



## Functional connectivity and alterations in baseline brain state in humans

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### ABSTRACT

This work examines the influence of changes in baseline activity on the intrinsic functional connectivity fMRI (fc-fMRI) in humans. Baseline brain activity was altered by inducing anesthesia (sevoflurane end-tidal concentration 1%) in human volunteers and fc-fMRI maps between the pre-anesthetized and anesthetized conditions were compared across different brain networks. We particularly focused on low-level sensory areas (primary somatosensory, visual, and auditory cortices), the thalamus, and pain (insula), memory (hippocampus) circuits, and the default mode network (DMN), the latter three to examine higher-order brain regions. The results indicate that, while fc-fMRI patterns did not significantly differ ( $p < 0.005$ ; 20-voxel cluster threshold) in sensory cortex and in the DMN between the pre- and anesthetized conditions, fc-fMRI in high-order cognitive regions (i.e. memory and pain circuits) was significantly altered by anesthesia. These findings provide further evidence that fc-fMRI reflects intrinsic brain properties, while also demonstrating that 0.5 MAC sevoflurane anesthesia preferentially modulates higher-order connections.

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### Introduction

Functional areas in the brain are highly interconnected, creating networks that allow complex processing of external and/or internal stimulus representations. To understand how the brain works it is necessary to study not only the brain regions involved in a given task but also how different functional areas of the brain are connected.

In their seminal work, Biswal et al. (1995), showed that during rest the blood oxygenation level dependent (BOLD) signal exhibits phase-locked low-frequency oscillations ( $< 0.1$  Hz) across functionally connected brain regions. This observation allowed the definition of a new method for studying non-invasively functional connectivity within the brain that is now referred to as functional connectivity fMRI (fc-fMRI). The vast majority of the fc-fMRI studies have been focused on the motor/somatosensory (e.g. Biswal et al., 1995; Cordes et al., 2001, 2000; De Luca et al., 2005), visual (Cordes et al., 2001, 2000; Lowe et al., 1998; Nir et al., 2006), and auditory (Cordes et al., 2001, 2000) systems. In addition, several studies have demonstrated functional connections within the high-order functional circuits such as the hippocampal-parietal memory network (Vincent et al., 2006) and the default mode network (DMN) during the developmental stage (e.g. Fair et al., 2008) as well as in adults (e.g. Fox et al., 2006,

2005; Greicius et al., 2003). Furthermore, recent studies have shown that the strength of the connectivity between specific cortical regions is related to task performance in both working memory (Hampson et al., 2006a) as well as in reading (Hampson et al., 2006b). Despite this widespread use of fc-fMRI to investigate the connections across brain regions, the origin of these phase-locked BOLD low-frequency oscillations remains unclear. In particular, the question as to whether fc-fMRI reflects a specific intrinsic (i.e. unrelated to consciousness) property of brain organization or is more related to the conscious state remains unanswered.

The hypothesis that fc-fMRI is a characteristic of brain organization that goes beyond consciousness is supported by results from non-human primates showing that connections within systems such as the ocular-motor, visual, and motor/somatosensory and even within the DMN (or its equivalent in monkeys) remain preserved even at deep levels of anesthesia (Vincent et al., 2007). This observation is also supported by results showing that fc-fMRI patterns reflect anatomical connections, as shown both with staining techniques (Vincent et al., 2007) and with diffusion tensor imaging (DTI; Greicius et al., 2009).

The preceding hypothesis has been challenged by other studies showing that fc-fMRI is modulated by anesthesia or sedation, though the results are often conflicting. Some studies have shown a decrease in fc-fMRI under anesthesia (e.g. Lu et al., 2007; Peltier et al., 2007), while others observed an increase in functional connectivity (e.g. Greicius et al., 2008; Kiviniemi et al., 2000, 2005). These results are however difficult to compare because of the differences in dosage, type of anesthetic agents used and brain networks investigated. In addition,

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**Table 1**  
Physiologic measures.

	Pre-anesthesia	Anesthesia	t-Test	
Heart rate (bpm)	53 ± 8.0	52 ± 6.1	$t_{(13)} = 0.611$	$p = 0.552$
Respiratory rate (cpm)	14 ± 2.9	16 ± 1.7	$t_{(13)} = 0.327$	$p = 0.136$
SpO <sub>2</sub> (%)	99 ± 0.4	99 ± 0.7	$t_{(13)} = -0.444$	$p = 0.664$
Systolic blood pressure (mmHg)	114 ± 9.2	109 ± 7.0	$t_{(13)} = 3.877$	$p = 0.002$
Diastolic blood pressure (mmHg)	68 ± 5.3	63 ± 5.2	$t_{(13)} = 2.667$	$p = 0.019$
Mean blood pressure (mmHg)	83 ± 6.2	78 ± 5.2	$t_{(13)} = 3.145$	$p = 0.008$
EtCO <sub>2</sub> (mmHg)	36 ± 3.2	35 ± 3.4	$t_{(13)} = 0.748$	$p = 0.468$

animal studies typically compared fc-fMRI maps between two different levels of anesthesia (Lu et al., 2007), whereas most other studies in humans have compared the results obtained under anesthesia with those obtained in the non-anesthetized condition either in the same group of subjects (Greicius et al., 2008; Kiviniemi et al., 2005; Peltier et al., 2005), or in a separate control group (Kiviniemi et al., 2000).

In the recent years, there has been a growing interest in the analysis of fMRI under anesthesia in humans, but the results are controversial. Some studies have shown no task-related BOLD response in the anesthetized condition (e.g. Antognini et al., 1997; Heinke et al., 2004), while others observed changes in the spatial extent of the response but not in the amplitude of the BOLD response (Marcar et al., 2004). Finally, other studies showed a dose- and region-dependent reduction of the BOLD response under anesthesia (e.g. Kerssens et al., 2005; Plourde et al., 2006). Similarly, fc-fMRI studies under anesthesia showed varying results reporting either increased in

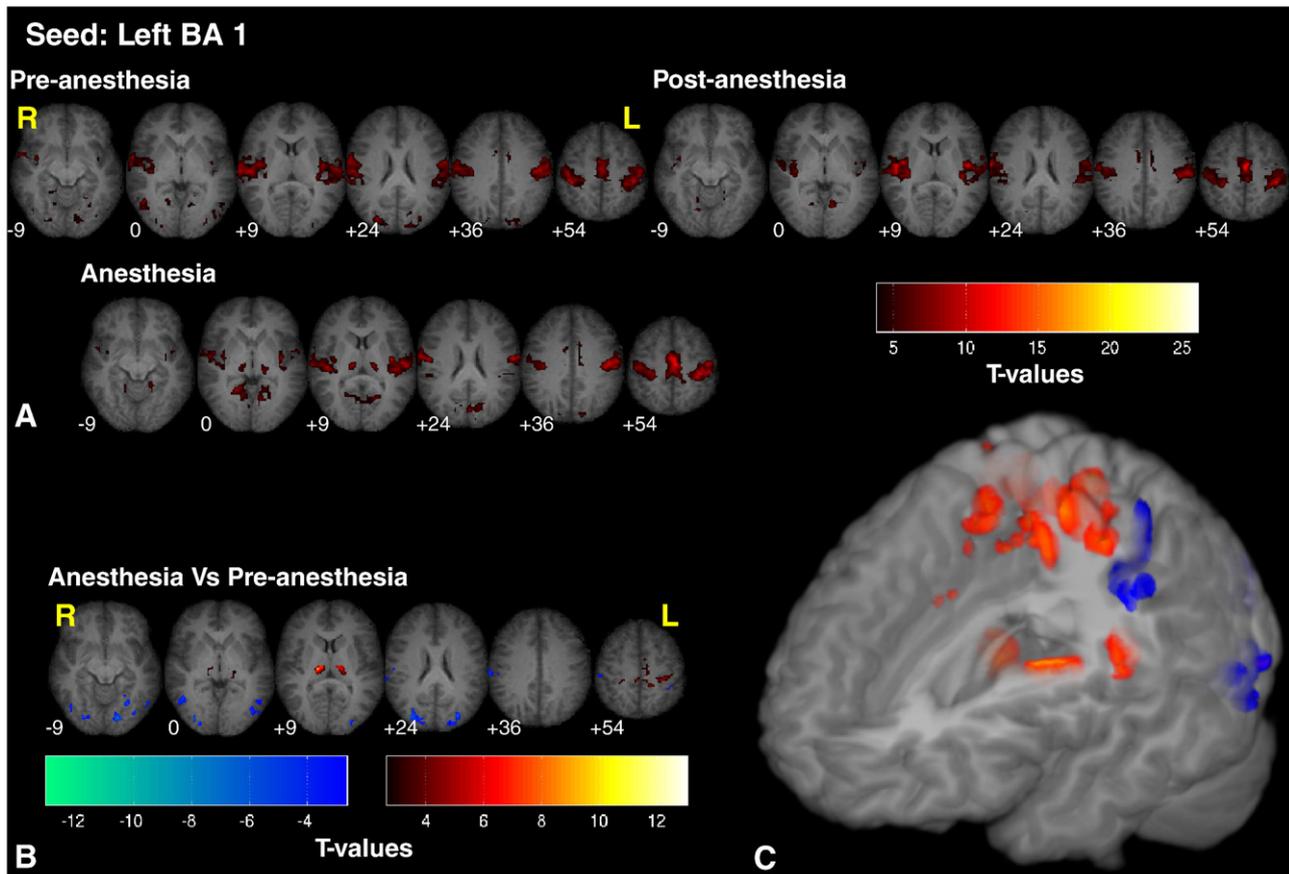
functional connectivity under anesthesia (e.g. Greicius et al., 2008; Kiviniemi et al., 2000, 2005), or a decrease in functional connectivity (e.g. Peltier et al., 2007). The explanation for the variation in the results can be found in the different doses and anesthetics agents used in these studies and in the different brain networks investigated.

