial E_1(u)}{\partial u} = -2\gamma L \frac{u}{\sqrt{h^2 + u^2}} \\ k_1(u) &= -\frac{\partial F_1(u)}{\partial u} = \frac{\partial^2 E_1(u)}{\partial u^2} \\ &= 2\gamma L \left(\frac{1}{\sqrt{h^2 + u^2}} - \frac{u^2}{(h^2 + u^2)^{\frac{3}{2}}} \right) \end{cases} \tag{13}$$

$$R_2 \begin{cases} F_2(u) &= -\frac{\partial E_2(u)}{\partial u} = -\gamma L \left(\frac{u}{\sqrt{h^2 + u^2}} + \cos \theta_b \right) \\ k_2(u) &= -\frac{\partial F_2(u)}{\partial u} = \frac{\partial^2 E_2(u)}{\partial u^2} \\ &= \gamma L \left(\frac{1}{\sqrt{h^2 + u^2}} - \frac{u^2}{(h^2 + u^2)^{\frac{3}{2}}} \right) \\ &= \frac{k_1(u)}{2} \end{cases} \tag{14}$$

$$R_3 \begin{cases} F_3(u) &= -\frac{\partial E_3(u)}{\partial u} = -\gamma L (\cos \theta_b + \cos \theta_t) \\ k_3(u) &= -\frac{\partial F_3(u)}{\partial u} = \frac{\partial^2 E_3(u)}{\partial u^2} \\ &= 0 \end{cases} \tag{15}$$

The formulation is consistent with energy and force continuity across adjacent domains, since $E_{i+1}(u_i) = E_i(u_i)$ and $F_{i+1}(u_i) = F_i(u_i)$ hold for all $i = 0, 1, 2$. Note that for $R_1|_{0 < u < h}$ the small displacement values $F_1 = -2\gamma L \frac{u}{h}$ and $k_1 = 2\gamma \frac{L}{h}$ of linear elastic models are recovered^{9,12,20,29}. Conversely, the absence of elastic work in R_3 is evidenced by the null constant value of k_3 . Also, $\theta_t \rightarrow \theta_b$ implies a singular domain for R_2 as $u_2 \rightarrow u_1$. Particularly, for the limiting case of full wetting of both pads—*i.e.* for $\theta_b = \theta_t = 0$ — $u_1 \rightarrow \infty$, *i.e.* the domain of R_1 extends indefinitely. The purely elastic regime is thus recovered, whereby partial dewetting of the surface of the pads is not possible. In this ideal condition further model convergence is given by $F_1|_{u \gg h} = F_3|_{\theta_b = \theta_t = 0}$. Plots of energy, gap and restoring force versus u for $AR = 1/20$ and $1/10$ ($h = 50$ and $100 \mu\text{m}$, respectively) are shown in figures 9 through 14—complementing those for $AR = 1/40$ presented in the main text.

Finally, by considering meniscus confinement within the pads by chemical contrast (figure 2(b)) rather than by topographical step, the formal derivation shown above can be adapted to account for the case of liquid bridge overflow²⁶. Overflow is here supposed to take place beyond the edge of the bottom pad onto an adjacent and less wettable surface (see figure 15). The case of overflow beyond the top pad is energetically equivalent. We assume that the two (pad and adjacent) surfaces are at

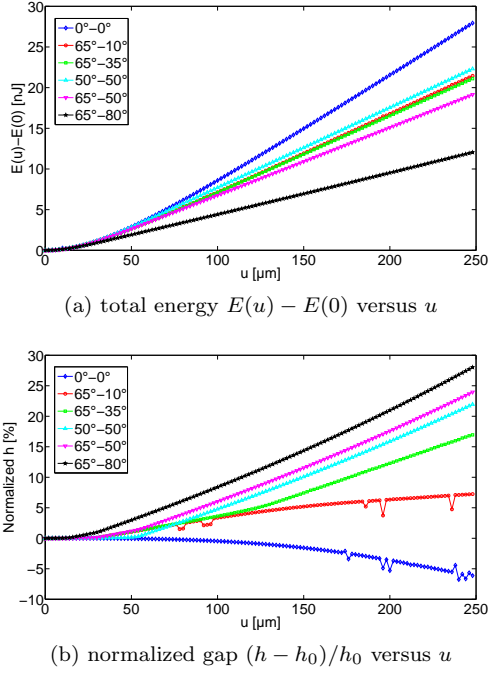


FIG. 9. SE simulations for $h_0 = 50 \mu\text{m}$ ($\text{AR} = 1/20$) parameterized by $\theta_b - \theta_t$ pairs.

