Scintillation particle detection based on microfluidics


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A novel type of particle detector based on scintillation, with precise spatial resolution and high radiation hardness, is being studied. It consists of a single microfluidic channel filled with a liquid scintillator and is designed to define an array of scintillating waveguides each independently coupled to a photodetector. Prototype detectors built using an SU-8 epoxy resin have been tested with electrons from a radioactive source. The experimental results show a light yield compatible with the theoretical expectations and confirm the validity of the approach.

1. Introduction

A novel type of particle detector based on capillaries filled with liquid scintillators is being studied. It is possible with microfabrication technologies to build microfluidic devices with dimensional resolutions in the order of μm with a single photolithographic step. Such devices allow the easy manipulation of fluids inside capillaries overcoming the difficulties encountered with previous high spatial resolution liquid scintillation detectors made of capillary bundles [1–4]. Moreover, the possibility to circulate and renew the liquid scintillator makes the active medium of the detector intrinsically radiation hard and by changing the type of scintillator in the microchannels the same device can be used for different types of measurements. Microfabricated devices have been developed and studied to demonstrate experimentally the feasibility of such a detector based on microfluidics. Results obtained with a first series of prototypes are reported elsewhere [5]. This paper describes the results of the experimental investigation performed on the second generation prototype that demonstrates the validity of the approach.

2. Microfluidic scintillation detector

The main characteristics of the particle detector investigated are high spatial resolution for precise reconstruction of particle tracks, high radiation resistance to operate in very high radiation environments and low material budget to interfere as least as possible with the particles. Microfabrication and microfluidic technologies are appealing to develop such detectors. With a simple process it is possible to fabricate a single microfluidic channel defining a dense array of optically independent scintillating capillaries with dedicated photodetectors (Fig. 1a). The design is based on the assumption that there is no light transmission between the different capillaries due to the right angles being necessary for fluidic circulation at the end of the straight sections. Fluidic operation of the single microchannel is simple and liquid scintillators can be circulated and renewed. To demonstrate the concept of microfluidic scintillation detection, different prototype detectors have been fabricated and characterized.

3. Prototype detectors

The design of the prototype devices defines a detection zone, where impinging particles are detected, with high spatial resolution. 50 μm wide waveguides are separated by 10 μm wide SU-8 structures on a total length of 1 cm. In this region the microchannels are straight and parallel. They then fan-out from a pitch of 60 μm to a pitch of 2.3 mm over 1 cm to match the inter-pixel dis-
Fig. 1. 3D schematic representation, not to scale, of (a) the principle of operation of the microfluidic scintillation detector and of (b) the fabricated prototype detector. A single microfluidic channel defines an array of optically separated waveguides. When a particle interacts with the liquid scintillator in one of the branches the scintillation light is guided towards the corresponding photodetector. In the ideal case (a) all the area covered by the microchannel is used for detection (dotted contour). The layout of the prototype detector (b) has a reduced detection zone (dotted contour) to cope with the pitch of the photodetector available in the experimental test bench.

Fig. 2. Top view of the open metallized SU-8 channels of the prototype microfluidic scintillation detector. The upper side of the chip, in contact with the photodetector pixels, is not metallized to allow light transmission between the microchannels and the photodetector.

Fig. 3. Schematic representation of the cross-section of the microchannels at the level of the detection zone (not to scale). 200 μm thick SU-8 structures (10 μm wide) are separated by 50 μm on a silicon substrate. A layer of Au is deposited by sputtering.

Fig. 4. SEM image of the cross-section of the detection zone of the device. The microchannels are separated by high aspect ratio structures in SU-8.

Fig. 5. Schematic representation of the cross-section of the microchannels at the level of the detection zone (not to scale). 200 μm thick SU-8 structures (10 μm wide) are separated by 50 μm on a silicon substrate. A layer of Au is deposited by sputtering.

4. Fabrication of metallized SU-8 microchannels

The fabrication of the microchannels starts with the spin coating of 200 μm thick homogeneous layers of SU-8 (GM1075 from Gersteltec) on silicon wafers (100 s at 950 rpm), followed by a soft bake (10 min at 120 °C) and a slow cooling down (4 °C/min) to avoid the formation of cracks. The coated substrates are then exposed to UV light at a dose of 500 mJ/cm² through a mask to polymerize the desired structures. The exposure is followed by a post exposure bake (1 h at 95 °C) for the cross-linking of the exposed regions. The non-polymerized resin is then dissolved for 20 min in propylene glycol methyl ether acetate (PGMEA) revealing the microchannels (Fig. 4).