To better understand whether fc-fMRI reflects a specific intrinsic property (i.e. unrelated to consciousness) of the brain, in the present study we investigated the effects of light anesthesia on functional connectivity between specific cortical regions. Anesthesia alters consciousness level (Alkire et al., 2008), and therefore if fc-fMRI reflects intrinsic properties of the brain, connectivity patterns should be unaffected by the administration of anesthesia. Based on this hypothesis, changes in the strength of connectivity, would suggest that connectivity patterns are influenced by or reflect a consciousness-related processes. This hypothesis was tested by comparing fc-fMRI maps in the awake and lightly-anesthetized conditions (sevoflurane end-tidal concentration 1%, equivalent to 0.5 MAC, minimum alveolar concentration) across different brain networks, with particular focus on low-level sensory areas (seeding the analysis in the primary somatosensory, visual, and auditory cortices), thalamus, memory (seeding in the hippocampus), and pain (seeding in the insula) circuits, and the default mode network.

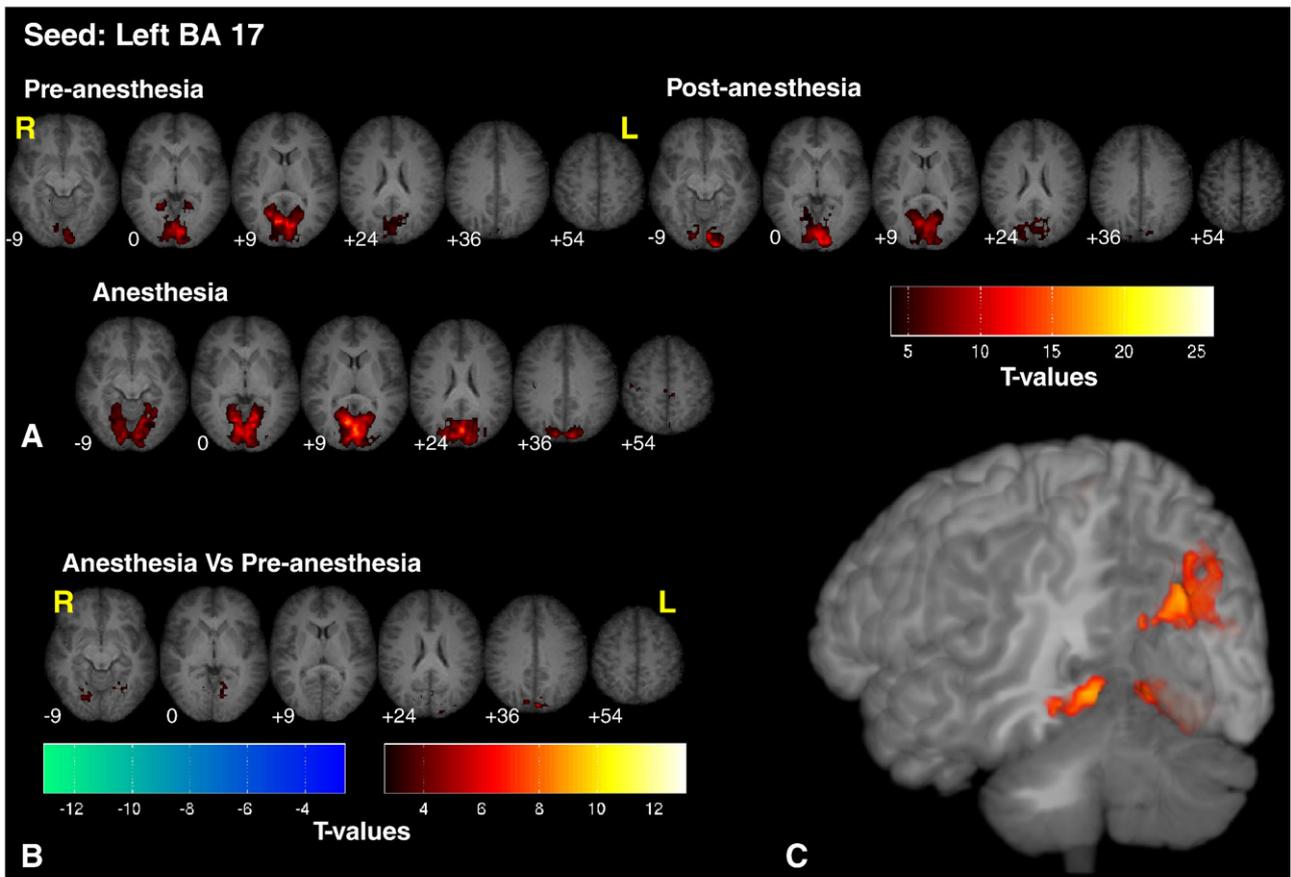
## Materials and methods

### Subjects and experimental procedures

14 healthy subjects (7 male; 11 right and 3 left handed) participated in the study. Subjects' age ranged 22–34 years (mean



**Fig. 1.** Significant fc-fMRI values relative to the left BA 1 seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as  $t$  values. Anesthesia increased connectivity with the thalamus and primary motor/somatosensory areas, and reduced the connectivity with extrastriate visual areas.



**Fig. 2.** Significant fc-fMRI values relative to the left BA 17 seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as *t* values. High-order visual areas showed an increased connectivity with BA 17 under anesthesia.

age  $\pm$  SD  $26.1 \pm 3$  years). All subjects gave written informed consent and the study protocol was approved by the Human Investigation Committee of the Yale School of Medicine (New Haven, CT).

The study was conducted in healthy ASA I (American Society of Anesthesiologists – physical status class I) in the age group of 22 to 34 years. Subjects were interviewed and basic pre-anesthesia screening was carried out prior to the study, to ensure that they fulfilled the inclusion and exclusion criteria. Subjects on psychoactive drugs or any centrally acting medication, history of epilepsy or renal disease, and presence of a potentially difficult airway were part of the exclusion criteria. As a precaution against pulmonary aspiration of gastric contents (causing difficulty in breathing), and in agreement with ASA guidelines (ASA Task Force, 1999), all subjects fasted for 8 h before the study and did not intake clear liquids for 2 h prior the experiment. Before the beginning of the acquisitions, an intravenous line was started with a 22-gauge cannula for maintenance infusion (lactated ringer was infused at 100 cc/h) and subjects were connected to MR-compatible ASA monitors (EKG, non invasive blood pressure, pulse-oximeter and end-tidal carbon dioxide). Additionally, systolic and diastolic blood pressures (BPs and BPD, respectively) were used to compute the mean blood pressure, defined as  $(BPs + 2BPD) / 3$ . Sevoflurane was administered through a facemask held in place with head straps and connected to a semi-closed circle absorber circuit.