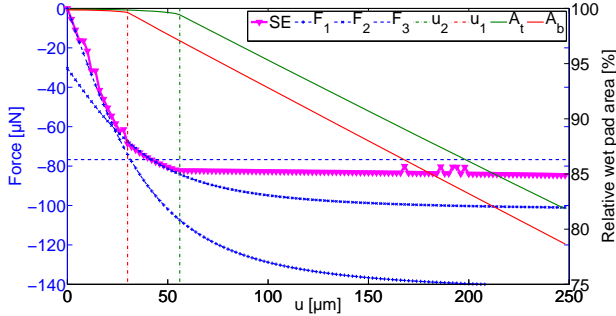


FIG. 10. SE simulation and analytical fit of $F(u)$ versus u for $h_0 = 50 \mu\text{m}$ ($\text{AR} = 1/20$) with $\theta_b = 65^\circ$ and $\theta_t = 50^\circ$. The relative error for $F(u = u_{\text{max}})$ is 7.4%.

the same level, and that the energetic barrier to overflow is only chemical in nature. For the less wettable surface the validity of a specific Young-Dupré equation is also assumed, yielding a contact angle $\theta_b^{of} > \pi/2 > \theta_b$. The overflow happens when the edge angle of the meniscus reaches the advancing value of the contact angle on the adjacent surface (hereby again assumed to coincide with its static value θ_b^{of}), prompting the unpinning of the contact line toward the adjacent surface. Unpinning takes place for $u \geq u_{of}$ and signals the transition to a regime akin to either the mixed (R_2^{of}) or the full sliding one (R_3^{of}). u_{of} can be either larger or smaller than u_1 , yet not larger than u_2 because in R_3 the inclinations of both perpendicular sides of the meniscus remain constant. For

the former case of $0 < u_{of} < u_1$ (fig. 15(a)):

$$R_2^{of} \begin{cases} F_2^{of}(u) &= -\frac{\partial E_2^{of}(u)}{\partial u} = -\gamma L \left(\frac{u}{\sqrt{h^2+u^2}} - \cos \theta_b^{of} \right) \\ k_2^{of}(u) &= -\frac{\partial F_2^{of}(u)}{\partial u} = \frac{\partial^2 E_2^{of}(u)}{\partial u^2} \\ &= \gamma L \left(\frac{1}{\sqrt{h^2+u^2}} - \frac{u^2}{(h^2+u^2)^{\frac{3}{2}}} \right) \\ &= \frac{k_1(u)}{2} \end{cases} \quad (16)$$

For the latter case of $u_1 < u_{of}$ (fig. 15(b)):

$$R_3^{of} \begin{cases} F_3^{of}(u) &= -\frac{\partial E_3^{of}(u)}{\partial u} = -\gamma L (\cos \theta_b - \cos \theta_b^{of}) \\ k_3^{of}(u) &= -\frac{\partial F_3^{of}(u)}{\partial u} = \frac{\partial^2 E_3^{of}(u)}{\partial u^2} \\ &= 0 \end{cases} \quad (17)$$