To prevent optical cross-talk between adjacent microchannels and to increase their optical properties, guaranteeing an efficient light transmission from the interaction point to the photodetector, the walls and the bottom of the channels are metallized. Two coat-
sions of 1.5 cm with Au-coated SU-8 microchannels. The results presented in this paper have been obtained by depositing metal in two steps. The reason to deposit metal in two steps is due to the temperature reached during the sputtering process. A single long deposition results in undulation and collapsing of the thin SU-8 walls while two shorter cycles are not harmful. Au and Al depositions have been performed. The results presented in this paper have been obtained with Au-coated SU-8 microchannels.

At this stage, the wafer is diced to separate 16 chips with dimensions of 1.5 cm x 2 cm (Fig. 2). They are then individually placed in a mechanical set-up to close the channels for microfluidic manipulation and to optically couple them to the photodetectors. Details of the set-up are given in the following section. The Au coating is removed from the side of the channels coupled to the photodetectors to allow transmission of the scintillation light. Removal is performed by dipping a small portion of the chip in an Au etching solution.

5. Experimental

The channel is closed by covering the chip with an Al-coated Mylar foil and encapsulating the whole in a black PMMA block. Optical gel is used to improve the light transmission between the microfluidic chip and the quartz window of the MAPMT. Tubes are connected to the inlet and outlet of the channel through the PMMA block. Filling and circulation of the liquid scintillator in the microchannel is performed with a syringe controlled by hand. In a later stage, and in particular for future beam test experiments, a fluidic circulation controller with a pump will be implemented. The channels are filled with a liquid scintillator (EJ-305 by Eljen Technology) selected for its high light output (80% of Anthracene) and for its emission spectrum peaking around 425 nm in the most sensitive region of the MAPMT. The photoelectric yield of the chip-MAPMT assembly is measured by exciting the liquid scintillator with electrons from a collimated 90Sr source which are considered as minimum ionizing particles (MIP). The coincidence of two plastic scintillating fibres (Kuraray SCF-78 0.5 mm square cross-section) placed underneath the detector is used as external trigger on the electrons. For each trigger the signals from the MAPMT channels are sent to a charge-to-digital converter (CAEN QDC V792).

Measurements have also been performed on an independent set-up with a non-pixelated photomultiplier tube (PMT) by masking all the microchannels except the one under test. Results from both test-benches match within the experimental uncertainties mainly due to the optical coupling of the thin microfluidic device orthogonal to the flat window of PMTs.

6. Results

The charge spectra of individual scintillating microfluidic channels (200 μm deep and 50 μm wide) are fitted with the convolution 
\[ F(x) \propto P(N, \bar{N}_{pe}) \otimes G(x, N, \sigma, \sqrt{N}) \]

where \( N \) is the number of events, \( \bar{N}_{pe} \) is the average number of photoelectrons per event and \( \sigma \) is the standard deviation of the distribution of single photoelectron counts. From the fit an average number of photoelectrons \( \bar{N}_{pe} \) per incident MIP of 1.65 is derived (Fig. 5).

This number is well in agreement with the theoretical expectations. Assuming that light is guided in the metal-cladded microchannels by attenuated total internal reflection (ATIR) [13] the expected photoelectric yield can be expressed as:

\[ \bar{N}_{pe} = N_{scint} \cdot \epsilon_{coll} \cdot \epsilon_{refl} \cdot \epsilon_{att} \cdot \epsilon_{in} \cdot \epsilon_{Qeff} \]

where \( N_{scint} \) is the number of scintillation photons produced isotropically in the microchannel by an impinging electron, \( \epsilon_{coll} \) is the collection efficiency of a rectangular metal-coated microchannel, \( \epsilon_{refl} \) is the gain due to the reflective end of the channel opposite to the photodetector, \( \epsilon_{att} \) is the transport efficiency due to optical absorption in the liquid scintillator, \( \epsilon_{in} \) is the transmission efficiency at the interface between the microchannel side where Au has been removed and the PMT and \( \epsilon_{Qeff} \) is the quantum efficiency of the PMT.

A MIP traversing a 200 μm channel filled with the liquid scintillator EJ-305 produces a number \( N_{scint} \) of photoelectrons in the order of 420 according to the technical data provided by Eljen Technology. The efficiencies \( \epsilon_{coll}, \epsilon_{refl} \) were estimated to be 0.03 and 1.4, respectively, by running Monte Carlo simulations. The attenuation length of the liquid scintillator EJ-305 is reported by Eljen Technology to be in the order of 3 m. One can safely assume that there is virtually no attenuation along the 2 cm long channels and that the transmission efficiency \( \epsilon_{att} \) is about 0.99. Around 425 nm, the wavelength of maximum emission of the liquid scintillator, the quantum efficiency of the photomultiplier tube \( \epsilon_{Qeff} \) is estimated to be about 0.14 [14]. The equation leads to \( \bar{N}_{pe} \approx 1.7 \).