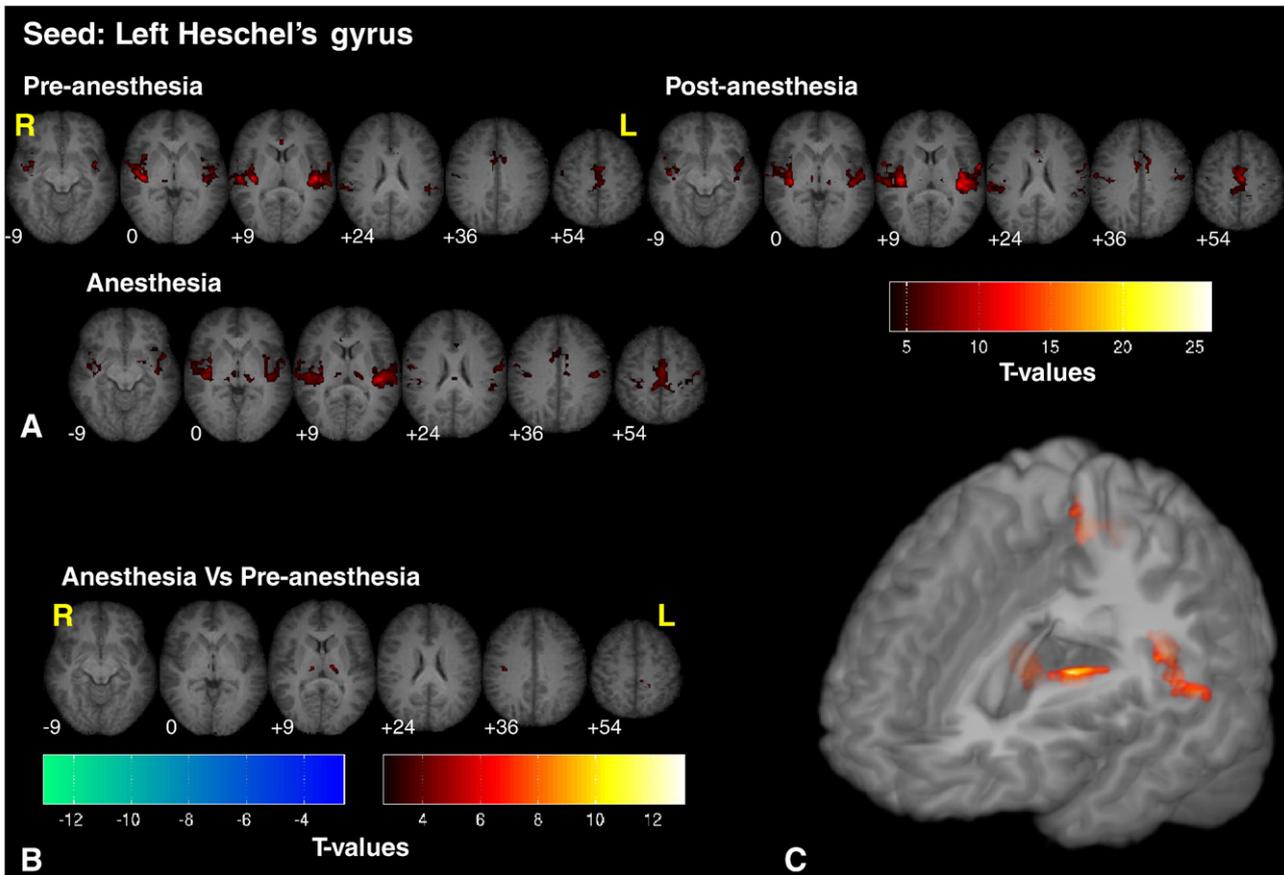
During the entire study, subjects were asked to lie in the scanner with the eyes closed, and to refrain from performing any goal-oriented mental activity. The acquisition protocol comprised of three experimental conditions. In the first condition (pre-anesthesia), pure oxygen was administered to the subjects, in the second condition (anesthesia) subjects received a mixture of  $O_2$  and sevoflurane (end-tidal concen-

tration 1%, equivalent to 0.5 MAC, minimum alveolar concentration), and in the third condition (post-anesthesia) they received pure oxygen again. Conditions were separated by 10 minute transition periods to allow for end-tidal sevoflurane concentration to reach a steady state and to allow for anesthetic washout (respectively).

At the end of the experiment subjects were monitored in a recovery area and they were discharged home when they were awake and alert, able to dress up and ambulate without help. At this point monitors were disconnected and the intravenous cannula was removed. Subjects were advised not to drive for the next 24 h.

#### MR data acquisition

Imaging was performed using a 3 T Siemens (Erlangen, Germany) Trio MR system with a circularly polarized head coil. After a first localizing scan, 33 axial slices (slice thickness 4 mm, no gap, FoV = 256 mm, matrix size  $64 \times 64$ ) parallel to the AC-PC line were acquired using a T1-weighted sequence (TR = 300 ms, TE = 2.43 ms, FoV = 256 mm, matrix size  $256 \times 256$ , flip angle  $60^\circ$ ). Functional imaging volumes were collected in the same slice position as the preceding T1-weighted data. During each of the three experimental conditions (i.e. pre-anesthesia, anesthesia, and post-anesthesia), three functional runs were acquired using a T2\*-sensitive gradient-recalled, single-shot echo-planar imaging pulse sequence (TR = 2 s, TE = 31 ms, FoV = 256 mm, flip angle  $90^\circ$ , matrix size  $64 \times 64$ ). Each volume consisted of 33 slices parallel to the bicommissural plane (slice thickness 4 mm, no gap), and each functional run was comprised of 210 volumes.



**Fig. 3.** Significant *fc-fMRI* values relative to the left Heschel's gyrus seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent *fc-fMRI* significance, reported as *t* values. Anesthesia increased the connectivity of the Heschel's gyrus with the thalamus and the right STS.

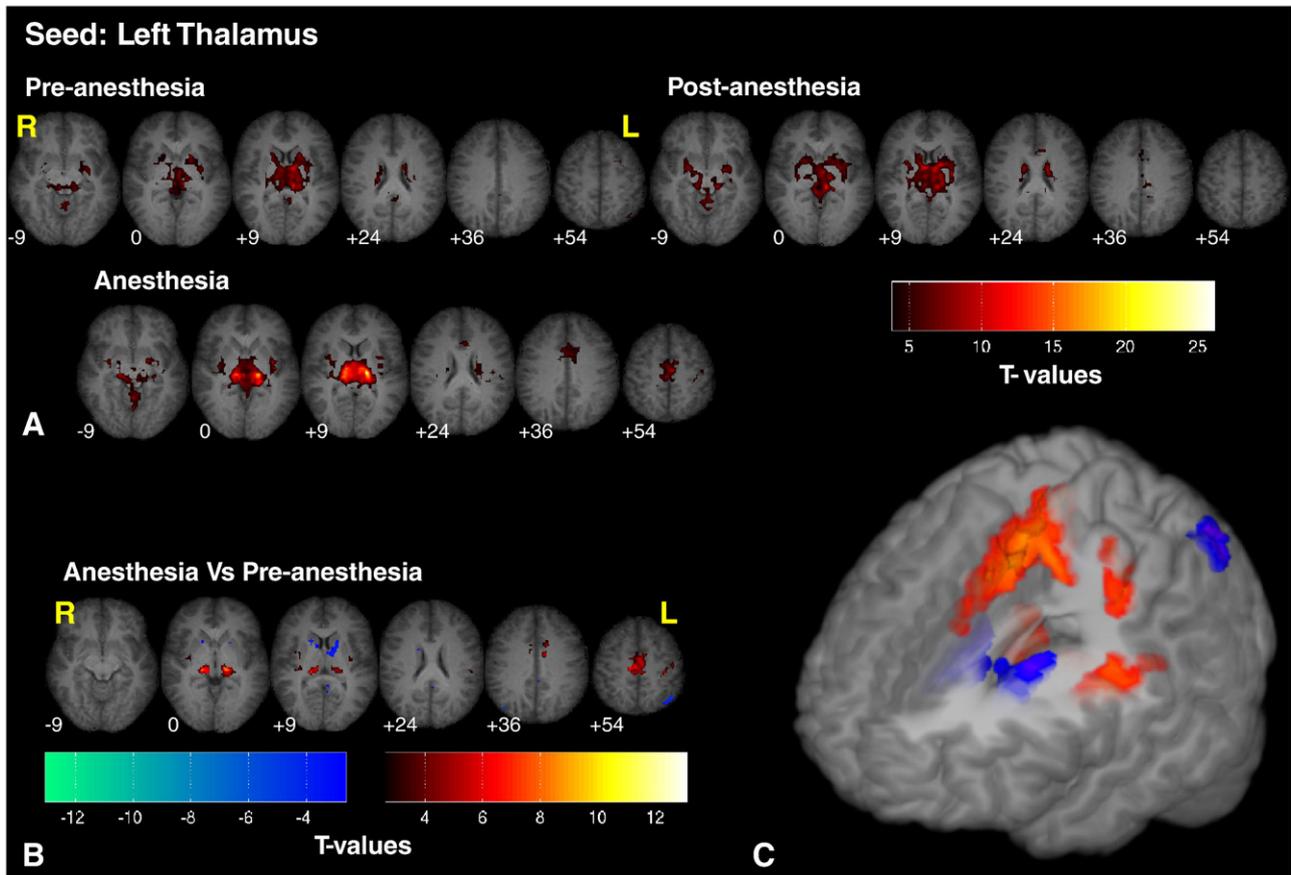
During the washout period, anatomical images were acquired using a T1-weighted sagittal gradient-echo (MPRAGE) sequence (176 contiguous sagittal slices, slice thickness 1 mm, matrix size  $256 \times 256$ , FoV = 256 mm TR = 2530 ms, TE = 3.34 ms, flip angle =  $7^\circ$ ).