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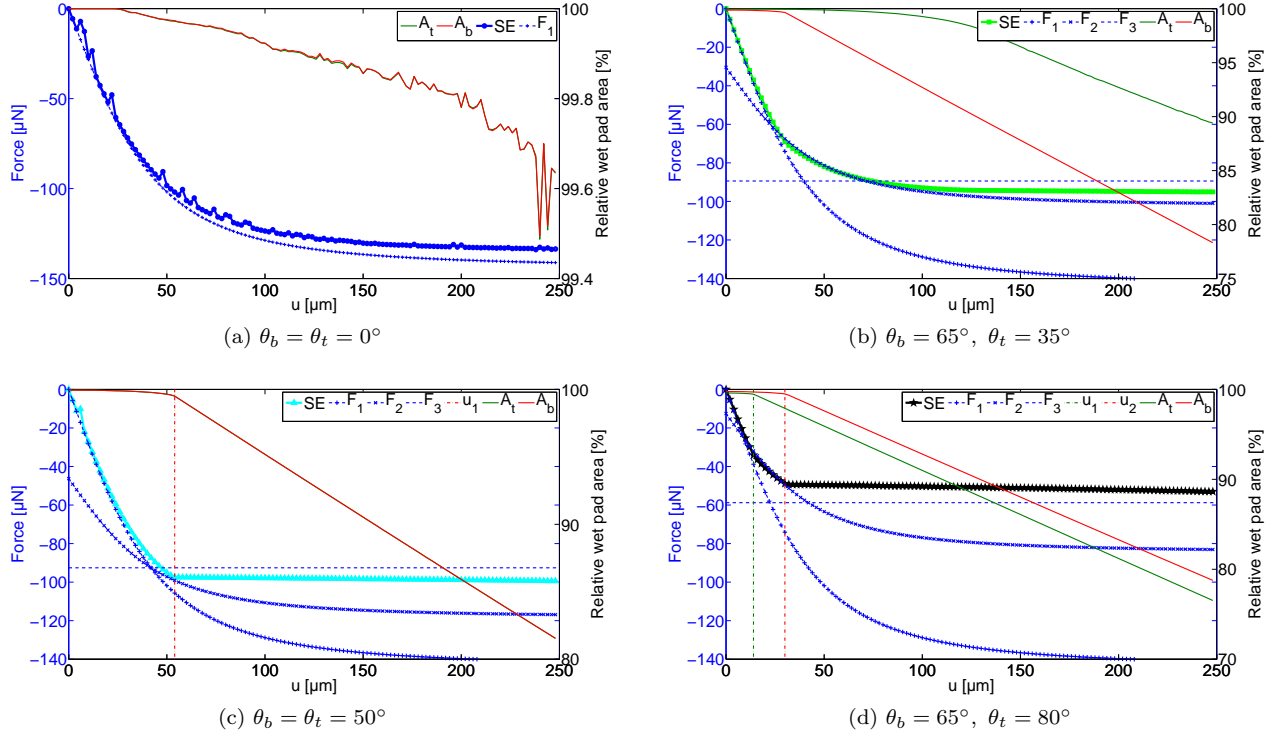


FIG. 11. Capillary forces predicted for $h = 50 \mu\text{m}$ ($AR = 1/20$) and various combinations of θ_* . (a) Perfect wetting (no contact line unpinning), (b) the three sequential regimes, first unpinning on bottom pad, (c) absence of second regime for $\theta_b = \theta_t$ ($u_1 = u_2 = u_d$, $F_1(u_d) = F_2(u_d) = F_3(u_d)$), (d) the three sequential regimes, first unpinning on top pad.

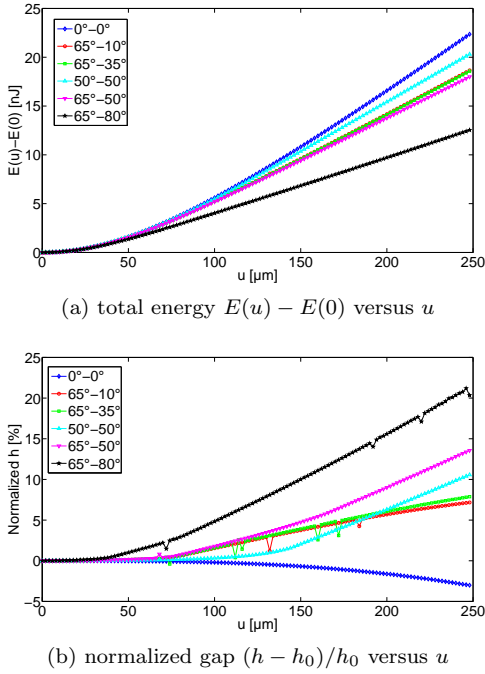


FIG. 12. SE simulations for $h_0 = 50 \mu\text{m}$ ($AR = 1/20$) parameterized by θ_b - θ_t pairs.

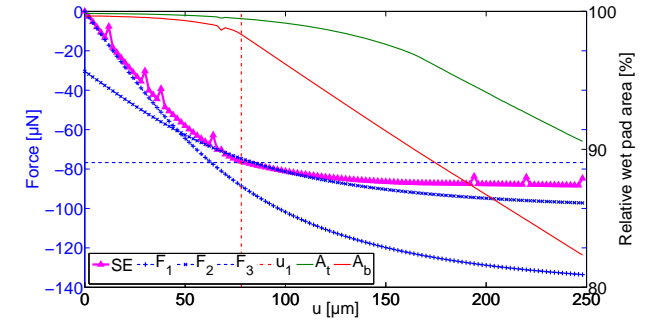


FIG. 13. SE simulation and analytical fit of $F(u)$ versus u for $h_0 = 100 \mu\text{m}$ ($AR = 1/10$) with $\theta_b = 65^\circ$ and $\theta_t = 50^\circ$. Relative error for $F(u = u_{\max})$ is 7.4%.