A yield of 1.65 photoelectrons leads to a detection efficiency \( \epsilon_{det} \) up to 80% as derived from:

\[ \epsilon_{det} \approx 1 - P(0, \bar{N}_{pe}) = 1 - e^{-1.65} = 80.1\% \]
The active area of the prototypes covers 83% of the detection zone. This coverage is dictated by the ratio between the size of the SU-8 structures and the size of the scintillating capillaries. By staggering at least 2 planes a fully active detector can be obtained with small inactive edges. Moreover by staggering 3 layers the device can be self-triggering by requesting a coincidence of 2 planes. The staggering also increases the spatial resolution. A device with 3 staggered planes will be implemented to demonstrate experimentally the increased spatial resolution and the self-triggering capabilities of a fully active detector.

7. Conclusions

The working principle of a novel type of scintillation detector based on microfluidics has been demonstrated experimentally. A standard process of UV photopatterning has been optimized to fabricate structures with high aspect ratios (1:20) in thick layers of SU-8 in the order of 200 μm. They define a dense array of microchannels that are filled with liquid scintillator and optically coupled to the photocathode of an MAPMT. The photoelectric yield of the device measured with MIPs is in the order of 1.65 photoelectrons per MIP for 200 μm deep microchannels and is in full agreement with calculations. The high fill factor of the scintillating microchannels, the possibility to measure very close (<2 μm) to the edge of the device and the increased radiation hardness makes this novel type of detector particularly interesting for applications such as tracking particles in the field of high energy physics. Moreover, the compact design of microfabricated scintillation detectors opens the way to numerous applications where macrodetectors cannot be used like in situ dosimetry for hadron therapy.

References


Biographies

Alessandro Mapelli received his MSc in microengineering from the Ecole Polytechnique Fédérale de Lausanne (EPFL), Lausanne, Switzerland in 2005. He has since been working at the European Organization for Particle Physics (CERN) in Geneva, Switzerland for the formation of a PhD from EPFL. He was involved in the development of a scintillating fibre tracker (ALFA—Absolute Luminosity For ATLAS) to measure the absolute luminosity of the LHC collider at the interaction point of the ATLAS experiment. His work is focused on the development, studies and integration of microsystems to particle detectors.

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Noelia Vico Triviño received her BSc in Physics and MSc in electronic engineering from the University of Granada, Spain, in 2007 and 2009, respectively. She carried out her MSc project in the Laboratoire des Microsystèmes (LMIS4) at the Ecole Polytechnique Fédérale de Lausanne (EPFL), Switzerland in 2009. She currently pursues her PhD in photonics at the Laboratory of Advanced Semiconductors for Photonics and Electronics (LASPE) at EPFL. Her research is focused on quantum dots and nanowires grown by molecular beam epitaxy (MBE).

Philippe Renaud was born in 1958. He received the diploma in physics from the University of Neuchatel, Neuchatel, Switzerland, in 1983, and the PhD degree from the University of Neuchatel, Neuchatel, Switzerland, in 1988. He was involved in the theoretical and experimental study of magnetoelastic effects. During 1988–1989, he was a postdoctoral researcher at the University of California, Berkeley. From 1990 to 1991, he was a postdoctoral researcher at the IBM Zurich Research Laboratory. In 1992, he joined the Sensors and Actuators Group, Swiss Center for Electronics and Microtechnology (CSEM), Neuchatel, Switzerland. In 1993, he became an assistant professor at the Swiss Federal Institute of Technology Lausanne (EPFL), Lausanne, where he was appointed a full professor in 1997 and is the director of the Center of MicroNanoTechnology (CMI), one of the largest state-of-the-art academic clean room facilities in the world, with processing equipment for training and scientific purposes in microelectronic and microfabrication processes. In the summer of 1996, he was a visiting professor at Tohoku University, Japan. His current research interests include microsystem design, microfabrication technologies for microelectromechanical system (MEMS) applications, microfluidics, and bio-MEMS applications. Prof. Renaud is the Chairman of the International Nanotech-Conference on Micro- and Nanotechnologies for the Biosciences and annually in Montreux, Switzerland.

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