#### Data analyses

After discarding the first 10 volumes of each run (to allow for the magnetization to approach steady state), data were temporally and spatially realigned and corrected to remove slice means and drift. Finally, signal at each voxel was low-pass filtered at a cut-off frequency of 0.08 Hz with a 4th degree elliptical filter and the 6 estimated motion parameters were regressed from the data (see e.g. Laufs et al., 2007), as were the mean signals of white matter and CSF. While cardiac and respiratory rates were continuously monitored, only half of the subjects had artifact free recordings of these physiologic parameters throughout the study and therefore this data was not used to decorrelate these noise components from the *fMRI* data. Because of the limited anesthesia induced changes in cardiac and respiratory rates, these noise components are not expected to impact the results. A more thorough discussion on this issue and an analysis of a subset of data where these factors are removed are included as [Supplementary text](#). For each of the three conditions, connectivity maps were computed using primary auditory, primary visual and primary somatosensory areas, thalamus, insula, hippocampus bilaterally, and the posterior parietal cortex (PCC) as the seed regions. These *fc-fMRI* maps were computed in the single-subject space and then transformed into the reference (i.e. MNI) space using a non-linear registration (see below for the details of the normalization proce-

duce). Seed regions were anatomically identified on a MNI-T1 template. All the seed regions, with the exclusion of the Heschel's gyrus and the PCC, were selected from the Brodmann Area atlas embedded in *BiImage Suite* ([www.bioimagesuite.org](http://www.bioimagesuite.org)). Heschel's gyrus was defined as a subregion of BA 41 (defined according to the *BiImage Suite* atlas) including only that gyrus. PCC was defined as a sphere of 10 mm-radius and centered in the coordinates ( $[-5 -49 40]$ ) as defined in the Talairach coordinates) reported in the meta-analysis by Shulman et al. (1997). In the *fc-fMRI* analysis, seed regions were transformed into the single-subject space by applying the inverse of the transformation from the single subject to the reference (i.e. MNI) space (see below). Correlation results were transformed into Gaussian values by applying a Fischer transform (Hays, 1981). Single-subject results were smoothed using a Gaussian kernel (FWHM = 6 mm) and normalized to the MNI standard template, using the intensity-only component of the method reported in Papademetris et al. (2004), as implemented within *BiImage Suite* software ([www.bioimagesuite.org](http://www.bioimagesuite.org)). Spatial normalization includes the computation of three transformations. First, functional EPI images were linearly coregistered to the co-localized T1-2D anatomical image. This individual 2D anatomical image was then linearly registered to the individual MPRAGE (3D anatomical image). Finally, a non-linear registration was applied to transform the individual 3D anatomical volume into the MNI reference space.

Group analyses were carried out as a second level of statistic. For each seed region and for each voxel, a one-sample *t*-test was used to identify statistically significant positive correlation values ( $p < 0.001$ , 20-voxel cluster threshold). Differences between conditions were tested using a paired *t*-test. These contrasts were computed only in



**Fig. 4.** Significant fc-fMRI values relative to the left thalamus seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as  $t$  values. Under anesthesia, thalamus showed a stronger connectivity with SMA and insula, while connectivity with the caudate and left IPL was decreased.

locations showing reliable positive correlations ( $p < 0.001$ ) with the seed region in either condition. Because correction for multiple comparisons was already accounted for in the identification of the positively correlated regions (i.e. the locations where contrasts between conditions were computed), similar to the approach of Beauchamp (2005) we identified significant differences between conditions using a more liberal threshold ( $p < 0.01$ , 20-voxel cluster threshold). Anatomical regions were identified from the fc-fMRI maps by using the Talairach Daemon Atlas (Lancaster et al., 2000), after transforming MNI coordinates into Talairach coordinates corrected using a non-linear transformation (Lacadie et al., 2008).

Head movement parameters estimated by the realignment algorithm were used to test whether under anesthesia subjects exhibited a different head movement. For each functional run, the variance of the displacement (translation) with respect to the first volume of the run was first computed. The mean variances across the three pre-anesthesia and the three anesthesia runs were then calculated. A non-parametric sign test was applied to assess whether these two sets of variances came from populations with equal median.

## Results

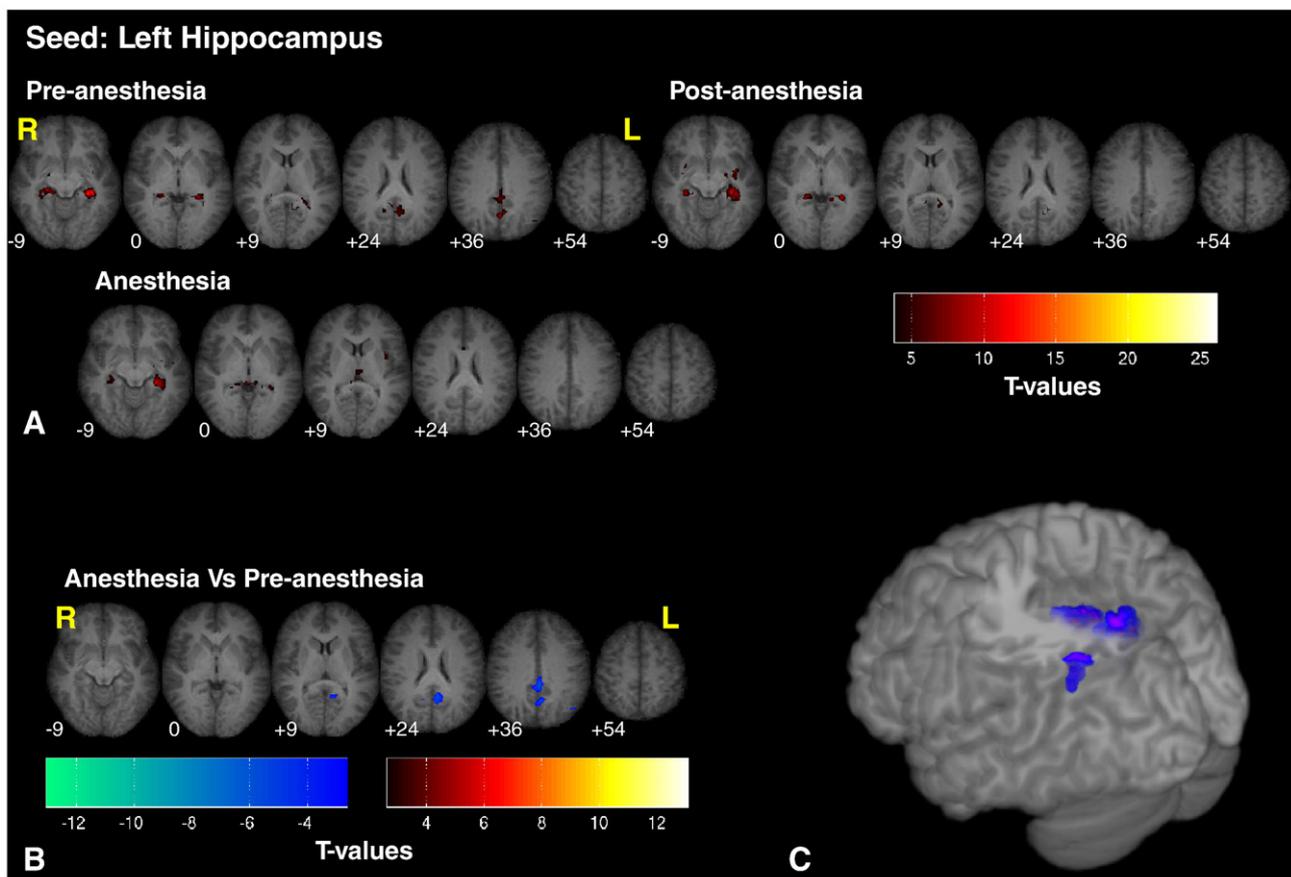
Though there were two non-anesthetized imaging cycles (pre- and post-anesthesia) only the comparison between the pre-anesthesia and anesthesia conditions is presented. The purpose of introducing a pre- and post-anesthesia imaging was to eliminate the possibility that the alterations in connectivity observed with anesthesia are simply due to order effects. Contrasts between pre- and post-anesthesia conditions revealed few sparse clusters show-