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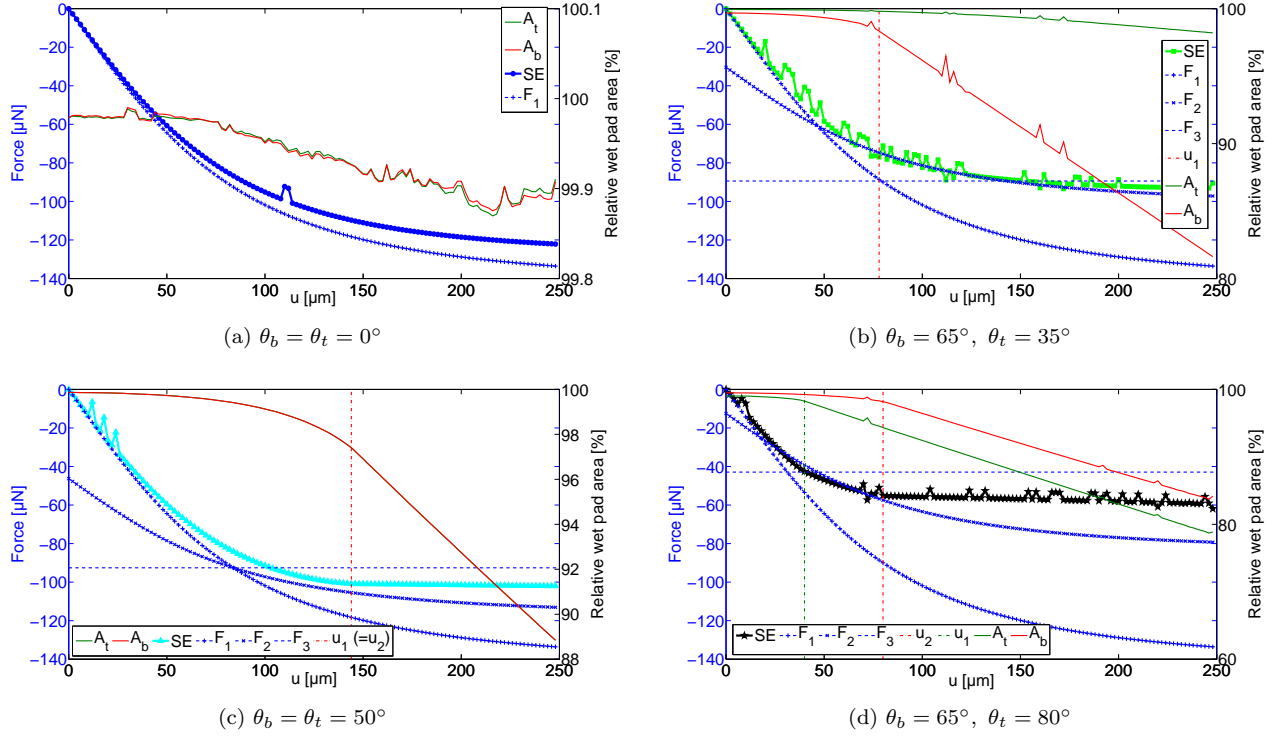
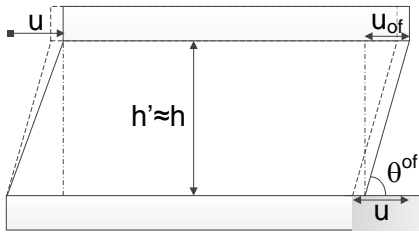
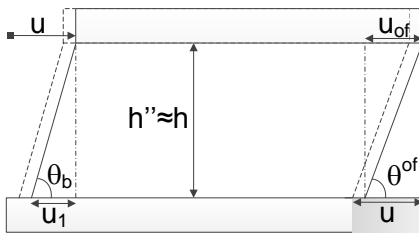


FIG. 14. Capillary forces predicted for $h = 100 \mu\text{m}$ ($AR = 1/10$) and various combinations of θ_b and θ_t values. (a) Perfect wetting (no contact line unpinning), (b) the three sequential regimes, first unpinning on bottom pad, (c) absence of second regime for $\theta_b = \theta_t$ ($u_1 = u_2 = u_d$, $F_1(u_d) = F_2(u_d) = F_3(u_d)$), (d) the three sequential regimes, first unpinning on top pad.



(a) Sketch for $0 < u_{of} < u_1$



(b) Sketch for $u_1 < u_{of}$

FIG. 15. Transitions to overflow regimes: (a) from R_1 to R_2^{of} , (b) from R_2 to R_3^{of} .

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