ing significant differences ( $p < 0.01$ , 20-voxel cluster threshold) between these two conditions (see Supplementary Table 1 for the complete list of clusters), indicating the within-session repeatability of our fc-fMRI patterns. However, the second post-anesthesia condition was confounded by subject movement and discomfort as the anesthesia state was reversed and so the results were noisier and thus not included.

To examine the possibility that differences in fc-fMRI results between the pre- and anesthetized conditions reflected changes due to the movement of the head in the subjects, head displacement parameters (in comparison to the first volume acquired for each run), as estimated by the motion correction algorithm, were compared under the pre- and anesthetized runs. This analysis did not reveal any significant head motion difference between the pre- and anesthesia runs (sign test,  $p > 0.79$ ).

## Physiological parameters

During the MR session physiological parameters, including heart and respiratory rates, blood pressure, end-tidal  $\text{CO}_2$ , and  $\text{O}_2$  partial pressure ( $\text{SpO}_2$ ), were constantly monitored and mean physiological values are summarized in Table 1. Comparison of these parameters between the pre-anesthesia and anesthesia states revealed a statistically significant change only in systolic (decreasing from  $114 \pm 9.2$  mmHg to  $109 \pm 7.0$  mmHg,  $p = 0.002$ ), diastolic (decreased from  $68 \pm 5.3$  mmHg to  $63 \pm 5.2$  mmHg,  $p = 0.019$ ) and mean blood pressure (decreased from  $83 \pm 6.2$  mmHg to  $78 \pm 5.2$  mmHg,  $p = 0.008$ ) moving from the pre-anesthetic to anesthetic condition. However this change in systolic and diastolic pressure was well within the autoregulatory



**Fig. 5.** Significant fc-fMRI values relative to the left hippocampus seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as  $t$  values. Connectivity between hippocampus and PCC and IPL was reduced by anesthesia.

range (Drummond, 1997) and was not expected to induce cerebral hemodynamic changes. Heart rate, respiratory rates, SpO<sub>2</sub>, and end-tidal CO<sub>2</sub>, did not show significant change ( $p > 0.1$ ) with 0.5 MAC sevoflurane anesthesia.

#### Connectivity maps

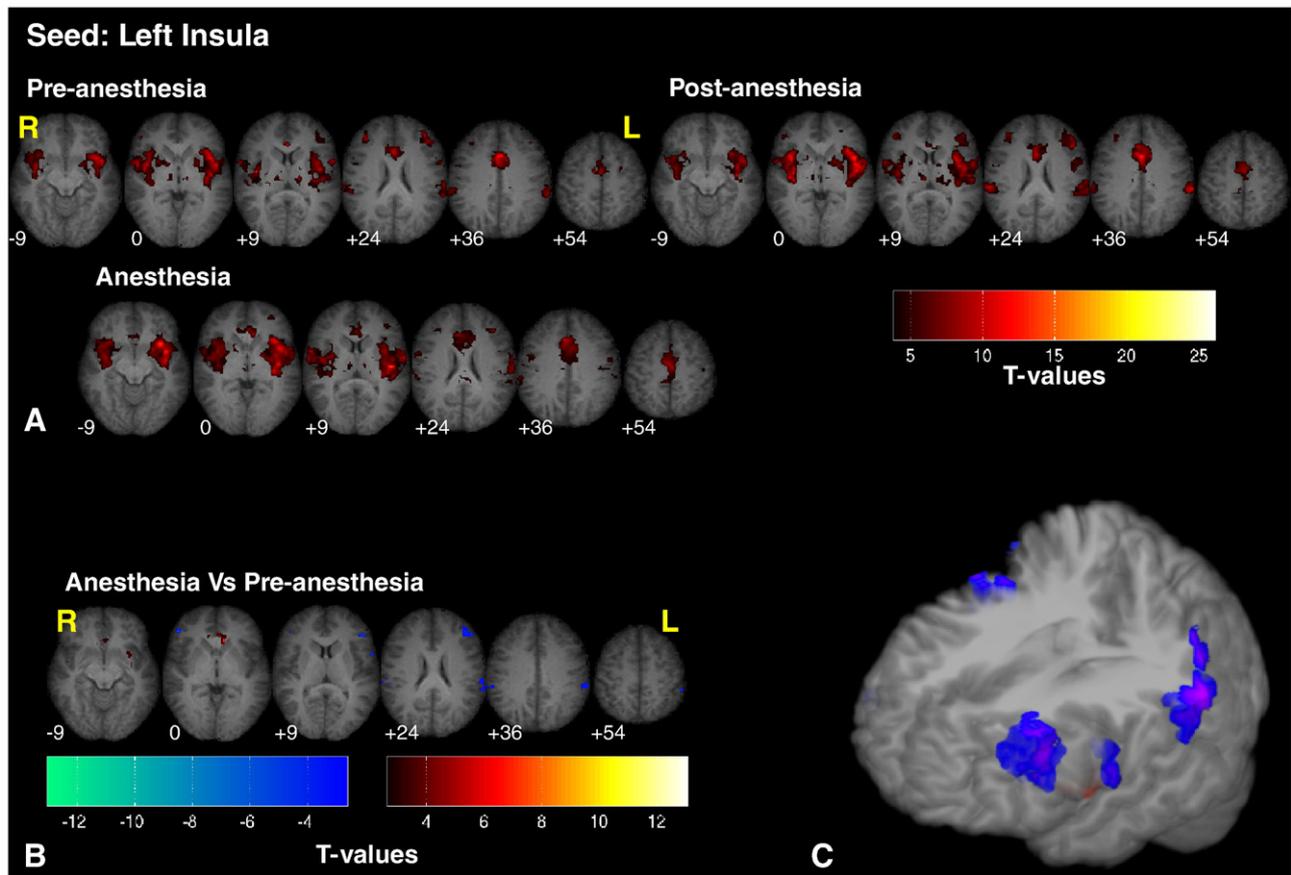
Connectivity maps were computed for the pre- and anesthesia states using primary somatosensory, visual, auditory cortices, thalamus, hippocampus, insula, and PCC as seed regions. To investigate functional alterations associated with 0.5 MAC sevoflurane anesthesia the following seed regions were selected: thalamus a region that modulates consciousness; the hippocampus which is linked to memory; the insula, a region consistently activated in acute pain; and the PCC which is part of the DMN, and may be involved in self referential processing (e.g. Buckner et al., 2008; Johnson et al., 2006). Visual and auditory cortices were chosen based on our previous data indicating that these regions are preferentially affected under low dose sevoflurane anesthesia (Qiu et al., 2008b).

Functional connectivity results ( $p < 0.001$ ; 20-voxel cluster threshold) were highly consistent across homologous seed regions within the two hemispheres. Therefore, Figs. 1–7 as well as Tables 2 and 3 report the results relative only to the seed regions in the left hemisphere. All the areas showing differences in connectivity between the two anesthetic levels are also reported in Tables 2 and 3. Results relative to the right seed regions are available as Supplemental data.

In the following section the results revealing the networks connected to the individual seed regions (significant at  $p < 0.001$ ;

20-voxel cluster threshold) and the changes in connectivity between the pre- and anesthetized conditions are described (significant at  $p < 0.01$ ; 20-voxel cluster threshold; analysis limited to the regions showing significant connectivity in either condition).

- 1) Functional connectivity with the Brodmann Area (BA) 1 (i.e. primary somatosensory cortex) was significant across the entire bilateral somatosensory and motor network in both the pre-anesthesia and anesthesia conditions (see Fig. 1 and Supplementary Fig. 1 for the right BA 1 seed). The areas that were part of this network included, primary somatosensory (S1) and motor areas (M1) bilaterally, supplementary motor area (SMA), pre-SMA, bilateral thalamus, secondary somatosensory area (SII), and the intraparietal sulcus (IPS). In addition, connections with other sensory cortices, such as the auditory and the visual areas (mostly with the extrastriate cortices) were also significant. Contrasting connectivity maps between the pre- and anesthetic conditions, we observed that under anesthesia left BA 1 showed increased connectivity with the thalamus as well as within limited regions within the primary motor/somatosensory areas. Conversely, reduced connectivity was observed between area BA 1 and the extrastriate visual areas, such as the lingual gyrus and the superior occipital gyrus, bilaterally.
- 2) Seeding in BA 17 (i.e. primary visual area) revealed significant connections only within the visual cortex (see Fig. 2 and Supplementary Fig. 2 for the right BA 17 seed). Bilateral high-order visual areas within the cuneus (BA 19) and the lingual gyrus showed stronger connectivity under anesthesia than in the pre-anesthesia condition. No regions showed decreases in functional



**Fig. 6.** Significant fc-fMRI values relative to the left insula seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as  $t$  values. Under anesthesia, connectivity with bilateral SII and with left middle frontal gyrus was reduced.

- connectivity under anesthesia when using the visual cortex as the seed.
- 3) Seeding in Heschel's gyrus (i.e. primary auditory cortex) revealed connectivity with the entire auditory cortex bilaterally, the thalamus, and the anterior cingulate cortex (ACC), as shown in Fig. 3 (see Supplementary Fig. 3 for the right Heschel's gyrus seed). We observed increased connectivity under anesthesia in the thalamus bilaterally, in the right STS, and in part of the motor areas. Under anesthesia no regions showed decreases in functional connectivity with Heschel's gyrus.
  - 4) Seeding in the thalamus revealed a network including all the deep structures of the brain, such as the putamen, the caudate nucleus bilaterally (basal ganglia), and the brainstem (see Fig. 4 and Supplementary Fig. 4 for the right thalamus seed). Anesthesia highlighted the connectivity between the thalamus and the SMA. In addition, anesthesia also increased connectivity between the thalamus and insula, while reducing the connectivity between the thalamus and the caudate and the left inferior parietal lobule (IPL).
  - 5) Seeding in the hippocampus, revealed significant connectivity with the contralateral hippocampus, posterior cingulate cortex (PCC) adjacent to the precuneus, and the left inferior parietal lobule (IPL), as shown in Fig. 5 (see Supplementary Fig. 5 for the right hippocampus seed). Connectivity with the PCC and bilateral IPL showed significant correlations only in the pre-anesthetized conditions. Under anesthesia no regions showed increased connectivity with the hippocampus.
  - 6) Connectivity maps to the insula seed region reveal significant connections with the ACC, SII and the middle frontal gyrus bilaterally (see Fig. 6 and Supplementary Fig. 6 for the right insula

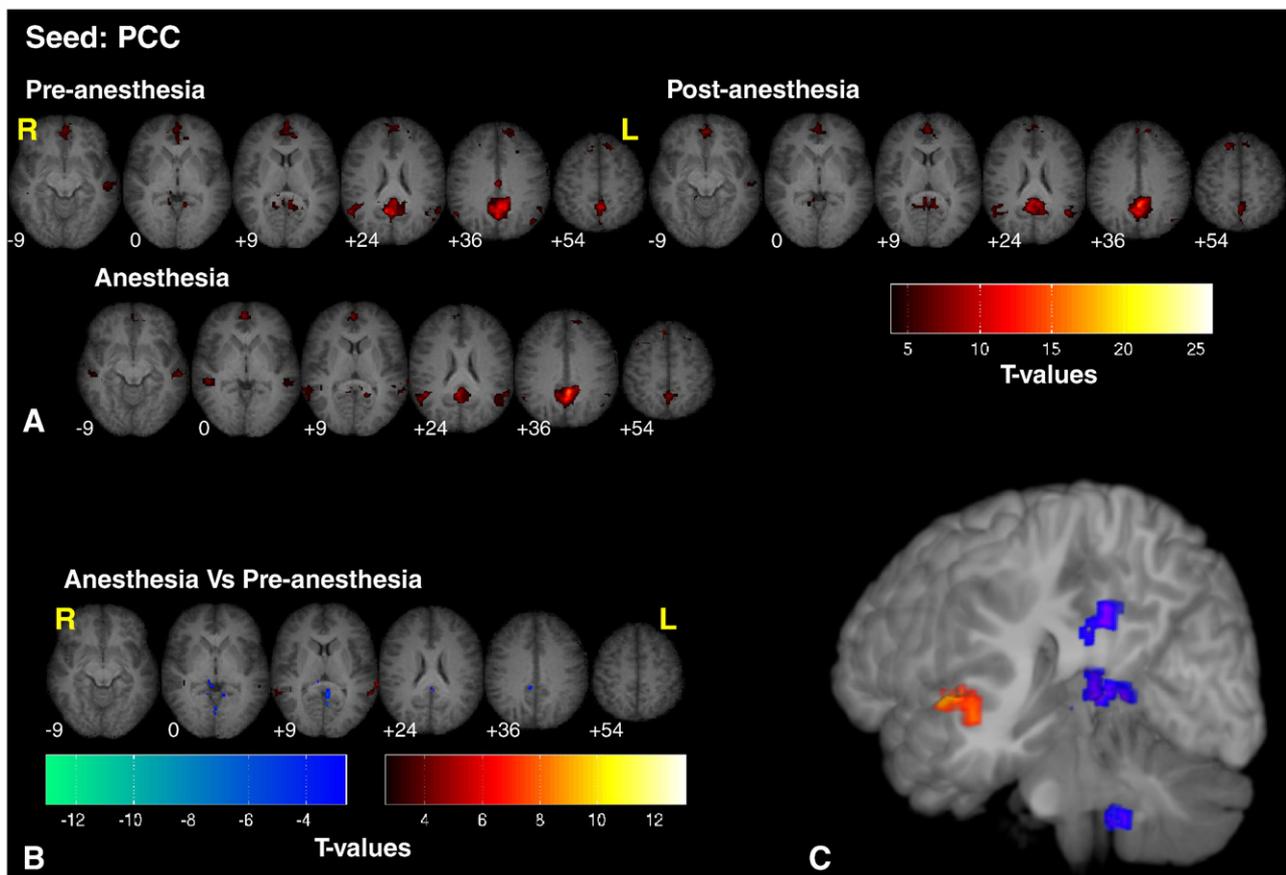
seed). Under anesthesia connectivity with the bilateral SII and with the left middle frontal gyrus was reduced, while connectivity with the ACC and the left putamen was increased.

- 7) Seeding with the PCC revealed significant connectivity with the anterior cingulate cortex (ACC) and with the IPL bilaterally (see Fig. 7). Anesthesia increased the connectivity between PCC and the superior temporal gyrus (STG) and reduced connectivity with areas adjacent to the seed region.

## Discussion

The main aim of this study was to investigate the effects of changes in brain baseline activity on fc-fMRI. This aim was pursued by analyzing the changes in fc-fMRI maps induced by 1% (equivalent to 0.5 MAC) sevoflurane anesthesia.

We observed high repeatability of within-session fc-fMRI patterns, also in agreement with recent results by Shehzad et al. (in press). This finding eliminates the possibility that the observed differences in fc-fMRI between pre- and anesthesia conditions were due to an order effect and/or changes in the baseline associated with starting another sequence. We also consider highly unlikely – while we cannot exclude completely this possibility – that the results shown are driven by anesthesia-related changes in the hemodynamics and not in the neuronal response for two main reasons. First, fc-fMRI is insensitive to signal amplitude. Indeed, the effect of a reduced range of BOLD signal fluctuations might change the correlations because it reduces the signal-to-noise ratio, and if this were the case a global decrease in connectivity under anesthesia should be observed. The concomitant presence of both increased and decreased connectivity, found in the



**Fig. 7.** Significant fc-fMRI values relative to the PCC seed region, under the pre-, post-, and anesthesia conditions (A) and the contrast between anesthesia and pre-anesthesia (B) within different axial slices shown in radiological convention (MNI z-coordinates reported in the inset), or in a three-dimensional reconstruction of the template brain (C). Colors represent fc-fMRI significance, reported as *t* values. Anesthesia increased the connectivity between PCC and STG and reduced connectivity with areas adjacent to the seed region.

present study, instead suggests a neuronal origin for these changes. Second, if the changes in correlations simply reflected a reduced range of the BOLD oscillations, we would expect correlations to decrease throughout the brain, irrespectively of the seed regions used. Instead, we observed changes in BOLD correlations only with some specific seed regions, and these changes were highly localized within specific brain circuits.

Because of technical limitations, the results presented in this paper were obtained without correcting the data for cardio-respiratory confounds. To evaluate the impact cardio-respiratory artifacts, physiologic noise correction was performed using the RETROICOR algorithm (Glover et al., 2000) on a subset of 7 subjects (results shown in Supplementary Figs. 7 and 8). Although in this analysis we used a more liberal threshold than in the analysis of all the 14 subjects, the results replicated the main findings of this study and illustrate the minimal impact that this correction has on the results shown. In addition, comparing the results obtained with and without applying the RETROICOR algorithm, it is difficult to dissociate the contribution of variations due to the noise correction approach itself and to that due to the reduced number of subjects.

Functional connectivity analysis revealed significant correlations within the sensory system (e.g. see Biswal et al., 1995; Cordes et al., 2001, 2000; De Luca et al., 2005; Lowe et al., 1998; Nir et al., 2006 for similar results involving motor/somatosensory, auditory, and visual cortices), as well as significant correlations between the primary and secondary somatosensory areas, visual and auditory cortices. These results were replicated when the primary auditory cortex was used as seed regions. Visuo-somatosensory connections have been demonstrated both with tracing techniques in primates (e.g. Cappe and

Barone, 2005; Négyessy et al., 2006) and with fc-fMRI in humans (Yu et al., 2008). Similarly, auditory-somatosensory connections have been identified by tracing studies (Smiley et al., 2007) as well as by electrophysiology (e.g. Fu et al., 2003; Lakatos et al., 2007; Schroeder et al., 2001). Our results did not reveal significant connections between auditory and visual cortices, as shown by Eckert et al. (2008). Several studies have shown that primary auditory and visual areas play a role in integrating multisensory inputs (e.g. Kayser et al., 2005, 2008; Martuzzi et al., 2007) and the present results add converging evidence of communications between sensory-specific brain areas. Functional connectivity however cannot reveal whether these communications occur directly between these areas or if they are mediated by other multisensory regions.

Functional connectivity maps obtained with and without administration of an anesthetic drug revealed consistent connectivity patterns, notwithstanding some significant differences, associated mostly with higher-order cognitive processing regions. The results suggest that functional brain organization is preserved under anesthesia and are in agreement previous studies showing that fc-fMRI patterns remain essentially unchanged even under deep anesthesia in monkeys (Vincent et al., 2007) as well as in humans during sleep, (Horowitz et al., 2008), sedation (Kiviniemi et al., 2005), and in comatose patients (Boly et al., 2008, in press). In addition, anatomical studies conducted with staining techniques (Vincent et al., 2007) and DTI (Greicius et al., 2009) confirmed anatomical connectivity between regions identified by fc-fMRI analysis.

While most networks are preserved under low levels of anesthesia, significant changes were observed between the pre- and anesthetized conditions for some seed regions. The most significant differences

**Table 2**

List of the regions showing differences in fc-fMRI between the pre- and anesthesia conditions with low-level sensory areas of the left hemisphere.

MNI coord (mm)			Talairach coord (mm)			t Values	Cluster size	Brain region	Brodmann Area
x	y	z	x	y	z				
<i>Left BA1</i>									
Anesthesia > pre-anesthesia									
18	-21	12	17	-21	14	9.17	58	R	Thalamus
-24	-30	60	-24	-26	54	7.72	423	L	Precentral gyrus
18	-30	63	19	-26	57	7.1		R	Precentral gyrus
-9	-15	9	-8	-16	11	7.08	50	L	Thalamus
-36	-33	21	-35	-32	21	5.1	28	L	Insula
Pre-anesthesia > anesthesia									
39	-81	-3	40	-80	2	8.68	163	R	Middle occipital gyrus
-27	-78	-12	-27	-77	-5	8.2	68	L	Lingual gyrus
36	-81	21	37	-78	22	7.94	91	R	Middle temporal gyrus
-15	-84	-9	-15	-81	-3	7.31	21	L	Lingual gyrus
-27	-66	-9	-26	-65	-3	7.21	44	L	Lingual gyrus
63	-27	39	62	-25	37	6.61	100	R	Postcentral gyrus
-27	-81	24	-27	-77	24	6.38	80	L	Superior occipital gyrus
-36	-45	57	-36	-42	52	4.72	49	L	Inferior parietal lobule
-57	-30	42	-56	-28	39	3.39	13	L	Postcentral gyrus
<i>Left BA17</i>									
Anesthesia > pre-anesthesia									
-3	-87	36	-3	-82	34	6.32	280	L	Cuneus
12	-81	36	12	-77	34	4.05		R	Cuneus
-18	-60	-3	-17	-59	1	5.28	137	L	Lingual gyrus
24	-75	-6	25	-73	0	4.73	145	R	Lingual gyrus
-33	-87	21	-33	-83	22	4.54	43	L	Superior occipital gyrus
Pre-anesthesia > anesthesia									
No suprathreshold clusters									
<i>Left Heschel's gyrus</i>									
Anesthesia > pre-anesthesia									
-12	-15	6	-11	-16	8	5.05	28	L	Thalamus
-42	-36	15	-40	-35	16	4.9	32	L	Superior temporal gyrus
12	-18	6	11	-19	8	4.71	34	R	Thalamus
39	-18	33	38	-16	32	4.62	20	R	Precentral gyrus
-18	-42	54	-18	-39	49	4.17	20	L	Paracentral lobule
Pre-anesthesia > anesthesia									
No suprathreshold clusters									
<i>Left thalamus</i>									
Anesthesia > pre-anesthesia									
-15	-24	3	-14	-25	6	10.76	120	L	Thalamus
15	-24	3	14	-24	6	10.2	122	R	Thalamus
-42	-12	12	-40	-13	13	7.53	73	L	Insula
39	-15	12	37	-15	14	7.48	99	R	Insula
12	-24	54	12	-21	49	6.84	488	R	Medial frontal gyrus
-3	-12	57	-2	-8	52	6.65		L	Medial frontal gyrus
-36	-27	51	-36	-24	47	6.32	62	L	Precentral gyrus
Pre-anesthesia > anesthesia									
42	-75	36	43	-71	34	7.83	21	R	Precuneus
-6	-45	48	-5	-42	44	5.94	23	L	Precuneus
-45	-60	54	-45	-56	50	5.86	30	L	Inferior parietal lobule
-3	-54	9	-2	-53	11	5.06	22	L	Posterior cingulate
-15	15	6	-14	12	7	4.88	104	L	Caudate
18	15	9	17	13	10	4.11	76	R	Caudate

were observed in the connectivity maps linked to the hippocampus and the insula. Connectivity between the hippocampus and the PCC/precuneus and IPL, bilaterally were present only in the pre-anesthetized state. These are regions previously shown to be involved in episodic memory retrieval (Meltzer and Constable, 2005; Rekkas and Constable, 2005, 2006; Shannon and Buckner, 2004; Wheeler and Buckner, 2004) among other functions. In the anesthetized condition, connectivity between the insula and the ACC increased, while connectivity between the insula and secondary somatosensory areas decreased, bilaterally. Functional imaging studies with pain activation have revealed consistent activation of insula, ACC and SII in response to painful stimuli across several studies (see Tracey and Mantyh, 2007 for a review). These changes in connectivity involving the pain and memory circuits may reflect the analgesic and amnesic effects of 0.5 MAC sevoflurane anesthesia (Ramani and Wardhan, 2008). Seeding in

the thalamus we observed that anesthesia led to reduced connectivity between the thalamus and the PCC, a region that, in conjunction with the mesial parietal cortex and the precuneus, is usually deactivated in the unconscious state (Alkire et al., 2008; Franks, 2008) and a region that is one of the first to recover functionally from coma (Laureys et al., 2006). Therefore, the reduced connectivity between thalamus and PCC may reflect the subjects' loss of consciousness, as at this level of anesthetic all subjects were asleep and did not respond to commands. We also observed an increase in connectivity between the thalamus and motor/somatosensory regions under anesthesia. A possible explanation for such behavior is related to the fact that under anesthesia, increased disinhibition (Fiset et al., 1999; Schlünzen et al., 2004) leads subjects to have a tendency to move, mostly the lower limbs, noting that significant changes ( $p > 0.79$ ) in head motion were not observed between the pre- and anesthetized periods. Increased

**Table 3**

List of the regions showing differences in fc-fMRI between the pre- and anesthesia conditions, with higher-order functional areas of the left hemisphere.

MNI coord (mm)			Talairach coord (mm)			t Values	Cluster size	Brain region	Brodmann Area	
x	y	z	x	y	z					
<i>Left Hippocampus</i>										
Anesthesia>pre-anesthesia										
No suprathreshold clusters										
Pre-anesthesia>anesthesia										
−3	−54	21	−2	−52	22	7.69	253	L	Posterior cingulate	BA23
−45	−66	48	−45	−62	45	5.13	28	L	Inferior parietal lobule	BA40
6	−51	18	6	−49	19	4.96	48	R	Posterior cingulate	BA30
<i>Left Insula</i>										
Anesthesia>pre-anesthesia										
−9	27	0	−9	24	1	8.02	69	L	Caudate	
−27	15	−3	−26	11	0	4.41	39	L	Putamen	
Pre-anesthesia>anesthesia										
−60	−39	30	−58	−37	30	7.19	148	L	Inferior parietal lobule	BA40
51	39	0	49	37	3	7.06	22	R	Inferior frontal gyrus	BA46
−42	36	21	−41	35	20	6.23	128	L	Middle frontal gyrus	BA46
−60	9	9	−57	6	11	5.73	18	L	Precentral gyrus	BA44
69	−27	30	67	−25	30	4.74	73	R	Inferior parietal lobule	BA40
<i>PCC</i>										
Anesthesia>pre-anesthesia										
−66	−39	9	−63	−39	12	5.18	66	L	Superior temporal gyrus	BA22
42	−42	3	41	−42	7	4.02	34	R	Superior temporal gyrus	BA41
63	−45	6	61	−44	10	4.09	29	R	Superior temporal gyrus	BA22
Pre-anesthesia>anesthesia										
−3	−48	12	−2	−47	14	6.59	126	L	Posterior cingulate	BA30
3	−57	−45	3	−59	−35	4.36	33	R	Cerebellum	
−9	−48	−39	−8	−49	−30	4.04		L	Cerebellum	

motor activity under anesthesia may account for the increased connectivity between the sensory-motor cortex and the thalamus. Another explanation for the increased thalamo-cortical connection rests on the observations that anesthesia reduces thalamic communication, including the afferent sensory input to the thalamus (Alkire et al., 2000, 2005; Fiset et al., 1999) and that, under anesthesia, thalamic spontaneous activity is mainly driven by feedback connections coming from the cortical neurons (Vahle-Hinz et al., 2007). Our results suggest that these feedback connections are not equally attenuated by anesthetics such that an uneven reduction of afferent input to the thalamus highlights the most robust and direct connections of thalamus, such as those with the primary motor and somatosensory cortices. Further investigations are required to clarify whether the increased thalamo-cortical connectivity is related to the anesthesia induced decrease in sensory input to the thalamus or to the disinhibitory effects of anesthesia. Seeding in the primary somatosensory regions, we replicated the finding of increased connectivity between the thalamus and somatosensory cortices under anesthesia. We also observed a decreased connectivity with extrastriate (i.e. non-primary) visual areas. Multisensory connections are mediated and/or modulated by high-order connections and these are among the first regions to be affected under anesthesia (Ramani et al., 2007). This could explain the decrease in connectivity with the extra striate visual areas. Functional connectivity of the primary visual (BA 17) and auditory (Heschel's gyrus) areas appeared to be minimally modified by anesthesia.

In accord with previous findings, seeding in the PCC revealed connection throughout the default mode network (DMN; e.g. Buckner et al., 2008; Shulman et al., 1997), and this functional pattern seems to be minimally altered by sevoflurane at 0.5 MAC. This result is in agreement with previous studies showing that DMN is preserved in anesthetized monkeys (Vincent et al., 2007) and in comatose patients (Boly et al., in press), suggesting that the DMN connectivity is still preserved even in case of loss of consciousness.

Despite the observation that fc-fMRI patterns were mostly preserved under anesthesia, this study also revealed that anesthesia modulates the strength of functional connectivity in a network-specific manner. Consistent with an earlier study using midazolam

sedation (Greicius et al., 2008) we observed decreased connectivity in the high-order association areas (hippocampus and insula). However in the primary sensory cortical areas there was minimal alteration in fc-fMRI under anesthesia, with a trend towards an increase in connectivity. Such an increase in functional connectivity has also been observed under midazolam sedation (Kiviniemi et al., 2000). Other studies using anesthesia have demonstrated a dose-dependent reduction in fc-fMRI, both in animals (Lu et al., 2007; Vincent et al., 2007) as well as in humans (Peltier et al., 2005). In the study by Peltier et al. (2005), they observed a significant reduction in functional connectivity with regions connected to the motor cortex (98% reduction in connectivity) when 1 MAC sevoflurane anesthesia was administered. We did not observe such a large decrease in connectivity in the present study possibly because of the lower dose used: 0.5 MAC sevoflurane. In animals studies (Lu et al., 2007; Vincent et al., 2007) bilateral fc-fMRI has been observed to be maintained even at higher anesthetic doses.

In addition to the observation that most fc-fMRI patterns remain consistent in the pre- and anesthetized conditions, some anesthetic-induced modulations were also observed. The differential responses to fc-fMRI observed here (decreases in connectivity with the anesthesia in some regions, no change in others, and even increases in a few regions) suggest that anesthesia does not affect the brain in a homogeneous manner. Initially anesthesia alters the functional networks involved in higher-order cognitive function, such as memory and pain processing. Subsequently at higher doses the thalamo-cortical connections (White and Alkire, 2003) are affected. This sequence of effects is also supported by previous studies from our group showing that 0.25 MAC sevoflurane alters resting brain perfusion in a non-homogeneous manner across several regions (Qiu et al., 2008a) and that it first affects the higher-order association areas (Ramani et al., 2007).

Together the results from this study suggest that BOLD functional connectivity reflects intrinsic properties of the brain and that the strength of the intrinsic connections can be modulated in a spatially dependent manner by anesthesia with the higher-order cognitive areas exhibiting the largest changes in connectivity at 0.5 MAC dose.

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## Appendix A. Supplementary data

Supplementary data associated with this article can be found, in the online version, at doi:10.1016/j.neuroimage.2009.07.028.

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